

Anatomically Accurate Motorized Shoulder Model



WPI

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Abstract

Despite its significance within the body, educational tools effectively modeling the intricacies of the shoulder joint are scarce. Seeking to address this void, our team continued the development of a life-sized model comprising the scapula, humerus, and a removable clavicle. Our model aims to more accurately replicate the nuanced scapulohumeral rhythm observed during abduction of the humerus, a process integral to understanding the shoulder joint. The scapulohumeral rhythm, orchestrating the coordinated movement between the scapula and humerus during various shoulder motions, particularly abduction, is paramount for maintaining shoulder joint stability and functionality. Our developed rig serves as an excellent foundation for future teams to supplement. A clear path forward is laid for any future teams to fully develop a valuable educational resource for students, healthcare professionals, and medical enthusiasts seeking a comprehensive understanding of the human shoulder.

Acknowledgements

Our team would like to thank several individuals for their efforts in aiding us in completing our project. We would like to thank Pradeep Radhakrishnan for providing us with a space where our team could thrive and construct the model. We would additionally like to thank Peter Hefti in providing us the tools we needed to build the final model. Finally, we'd like to thank our advisor, Fiona Levey, for her incredible guidance and support throughout this project.

Authorship

Our MQP project in creating an anatomically accurate motorized shoulder model was completed through the efforts of Gray Rahm, Cameron Leffler, and Sean Merone. Each member contributed towards the research behind the construction of the model and the materials necessary for the project. Construction of the model's cage, design, schematics, and circuitry was a team effort led by Gray Rahm. The code for the project was developed by Cameron Leffler. The final report submitted to the standards of the WPI MQP report guidelines was a team effort led by Sean Merone.

Cameron Leffler will continue to work on the project for the remainder of the academic year and will submit his MQP report at the conclusion of the academic year. He will be working on creating a 3D animation of the scapulohumeral rhythm using Blender.

Table of Contents

Abstract	0
Acknowledgements	1
Authorship	3
Table of Contents	4
Table of Figures	6
Table of Tables	8
1.0 Introduction	9
2.0 Background	10
2.1 Scapulohumeral Relationship.....	10
2.2 Previous Work on the Model.....	14
2.2.1 2021-2022 MQP: Anatomically Accurate Motorized Shoulder Model with Scapula Movement.....	15
2.2.1.1 3D Printed Bones.....	16
2.2.1.2 Mounting the Bones and Motors.....	19
2.2.1.3 2021-2022 Team's Final Product and Data Collection.....	21
2.2.2 2022-2023 MQP: Realistic Shoulder Model with Soft Tissue Attachments.....	22
3.0 Methodology	23
3.1 Design Goals and Constraints.....	23
3.2 Rig Design Concepts.....	24
3.2.1 Channel Design Concept.....	24
3.2.2 Cage Design Concept.....	25
3.3 Scapular Rotation.....	30
3.4 Humeral Abduction.....	33
3.5 Material Selection.....	40
3.5.1 Motor Selection.....	40
3.5.2 Connecting Wires.....	43
3.5.3 Motor Driver.....	46
3.6 Cage Construction and Implementing a Matlab Code.....	48
3.6.1 The Cage.....	48
3.6.2 Coding and the MATLAB Model.....	52
3.6.3 Circuit Design.....	57
3.7 Testing.....	61
3.7.1 Testing Relative Position.....	62
3.7.2 Motor Calibration.....	62
3.7.3 Testing Individual Motors.....	62
3.7.4 Troubleshooting.....	63
3.8 Results.....	63
3.8.1 Partially Completed Rig.....	63
3.8.2 Interactive Scapula Position Graph.....	64

4.0 Discussion.....	65
4.1 Motor Location and Function.....	65
4.2 Materials Selection.....	65
5.0 Broader Impacts.....	66
5.1 Engineering Ethics.....	66
5.2 Social and Global Impact.....	67
5.3 Environmental Impact.....	68
5.4 Economic Impact.....	69
6.0 Conclusions and Future Work.....	70
7.0 Appendices.....	71
7.1 MatLab Code.....	71
8.0 References.....	93

Table of Figures

Figure 1: Depiction of the Scapula and its varying regions (Teach Me Anatomy, 2022).....	10
Figure 2: Depiction of the Scapula Ridge and its varying joints (Teach Me Anatomy, 2022).....	11
Figure 3: Depiction of the Humerus and its varying regions (Teach Me Anatomy, 2022).....	11
Figure 4: The type A pattern of scapulohumeral rhythm. (Bagg, 2016).....	12
Figure 5: The type B pattern of scapulohumeral rhythm. (Bagg, 2016).....	13
Figure 6: The type C pattern of scapulohumeral rhythm. (Bagg, 2016).....	13
Figure 7: Sketch of the Secondary Rod Preliminary Design (Deane et al., 2022).....	15
Figure 8: Sketches of top, Front and side view of the Scapulothoracic Joint utilized within the Secondary Rod Design (Deane et al., 2022).....	16
Figure 9: Sketches of top, front, and side view of the unique slot feature representing the Scapulothoracic joint (Deane et al., 2022).....	16
Figure 10: Front and back view of model true to scale (Biomedical Modeling Inc.).....	17
Figure 11: Left and right view of the model true to scale (Biomedical Modeling Inc.).....	17
Figure 12: Front and Side Views of Full Shoulder Rig Assembly without Soft Tissue (Deane et al., 2022).....	17
Figure 13: Front and Right-side View of Rib Connections (Deane et al., 2022).....	18
Figure 14: Corresponding digital plot (left) that was transferred to the plywood (right) for accurate bone positioning (Deane et al., 2022).....	19
Figure 15: Clavicle and plywood attachments (Deane et al., 2022).....	20
Figure 16: Second stationary motor mount designed to secure a single Planetary Gearbox Nema 17 stepper motor to the top of the t-slot beam (Deane et al., 2022).....	20
Figure 17: Sketch of glenohumeral joint design (Deane et al., 2022).....	20
Figure 18: Sketch of glenohumeral joint design (Deane et al., 2022).....	21
Figure 19: Isolated sketch of sternoclavicular joint design (Deane et al., 2022).....	21
Figure 20: Side, top, and front view of shoulder model (Deane et al., 2022).....	22
Figure 21: Humeral and Scapular Motion.....	23
Figure 22: Channel Design Concept.....	25
Figure 23: Model in the cage.....	26
Figure 24: Vertice motor design (left) and track method design (right).....	27
Figure 25: Motor placements along the faces of the cage.....	28
Figure 26: Constructed and Realized Cage.....	29
Figure 27: Potential movements of the Scapula (Physiotutors, 2023).....	30
Figure 28: A simplified view of each of the motor attachment points.....	32
Figure 29: Key Points of Mass Distribution within the Scapula.....	32
Figure 30: An example of the Rodrigues' Rotation Formula. (YouTube channel Mathoma).....	33
Figure 31: All Angles and Lengths during Humeral Abduction.....	35
Figure 32: The model 17HS13-0404S-PG27 data sheet (StepperOnline, 2020).....	42
Figure 33: The NEMA model 17HS19-1684S-PG27 motor (StepperOnline, 2020).....	43
Figure 34: The NEMA model 17HS13-0404S-PG27 motor (StepperOnline, 2020).....	44

Figure 35: The Young's modulus (10^6 psi) of different materials similar to collagen.....	45
Figure 36: Braided Fishing Line.....	46
Figure 37: Braided Fishing Line attached to a 17HS13 motor.....	47
Figure 38: The figure of the driver (Pololu, 2024).....	48
Figure 39: How to adjust current limit potentiometer.....	49
Figure 40: Posterior View of the Cage.....	50
Figure 41: Lateral View of the Cage.....	51
Figure 42: Lateral Midline View of the Cage.....	52
Figure 43: Top View of the Cage.....	52
Figure 44: Bottom View of the Cage.....	52
Figure 45: Supporting Bars of the Cage.....	53
Figure 46: A simplified view of each of the motor attachment points.....	54
Figure 47: Acceleration of point A over degrees Abduction.....	55
Figure 48: Acceleration of point B over degrees Abduction.....	56
Figure 49: Acceleration of point C over degrees Abduction.....	57
Figure 50: Acceleration of point D over degrees Abduction.....	57
Figure 51: Acceleration of point E over degrees Abduction.....	57
Figure 52: Acceleration of point F over degrees Abduction.....	58
Figure 53: The 2022-2023 Team's Fully Assembled Physical Circuit (McEvelly et al., 2022).....	59
Figure 54: Second Iteration of the Circuitry.....	60
Figure 55: Updated Schematic of the Circuitry.....	62
Figure 56: Zoomed in Schematics of the Arduinos.....	63
Figure 57: The Interactive Scapula Position Graph.....	67

Table of Tables

Table 1: Abduction Ratio (Average Arm Rotation:Scapular Rotation) (Bagg, 2016).....	12
Table 2: Rib Connection Points (Deane et al., 2022).....	18
Table 3: Total rotation of the scapula in all three directions during 30° increments of abduction under “control” (Yabata, 2022).....	31
Table 4: Total rotation of the scapula in all three directions during 30° increments of flexion under “control” (Yabata, 2022).....	31
Table 5: Nomenclature Table for Humeral Abduction.....	34
Table 6: Solving for the Necessary Force and the Position of the Motor.....	36
Table 7: Rotation of the Humerus during Abduction and Flexion (Yabata, 2022).....	37
Table 8: The chosen orientation of the wires from the motor to the driver.....	48
Table 9: Details of Aluminum Extrusion Rods.....	50
Table 10: Cost of Materials Used to Modify the Rig.....	73

1.0 Introduction

The human shoulder stands as a marvel of anatomical complexity, functioning as a pivotal joint essential for a wide range of movements. Despite its significance, educational tools that effectively model the intricacies of the shoulder joint are scarce. In response to this gap, we have continued the mechanization of a life-sized model encompassing the scapula, humerus, and clavicle. This creation aims to replicate the nuanced motion observed during abduction, a process integral to understanding the scapulohumeral rhythm.

The scapulohumeral rhythm refers to the coordinated movement between the scapula (the shoulder blade) and the humerus (the upper-arm bone) during various shoulder motions, particularly abduction. This rhythm plays a crucial role in maintaining the stability and functionality of the shoulder joint. Our mechanization of the model seeks to provide a tangible and visually instructive representation of this intricate interplay, offering a valuable educational resource for students, healthcare professionals, and anyone interested in comprehending the complexities of the human shoulder.

By combining anatomical accuracy with a focus on motion dynamics, our model offers a hands-on approach to learning about the scapulohumeral rhythm. Through its open and spacious design, users can gain a tangible understanding of the spatial relationships and articulations involved in shoulder abduction. This educational tool not only serves as a valuable asset in academic settings but also contributes to a broader appreciation of human anatomy and biomechanics.

In the subsequent sections, we will delve into the key components of our contribution to the shoulder model's development through accurate relative motion, visual representation, exploring the anatomical principles it embodies, and elucidating the educational benefits it presents. From biomechanical insights to practical applications, this life-sized shoulder model is poised to enhance the understanding and appreciation of one of the body's most intricate and essential joints.

2.0 Background

2.1 Scapulohumeral Relationship

The movement of the shoulder consists of two primary bones, those being the the scapula and the humerus, with the clavicle factoring in largely as support and a connection to the sternum in the center of the ribcage. Understanding the relationship of movement between these two bones is key towards accurately modeling and displaying how the shoulder joint functions. The joints connecting these bones are equally as integral to this system, with the two most prominent in the system being the glenohumeral joint, which serves to connect the scapula and the humerus, and the acromioclavicular joint, which connects the scapula and the clavicle.

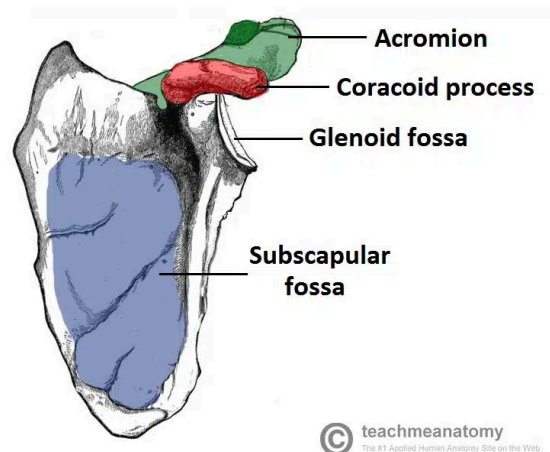


Figure 1: Depiction of the Scapula and its varying regions (Teach Me Anatomy, 2022)

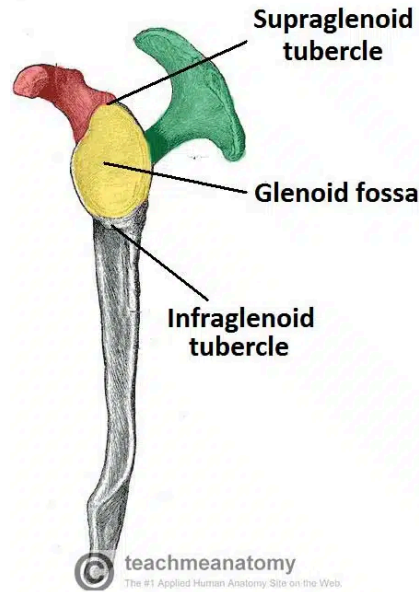


Figure 2: Depiction of the Scapula Ridge and its varying joints (Teach Me Anatomy, 2022)

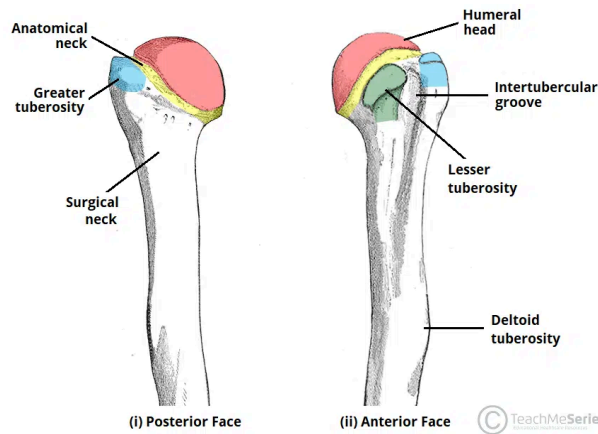


Figure 3: Depiction of the Humerus and its varying regions (Teach Me Anatomy, 2022)

Upon abduction of the humerus, the scapula transitions and rotates to accommodate the movement in several stages, however, where the humerus exists and moves on a two dimensional plane assuming there is no antepulsion or retropulsion, the scapula shifts and rotates in a three dimensional manner, with each stage of movement being met with a different facet of rotation. Nikita Igoshin’s 2022 Independent Study Project (ISP) focused heavily on these different stages of movement. Igoshin’s ISP based its findings on the work from “A Biomedical Analysis of Scapular Rotation During Arm Abduction in the Scapular Plane” written by Stephen D. Bagg, MD, MSc and William J, Forrest MD, MSc. with their results displayed below in Table 1.

Range	Average Arm Rotation (AA) : Scapular Rotation (SR)
0-20.8°	1:0
20.8-81.8°	4.29:1
81.8-139.1°	1.71:1
139.1-170°	4.49:1
20.8-170°	2.25:1

Table 1: Abduction Ratio (Average Arm Rotation:Scapular Rotation) (Bagg, 2016)

The results displayed indicate the ratio of movement between the humerus and the scapula, with the first range being especially of note as until the humerus meets a 20.8° angle with the horizontal axis, there is negligible movement in the scapula. As abduction of the humerus continues, transitional movement of the scapula and rotational movement of the scapula differentiate. The angle of the scapula was found to follow one of three patterns in its rotational movement with respect to the angle of the humerus through the analysis of a large number of subjects. The patterns are depicted below in figures 4, 5, and 6.

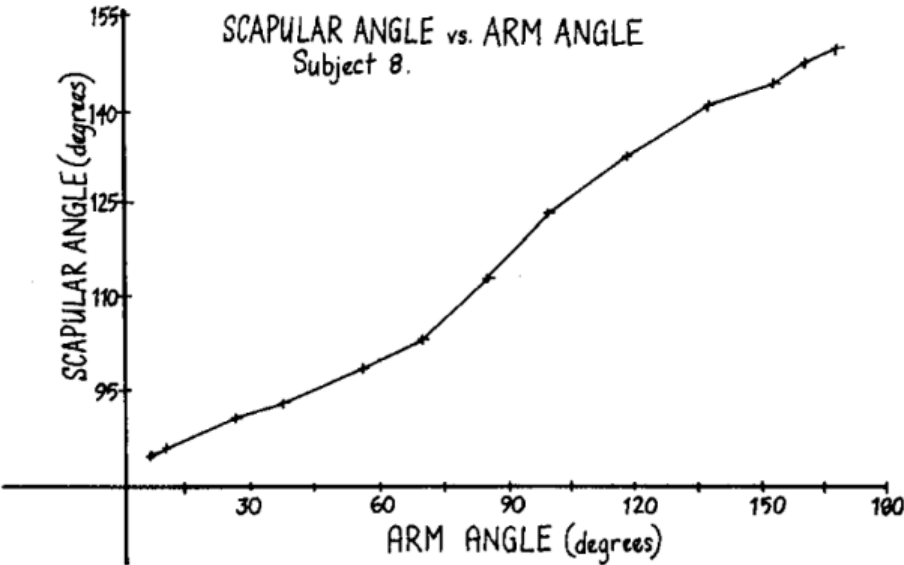


Figure 4: The type A pattern of scapulohumeral rhythm. (Bagg, 2016)

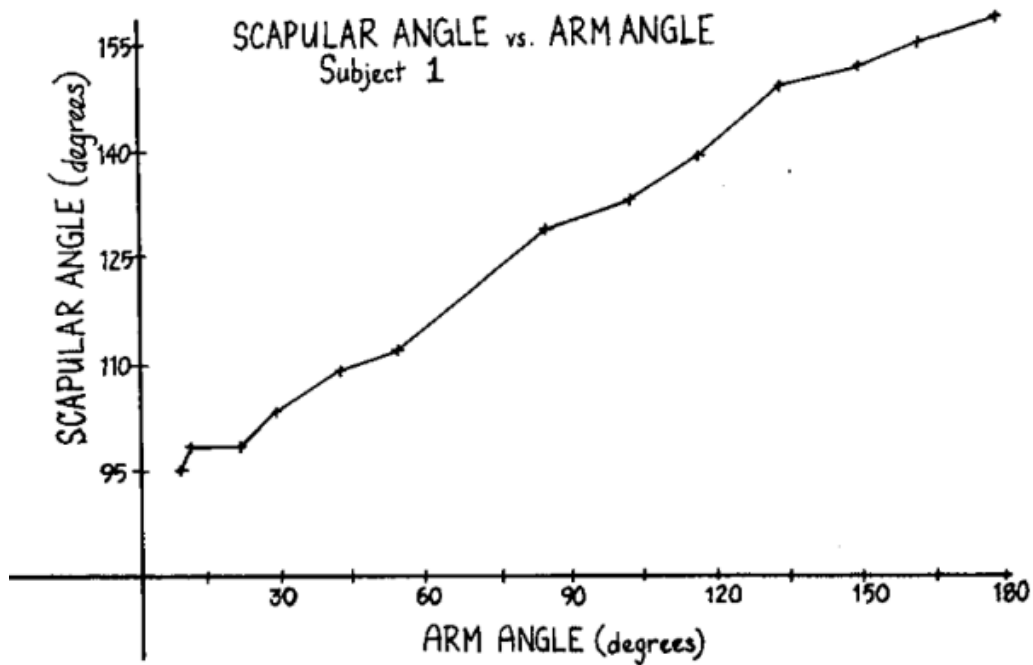


Figure 5: The type B pattern of scapulohumeral rhythm. (Bagg, 2016)

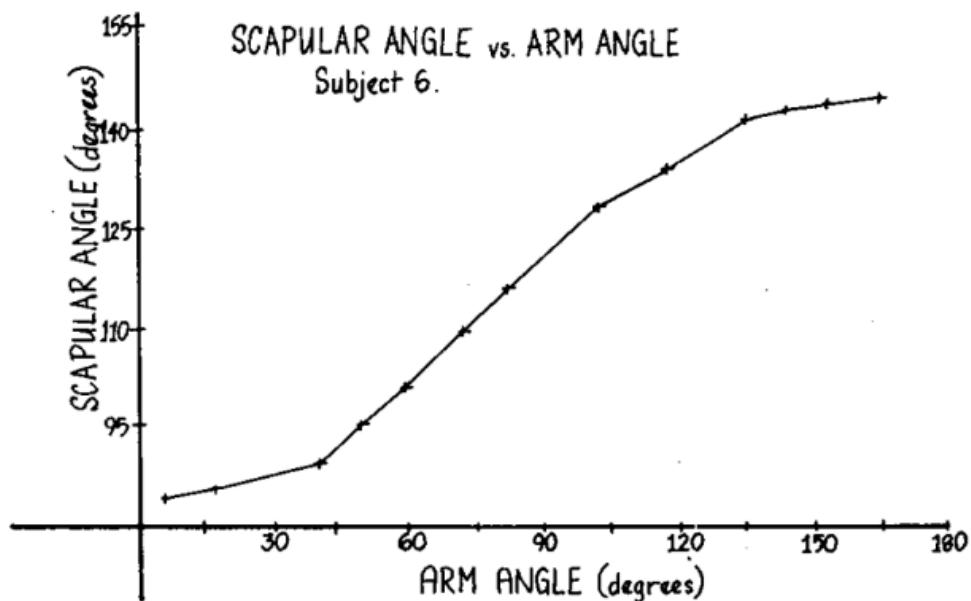


Figure 6: The type C pattern of scapulohumeral rhythm. (Bagg, 2016)

The beginning position of the scapula and the point at which the scapula begins to rotate in accordance with the movement of the arm differ greatly between the three patterns, with patterns A and C beginning at a starting angle of around 85 degrees to the vertical axis with

pattern B beginning at 95 degrees to the vertical axis. The rate at which the scapula rotates and shifts, while not uniform between the patterns, is largely comparable at the later stages of rotation, with an arm angle of 60 to 80 degrees being the point where the three patterns begin to line up. These results indicate that while the scapulohumeral rhythm differs between individual subjects, it can be approximated and averaged to produce tangible and uniform results. Understanding this, the team opted to use the ratios found by Nikita Igoshin for the scapulohumeral rhythm as the foundation for the project.

2.2 Previous Work on the Model

This project is a continuation of two previous MQP efforts. Two prior teams similarly conducted their own work and tackled the project with different concepts. The 2021-2022 team was largely centered around the development of the bones and structure that the model would rest on and the construction of a rig to demonstrate scapulohumeral rhythm during abduction from 0 to 60 degrees. The group of students procured 3D models of the bones of the shoulder, the scapula, the humerus, and the clavicle as well as the rib cage; to which they added blocks for mounting. The team then 3D printed the models out of PLA (Polylactic acid; a common 3D printing filament). They then mounted the rib cage on to plywood and created a simple rig focused on replicating abduction movement of the shoulder through nylon threads and motors, with partial success.

The 2022-2023 team continued construction of the model, this time focusing on the addition of ligaments and altering motor attachment points to properly replicate the components of an anatomical shoulder. Their team intended to select materials that accurately replicated the function of shoulder tendons, ligaments, and muscles, utilizing a number of different materials to replicate the movement of the humerus.

Our team similarly continued the construction of a rig to replicate movements, utilizing the models produced by the 2021-2022 team and the ideas of an extraneous point of connection from the 2022-2023 team. This was the foundation that our team worked from, building and improving upon their previous designs and accounting for facets and complications the previous teams did not have the time to consider.

2.2.1 2021-2022 MQP: Anatomically Accurate Motorized Shoulder Model with Scapula Movement

The 2021-2022 team gave a clear indication of their design process throughout their project. The shoulder joint, including the scapula, humerus, clavicle, and rib cage would be mounted on a supporting board with motors providing the force needed to conduct movement of the humerus and scapula. Their primary designs were as follows: a secondary rod design and a pulley system trailing the length of the humerus.

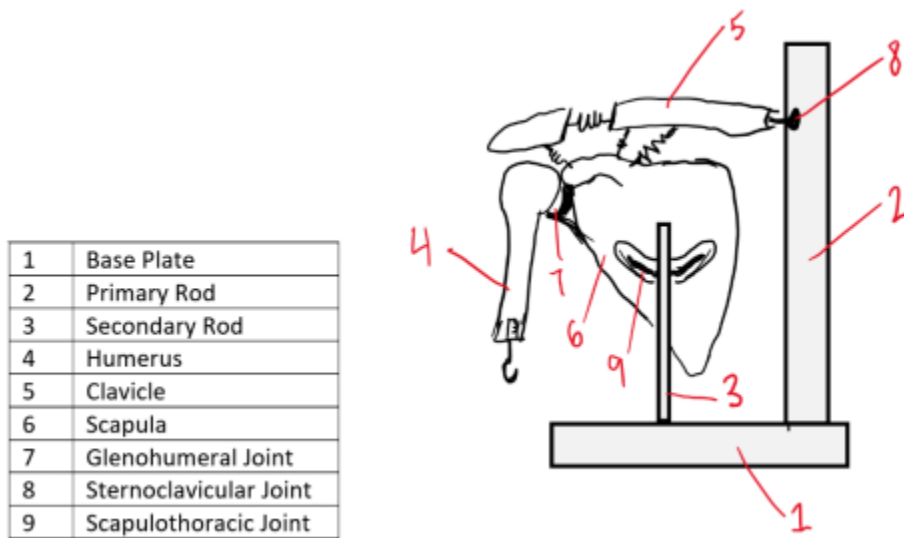


Figure 7: Sketch of the Secondary Rod Preliminary Design (Deane et al., 2022)

The above figure displays the shoulder joint in its entirety alongside the secondary rod system, with each part labeled within the table on the left. The Secondary Rod was intended to function as another source of support as well as a guiding hand for scapular rotation. It would achieve these goals by connecting to the scapula through a ball and joint socket in a slot displayed below in figure 8 and figure 9. The slot is curved and hollow so as to allow the scapula to rotate during translation throughout the humeral abduction process. During the rotation and translation of the scapula, the ball is free to slide through the hollow interior of the slot from the center to the edges to accurately mimic the movement of the scapula within the shoulder joint. Similarly during humeral flexion, the ball is free to return to its initial position.

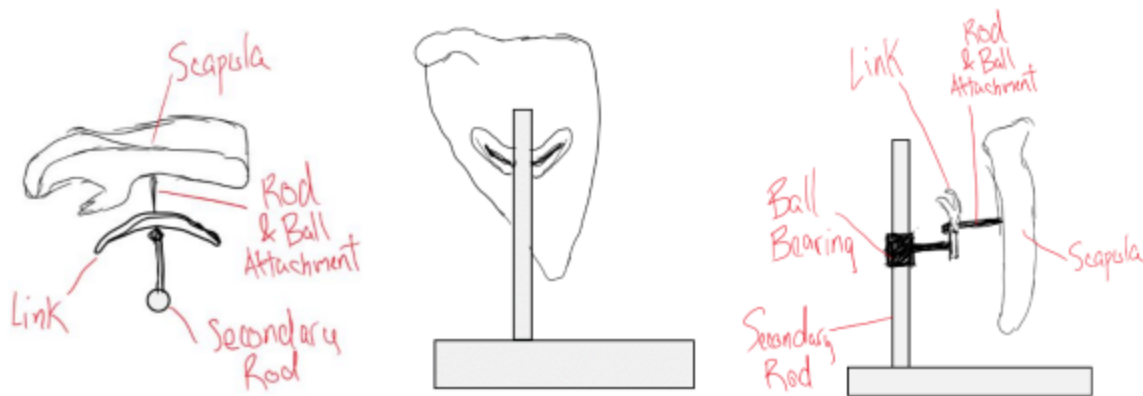


Figure 8: Sketches of top, Front and side view of the Scapulothoracic Joint utilized within the Secondary Rod Design (Deane et al., 2022)

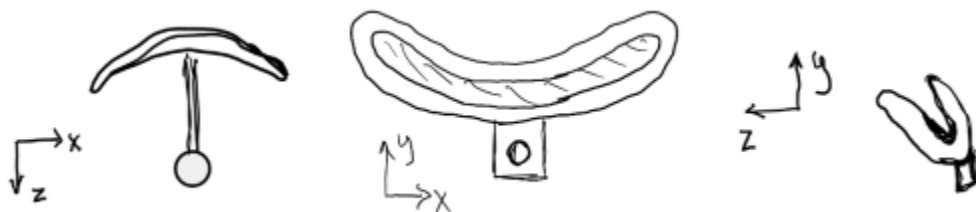


Figure 9: Sketches of top, front, and side view of the unique slot feature representing the Scapulothoracic joint (Deane et al., 2022)

The secondary rod idea was ultimately scrapped by the 2021-2022 team due to the additional parts that would be required to provide the force necessary to replicate the motion of the scapula and humerus. These additional parts physically intersected the secondary rod, preventing the motion from completion. However, this idea of another point of connection is something our team sought to continue with our project. The 2021-2022 team's second primary design was the development of a pulley system that trailed the length of the humerus and scapula as described in section 2.2.1.3.

2.2.1.1 3D Printed Bones

The 2021-2022 team purchased files of the bones that they then 3D printed (Figure 10 and Figure 11). In order to fasten the ribcage to the plywood, a 0.75in x 0.75in rectangular segment was added to each rib at varying lengths to meet at one plane. These fastenings are

shown in Figure 12 and Figure 13. The points of these connections are displayed below in Table 2 and Figure 14.

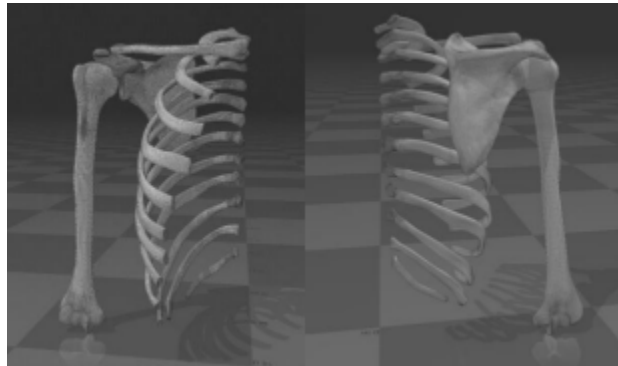


Figure 10: Front and back view of model true to scale (Biomedical Modeling Inc.)

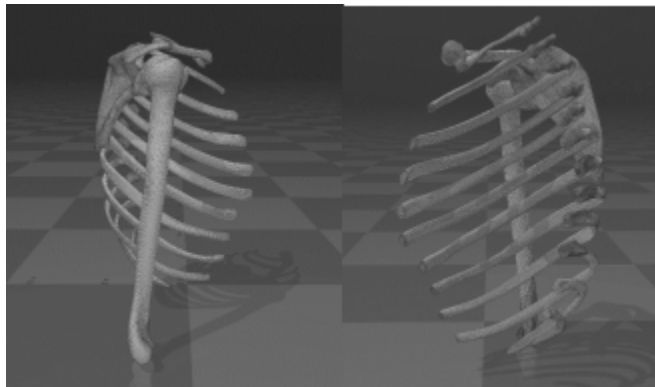


Figure 11: Left and right view of the model true to scale (Biomedical Modeling Inc.)

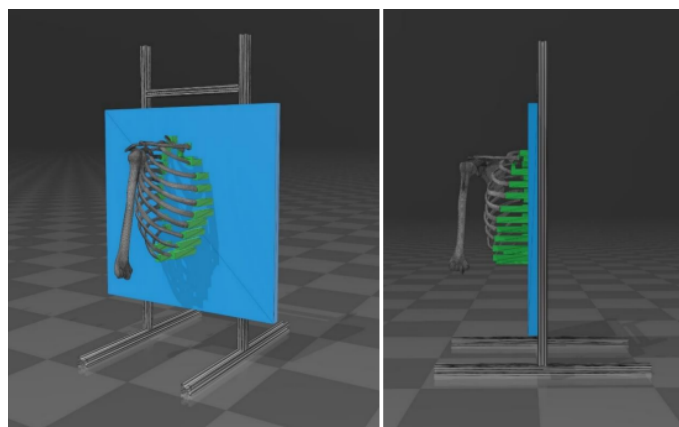


Figure 12: Front and Side Views of Full Shoulder Rig Assembly without Soft Tissue (Deane et al., 2022)

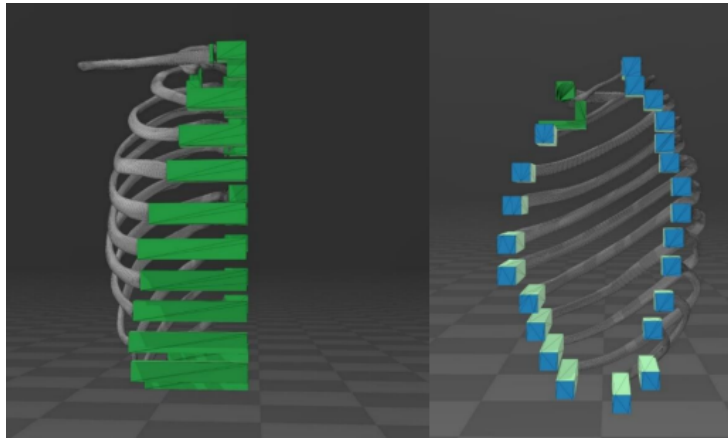


Figure 13: Front and Right-side View of Rib Connections (Deane et al., 2022)

Y	Z	Y	Z
38.8411	277.6354	160.753	105.5732
15.2039	238.4864	168.1988	142.0047
5.6789	204.5192	170.3961	171.297
0	164.5711	177.8404	196.7875
0	132.4797	177.8404	223.5691
22.1709	103.6558	165.7629	248.0114
29.3163	74.9135	160.8711	268.1104
42.4981	44.6453	160.8711	290.4167
59.4609	14.6593	149.1488	312.0448
117.1742	0	130.0988	325.9589
145.7492	24.1843	126.6992	345.0089
149.1488	76.648	59.4608	322.4804

Table 2: Rib Connection Points (Deane et al., 2022)

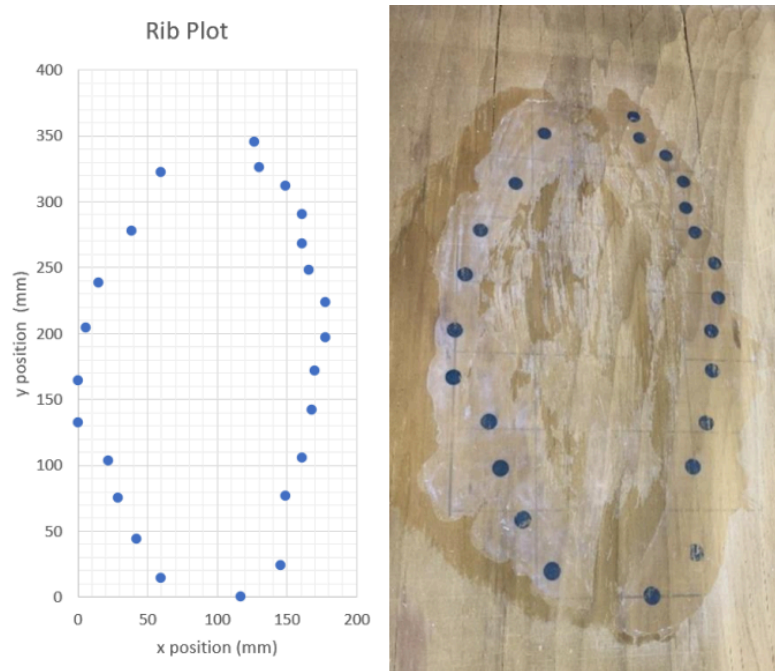


Figure 14: Corresponding digital plot (left) that was transferred to the plywood (right) for accurate bone positioning (Deane et al., 2022)

2.2.1.2 Mounting the Bones and Motors

The bones were mounted and secured to 3D printed blocks which were then fastened to the points on the plywood above as designated in section 2.2.1.1, the clavicle and motors were mounted differently due to their differing functions. The clavicle was mounted to a plywood block through a ball and socket joint that allowed for limited rotational movement. The motors and circuits of the 2021-2022 team were mounted to the rear side of the plywood to not obstruct the movements or visual of the shoulder during its abduction, however, doing so introduced a large amount of friction between the plywood board and the nylon monofilament fishing line utilized in their pulley system as they travel over the top of the plywood. The mounts utilized are displayed below in Figures 15 through 19.

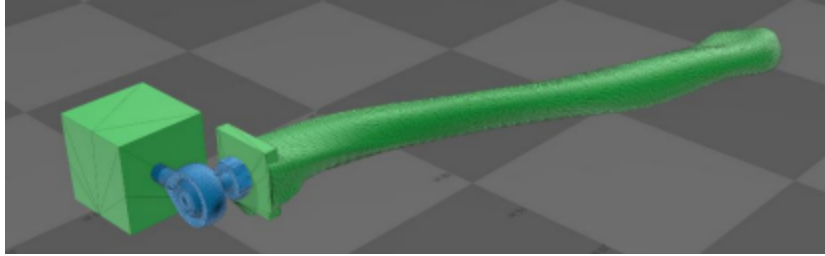


Figure 15: Clavicle and plywood attachments (Deane et al., 2022)

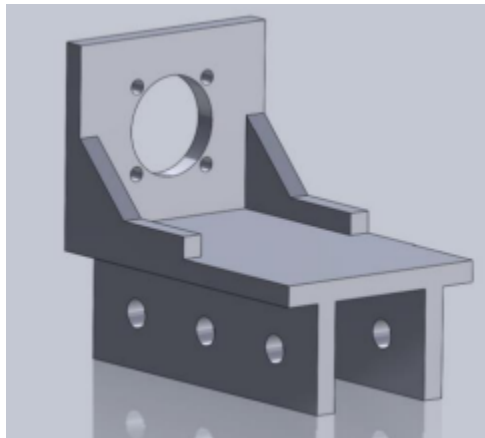


Figure 16: Second stationary motor mount designed to secure a single Planetary Gearbox Nema 17 stepper motor to the top of the t-slot beam (Deane et al., 2022)

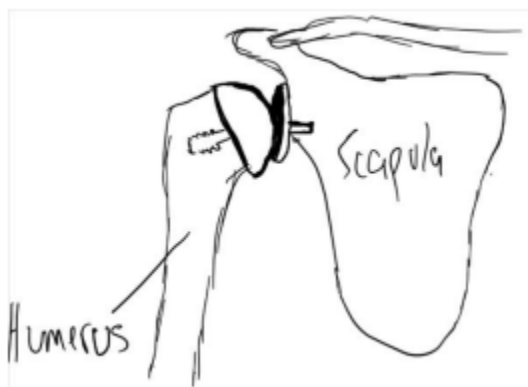


Figure 17: Sketch of glenohumeral joint design (Deane et al., 2022)



Figure 18: Sketch of glenohumeral joint design (Deane et al., 2022)

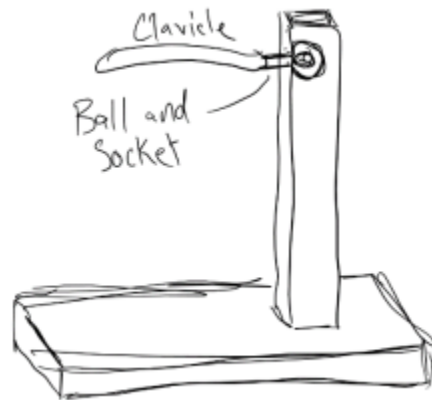


Figure 19: Isolated sketch of sternoclavicular joint design (Deane et al., 2022)

2.2.1.3 2021-2022 Team's Final Product and Data Collection

The 2021-2022 team unfortunately did not have the time to flesh out a fully functioning system to induce movement in the arm, as their project focused much more heavily on creating the models of the bones and bringing them to fruition. That being said, their motorized design had numerous aspects that our team built upon. Their design utilized a motor system that trailed the length of the arm and was attached to the other side of the wooden board used to hold and support the ribcage. While the use of a motor system is the most cost-effective option available, the angle the force was delivered made vertical movement of the arm incredibly intensive, as a

vast majority of the force was pulling the arm into the shoulder socket rather than upwards to display abduction.

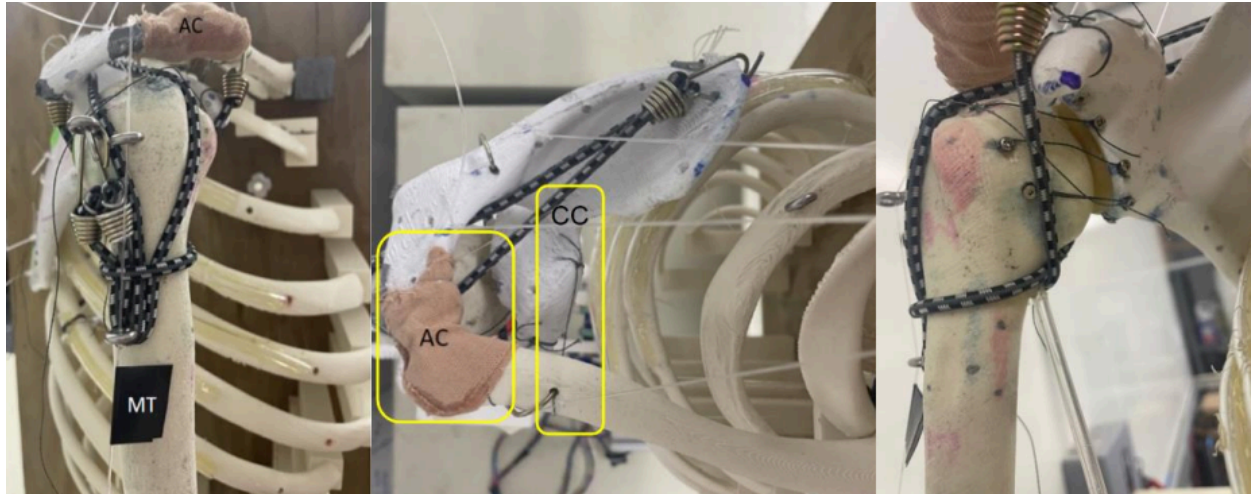


Figure 20: Side, top, and front view of shoulder model (Deane et al., 2022)

2.2.2 2022-2023 MQP: Realistic Shoulder Model with Soft Tissue Attachments

The 2022-2023 team focused far more heavily on the addition of materials that would replicate biological functions within the shoulder. The team 3D printed several slabs of polymer materials and attached them to the areas of important tendons and muscle groups to simulate restrictions the shoulder would experience. However, these materials had difficulty remaining attached in the intended manner and often blocked visibility of the more important movements of the model. The inefficiency and other problems introduced by these design options were heavily accounted for when forming our own designs for the rig.

3.0 Methodology

3.1 Design Goals and Constraints

Our team focused our project around numerous different smaller scale goals, each of which were focused on completing our overarching goal of improving upon the design of the two previous MQP team's models to more accurately reflect shoulder movement through abduction of the humerus. To achieve this goal, our team had to operate under a number of constraints, primarily seeking to minimize the cost of the project so as to make the final product as accessible and affordable as possible. Other constraints such as accessible materials and machines to shape these materials would additionally limit the abilities of the team to develop the final product. Further constraints including the size and the transportability of the rig similarly limited potential designs. Our overarching objective would be completed through our other goals which were similar to the previous MQP team's goals in developing an efficient rig that would provide adequate force to lift the humerus whilst rotating and transitioning the scapula appropriately in response to the humerus's position. The rig should additionally be capable of completing the motion displayed in figure 21 an indefinite number of times without requiring frequent replacement of parts.

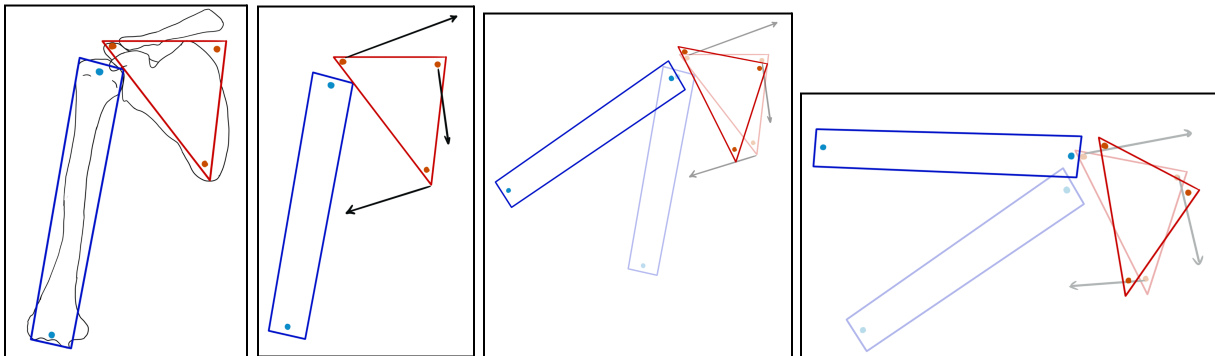


Figure 21: Humeral and Scapular Motion

Our first goal was to calculate and replicate accurate motion of the scapula. The scapula shifts and rotates on a three dimensional plane and has a constantly shifting center of rotation alongside a complex geometric shape that can make accurately replicating its movement

difficult. Our efforts to reflect this movement are detailed in section 3.3 Scapular Rotation. Our second goal was to achieve the full desired range of motion, raising the humerus from 0° to 120° with the vertical axis. Our final goal to improve the previous design of the model was to accurately replicate relative motion between the scapula and humerus. While the movements of the scapula and humerus aren't causing relative motion between one another in the model like they would in the body, the motors in our rig would accurately replicate the relative movement of the bones associated with the scapulohumeral rhythm described in our design concepts and rig designs in section 3.2.

3.2 Rig Design Concepts

To achieve the scapulohumeral rhythm and motion desired, our team created two preliminary design concepts with a number of smaller variations.

3.2.1 Channel Design Concept

One preliminary design concept our team focused on was the idea of implementing a channel to follow the length of the humerus, mimicking the design of the previous MQP team's final implemented design. Where the previous teams had the wires and supporting materials on the outside surface of the humerus, this design would involve drilling a channel into and along the length of the humerus and a portion of the scapula, where the wires would be run through and over the collar into the plywood board supporting the model where the motors would pull from. This design is displayed below in figure 22.

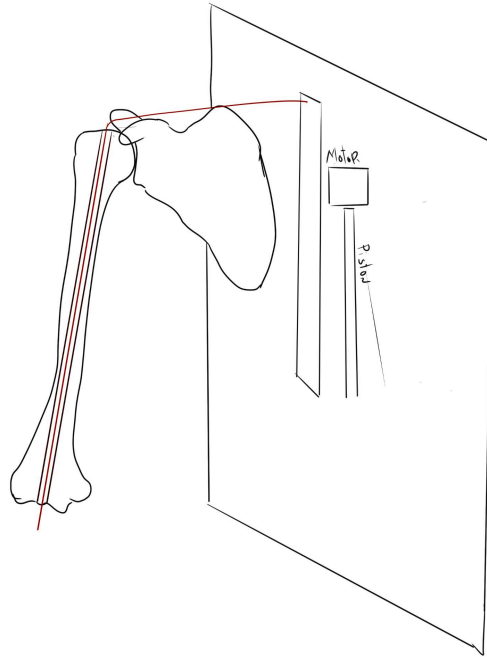


Figure 22: Channel Design Concept

The channel design allows for a much cleaner final model without the clutter of the previous team's approach in attaching motors, wires, and other materials to the exterior of the humerus and allows for the most visibility of the bones as they complete their motions. However, the channel design invites a number of complications including the question of force vector angles and friction of the internal wires as they travel through the bones and their connections.

3.2.2 Cage Design Concept

Our other preliminary design focused on creating a structure surrounding the bones to avoid the complications of the motor weights on the bones and suboptimal force vector angles. We referred to this structure as the cage. The bones of the ribcage and shoulder would be surrounded by a cage as shown in Figure 23 with the dimensions 0.5 meters x 0.8 meters x 0.8 meters, with the width of the cage being the shortest dimension of the cage.

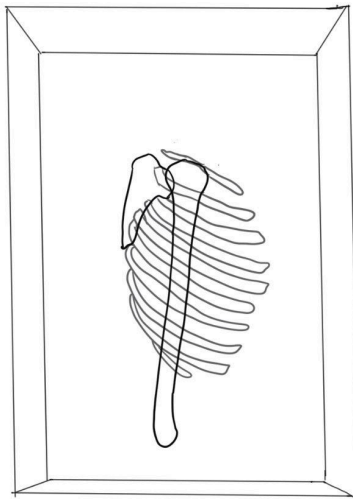


Figure 23: Model in the cage

Along the faces of the cage, motors would be placed and supported by beams with wire connections to the humerus and scapula to pull on the bones with adequate forces and angles to accurately replicate shoulder movement and scapulohumeral rhythm. The original placements of the motors were at the vertices of the cage where they would pull a final motor along the open face of the cage to guarantee the optimal angles for force vectors, however, this would restrict visibility and introduce difficulties in reinforcing the motor under its own force as well as simply being inefficient. Other placements were considered such as a moving track along the face of the cage, however, the final placements were decided to be constrained to one position and unmoving throughout the shoulder movements. These original motor placements and design concepts are shown below in figure 24.

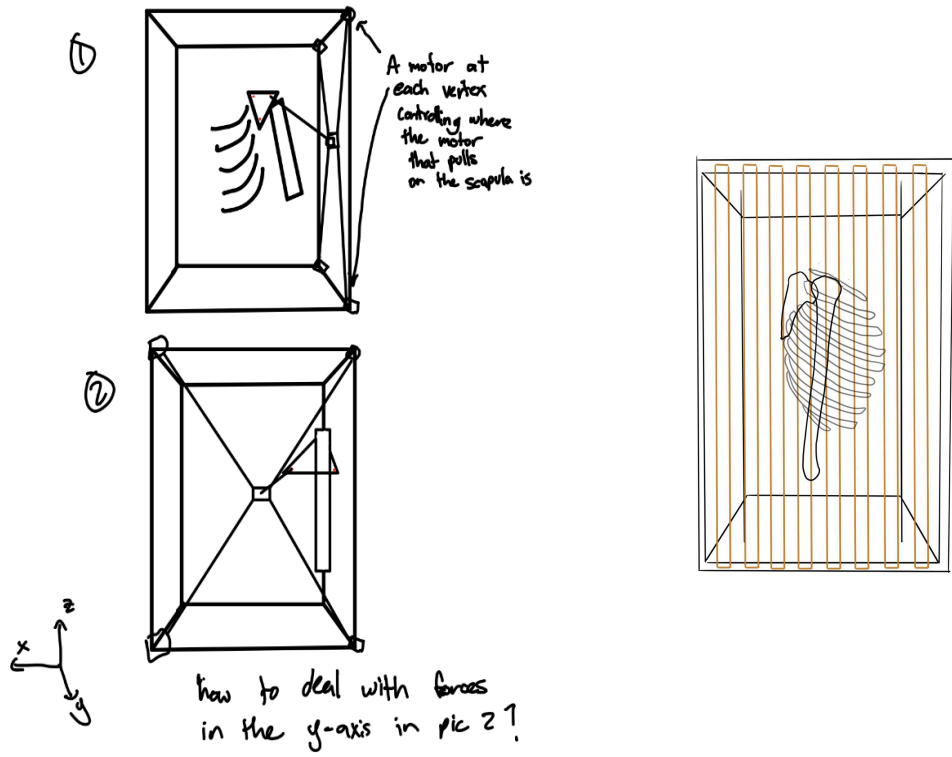


Figure 24: Vertice motor design (left) and track method design (right)

The exact placements of these motors are displayed in Figure 25 below. The materials utilized for the wires and the models of motors are discussed in sections 3.5.2 and 3.5.1 respectively. The motors were mounted to the cage through the use of 3D printed motor mounts left by the previous team. Additional mounts were printed using the same file the previous team used.

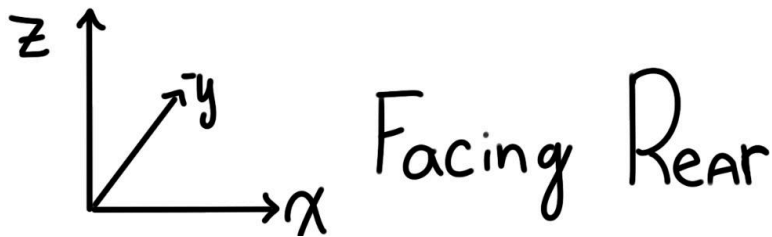
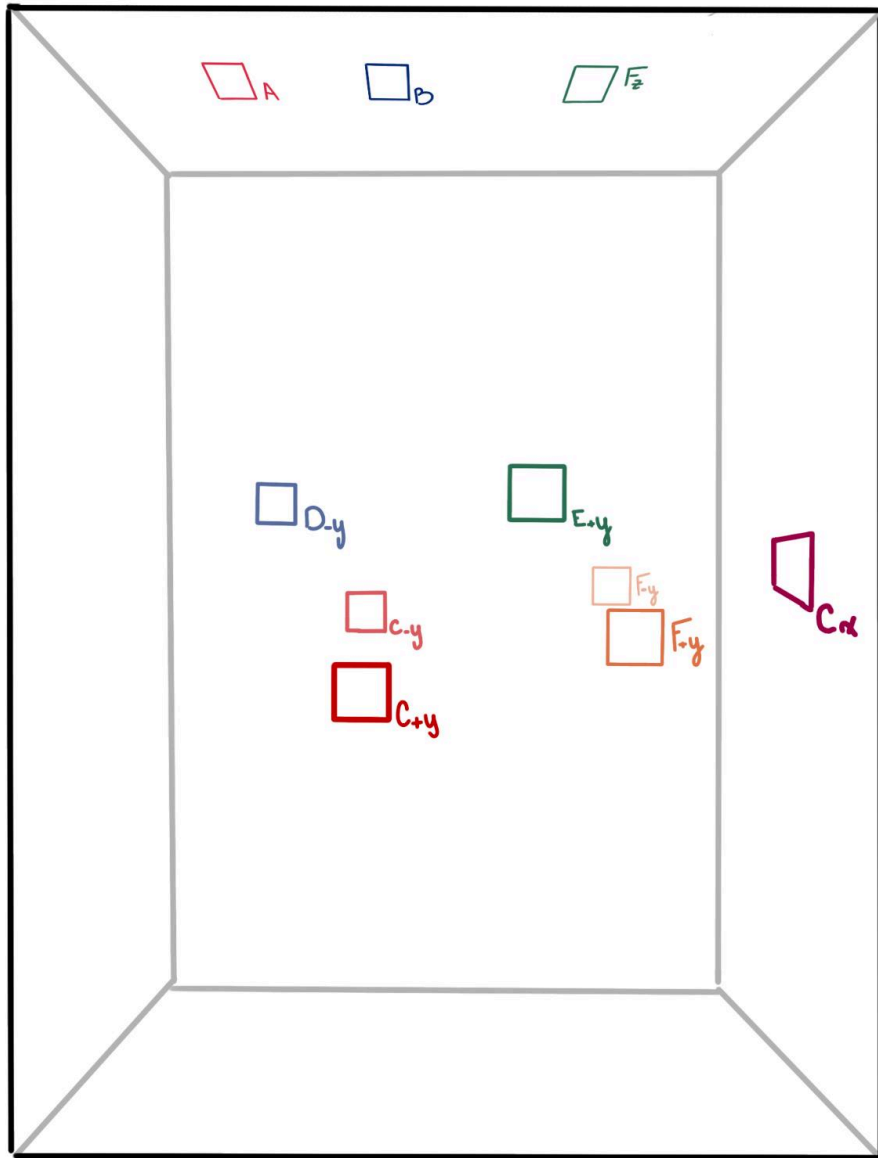


Figure 25: Motor placements along the faces of the cage

The primary benefits of the cage design were the visibility of the model and its movements it provided due to the lack of additional items cluttering up the humerus and scapula,

which additionally made it much more efficient to design methods to move the humerus and scapula since factors such as the weight of the motors did not have to be considered when focusing on the movement of the bones.

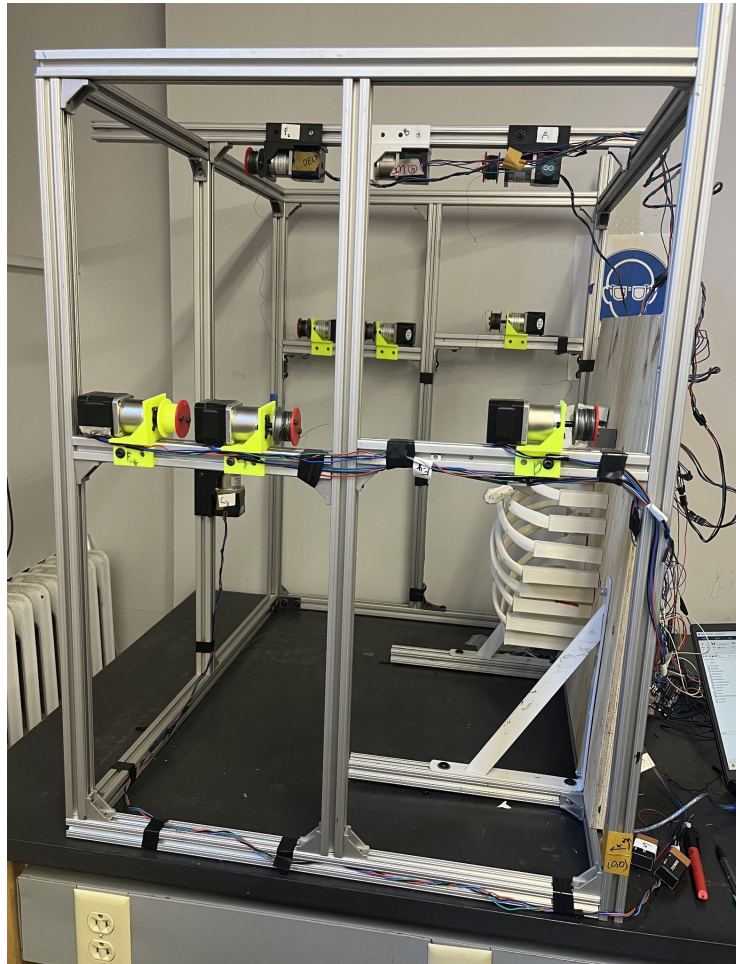


Figure 26: Constructed and Realized Cage

3.3 Scapular Rotation

Calculating how the scapula will rotate while the humerus abducts and flexes was vital to this project. The scapula's unorthodox shape and uneven distribution of mass caused the process to be complex, with the numerous directions of movement and constant uneven shifts of the scapula discussed in section 2.1 further complicating the process.

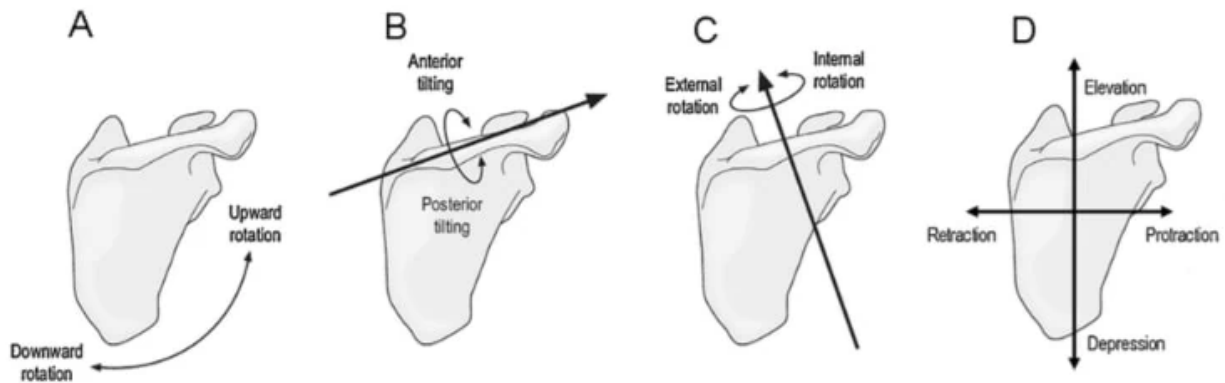


Figure 27: Potential movements of the Scapula (Physiotutors, 2023)

The position of the scapula was found by calculating where all five motor attachment points, A, B, C, D, and E, will be relative to the initial position of motor attachment point A. The attachment points are displayed below in figure 28. The amount of scapular rotation in each direction—upward rotation, anterior tilt, and external rotation—in 30° increments of humeral rotation were taken from tables 3 and 4. The team then assumed that rotation during each 30° increment was linear in its rotation, with the positions indicated on the scapula transitioning in a consistent fashion within the 30° periods.

Difference amount of change in scapula angle during shoulder abduction

Humeral abdction angle	Upward rotation angle (°) ^a			Anterior tilt angle (°) ^b			External rotation angle (°) ^c		
	Control	Thorax flexion	Thorax extention	Control	Thorax flexion	Thorax extention	Control	Thorax flexion	Thorax extention
0°–30°	3.39 ± 4.23	1.60 ± 3.23	2.05 ± 5.38	-6.04 ± 2.55	-4.95 ± 3.11	-5.55 ± 3.28	1.29 ± 1.65	0.93 ± 1.50	1.19 ± 1.72
30°–60°	26.34 ± 11.94	17.89 ± 8.98	22.38 ± 14.78	-22.28 ± 7.55	-24.13 ± 7.66	-19.31 ± 7.57	5.93 ± 2.90	6.45 ± 3.66	4.51 ± 3.63
60°–90°	41.25 ± 9.22	34.09 ± 9.32	35.20 ± 15.45	-31.45 ± 11.47	-39.25 ± 12.99 ^d	-26.47 ± 10.80	8.92 ± 4.52	8.92 ± 4.52 ^d	6.09 ± 5.15
90°–120°	50.85 ± 11.20	45.80 ± 10.60	42.58 ± 16.34	33.49 ± 16.02	-46.24 ± 17.61 ^d	-26.97 ± 14.55	10.71 ± 6.08	15.69 ± 4.95 ^d	6.46 ± 5.94

Table 3: Total rotation of the scapula in all three directions during 30° increments of abduction under “control” (Yabata, 2022)

Difference amount of change in scapula angle during shoulder flexion

Humeral flexion angle	Upward rotation angle (°) ^a			Anterior tilt angle (°) ^b			External rotation angle (°) ^c		
	Control	Thorax flexion	Thorax extention	Control	Thorax flexion	Thorax extention	Control	Thorax flexion	Thorax extention
0°–30°	1.55 ± 2.52	2.29 ± 2.55	0.83 ± 3.15	1.82 ± 2.38	1.91 ± 3.45	2.75 ± 2.68	-1.13 ± 1.52	-1.00 ± 1.76	-1.38 ± 1.07
30°–60°	9.14 ± 5.03	9.14 ± 5.33	7.91 ± 6.98	0.08 ± 6.01	0.09 ± 8.65	1.01 ± 6.38	-1.93 ± 1.76	-1.75 ± -3.09	-2.89 ± 2.97
60°–90°	15.03 ± 5.60	14.50 ± 5.62	14.85 ± 8.01	-3.80 ± 9.15	-4.65 ± 12.99	-2.71 ± 9.61	-1.95 ± 3.69	-1.95 ± 3.69	-3.71 ± 4.27
90°–120°	26.35 ± 7.02	24.84 ± 5.99	23.09 ± 8.62	-11.16 ± 13.45	-14.99 ± 16.86	-6.74 ± 13.52	0.22 ± 4.49	3.61 ± 5.64 ^d	-3.47 ± 5.88

Table 4: Total rotation of the scapula in all three directions during 30° increments of flexion under “control” (Yabata, 2022)

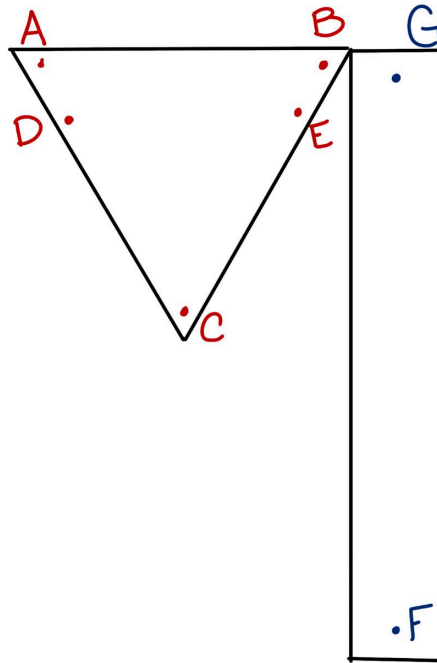


Figure 28: A simplified view of each of the motor attachment points

The team then defined two axes of rotation, one for upward rotation and one for anterior tilt, IJ and IK respectively. These axes of rotation were formed from the vector between two points on the scapula as displayed in figure 29. External rotation of the scapula is centered around a point called the instantaneous center of rotation, or the ICR.

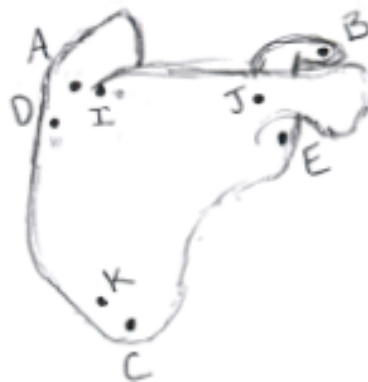


Figure 29: Key Points of Mass Distribution within the Scapula

The team then applied the Rodrigues' Rotation Formula, a formula for rotating a vector around a normal vector being used as an axis of rotation, for each direction of rotation in increments of 0.1° of humeral abduction or flexion up to 120°, and averaged the three outputs to find the new position of each motor attachment point. This strategy was also applied to points I, J, and K, so that the axes of rotation stayed within the scapula. An example of the Rodrigues' Rotation Formula is shown below. In this case, vector v is being rotated around the normal vector n by theta degrees to create vector v prime. The equation is the form of the Rodrigues' Rotation Formula the team used in their math.

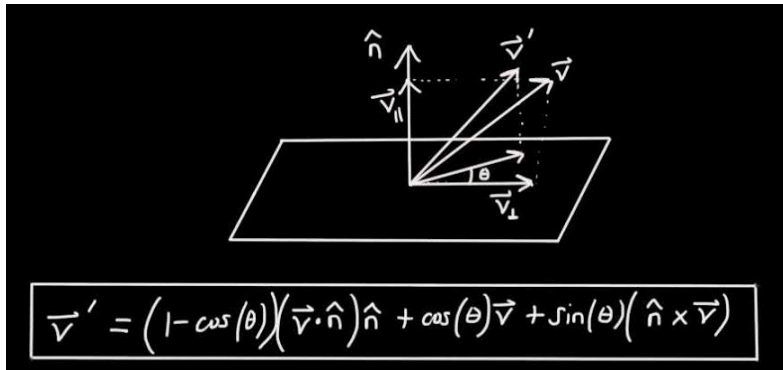


Figure 30: An example of the Rodrigues' Rotation Formula (YouTube channel Mathoma)

3.4 Humeral Abduction

Scapulohumeral rhythm was modeled for both humeral abduction and flexion. Humeral movement was confined to a two dimensional plane in its movements while it is moving in each direction, with additional safeguards in attached motors ensuring the humerus does not stray from its path of movement. The force required to lift the humerus was calculated through trigonometry utilizing a number of variables displayed in the nomenclature table below.

Variable	Definition (unit)
L_H	Length of the humerus (meters)
W_H	Mass of the humerus (kilograms)
α_i	Initial angle between the humerus and the vertical axis (°)
Θ_i	Initial angle between the humerus and the thread (°)

Θ'	Angle between the humerus and the thread post humeral abduction ($^{\circ}$)
L_{Ti}	Initial thread length (meters)
L_T'	Thread length following humeral abduction (meters)
$\Delta\alpha$	Desired change in angle alpha ($^{\circ}$)
t	Time (seconds)
L_{HM}	Distance between the top of the humerus and the motor (meters)
β_i	Initial angle between the motor wire and the humerus ($^{\circ}$)
β'	Angle β after abduction of the humerus ($^{\circ}$)
d_{Hbot}	Distance traveled by the bottom of the humerus (meters)
v_{Hbot}	Velocity of the bottom of the humerus (meters/second)
a_{Hbot}	Acceleration of the bottom of the humerus (meters/second ²)
F_{gopp}	The force of gravity opposite to the direction of movement (Newtons)
F_{Net}	Net force acting on the humerus (Newtons)
$F_{Required}$	Required force to lift the humerus (Newtons)

Table 5: Nomenclature Table for Humeral Abduction

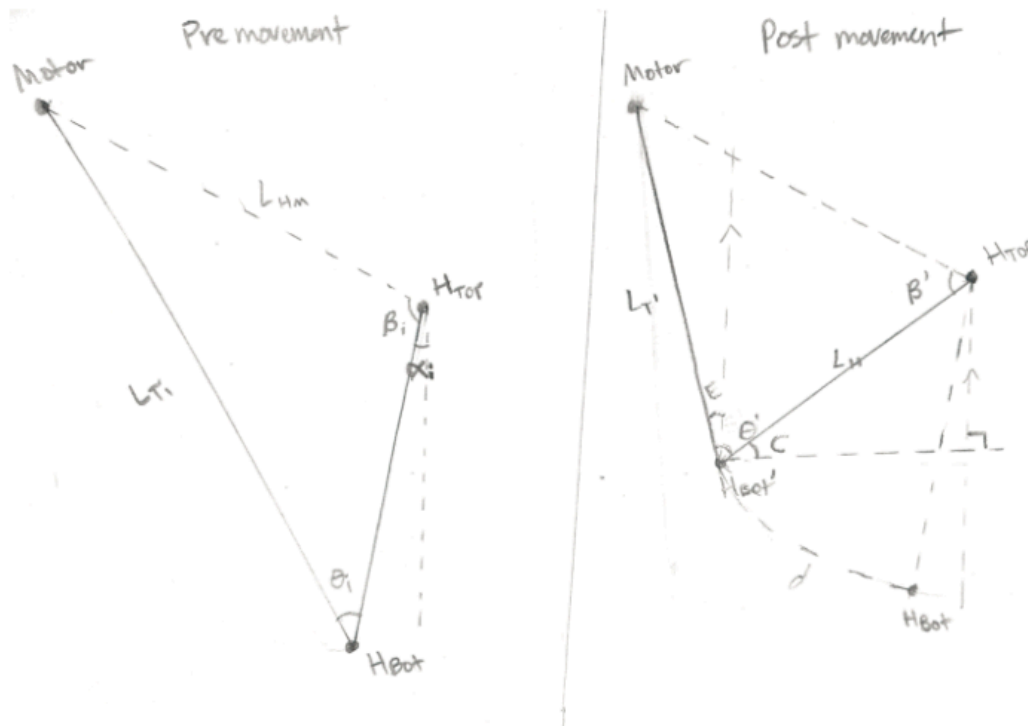


Figure 31: All Angles and Lengths during Humeral Abduction

The steps to solve for the force necessary to lift the humerus and the ideal position of the motor are displayed below in table 6.

Step Description	Equation
Beginning with the length of the humerus, the value for L_{HM} can be found using the law of cosines:	$L_{HM} = \sqrt{(L_H^2 + L_{Ti}^2 - 2L_H L_{Ti} \cos \Theta_i)}$
Using other given variables, L_{Ti} , L_H , and Θ_i the team can similarly solve for β_i	$(\sin \beta_i) / L_{Ti} = (\sin \Theta_i) / L_H$
With the initial value for the angle found, the team can then find the angle after the abduction of the humerus, β' :	$\beta' = \beta_i - \Delta \alpha$
With these variables defined, the desired thread length following humeral abduction can be found:	$L_T' = \sqrt{(L_H^2 + L_{HM}^2 - 2L_H L_{HM} \cos \beta')}$

With this final thread length determined, other values can be solved to determine the other kinematics needed to solve for the force required to lift the humerus.	$\Theta' = \sin^{-1}(L_{HM}\sin\beta'/L_T')$
With the new angle found, the team can then solve for the distance, velocity, and acceleration of the humerus.	$d_{Hbot} = \Delta\alpha\pi L_H/180$ $v_{Hbot} = d_{Hbot}/t$ $v_c = 2v_{Hbot}$ $a_{Hbot} = v_c/t$
New angles, E and C, must first be defined to relate F_g and solve for the force:	$C = 90 - (\alpha_i + \Delta\alpha)$ $E = (\Theta' + C) - 90$
Now with all values known, the force can be solved for using Newton's Second Law:	$F_g = 9.8W_H$ $F_{gopp} = F_g \cos E$ $F_{net} = W_H a_{Hbot}$ $F_{required} = F_{net} + F_{gopp}$

Table 6: Solving for the Necessary Force and the Position of the Motor

To track the position of the humerus, the team calculated where motor attachment point F will be relative to the initial position of motor attachment point A. This was done by setting the center of rotation at motor attachment point B and applying the Rodrigues' Rotation Formula and calculating the positions of motor attachment point F in increments of 0.1° of abduction and flexion up to 120° . In order to account for the movement of point B during this rotation, the team used geometry to "drag" the attachment point to its proper final position.

Givens:

All values are in meters and degrees. All distances are measured from the origin which is set at the bottom left corner of the cage as seen in figure 40.

Initial Wire Attachment Points:

$$A = [0.073; 0.507; 0.445];$$

$$B = [0.203; 0.509; 0.458];$$

Initial Axes Points:

$$I = [0.074; 0.508; 0.434];$$

$$J = [0.2; 0.508; 0.434];$$

Motor Placement:

$$\text{motorA} = [-0.045; .534; 0.825];$$

$$\text{motorB} = [0.18; 0.534; 0.825];$$

$C = [0.083; 0.525; 0.312];$ $K = [0.074; 0.508; 0.313];$ $motorCPosY = [0.44; 0.852; 0.54];$
 $D = [0.154; 0.522; 0.383];$ $motorD = [0.185; 0; 0.5];$
 $E = [0.077; 0.524; 0.388];$ $motorE = [0.19; 0.852; 0.366];$
 $F = [0.11; 0.035; -0.3696];$ $motorFZ = [0.405; 0.534; 0.825];$
 $motorFPosY = [0.57; 0.852; 0.54];$
 $motorFNegY = [0.505; 0; 0.48];$

The variation in angle of the bones was based on a study (Yabata, 2022), where the angles are measured in cartesian coordinates relative to an origin.

Angle of Abduction	Total Upward Rotation	Total Anterior Tilt	Total External Rotation
0-30°	-3.39°	6.04°	1.29°
30-60°	-22.95°	16.24°	4.46°
60-90°	-14.91°	9.17°	2.99°
90-120°	-9.60°	2.04°	1.79°
Angle of Flexion			
0-30°	-1.55°	-1.82°	-1.13°
30-60°	-7.59°	1.74°	0.80°
60-90°	-5.89°	3.88°	-0.02°
90-120°	-11.32°	7.36°	2.17°

Table 7: Rotation of the Humerus during Abduction and Flexion (Yabata, 2022)

Calculations:

1. How to rotate the scapula. The example provided will be point E moving as the humerus abducts from 0° to 10°. Each step calculated by the code is 0.1°; the 10° increment is used for illustrative purposes.
 - 1.1. Find how much E externally rotates during this interval using the table and step size.
 - 1.1.1. $1.29° / (30/10) = 0.43°$

1.2. Find the normal axis of rotation, \widehat{IK} in this case

1.2.1. Move the origin to I

$$1.2.2. \quad I = [0.074; 0.508; 0.434] - [0.074; 0.508; 0.434] = [0; 0; 0]$$

$$K = [0.074; 0.508; 0.313] - [0.074; 0.508; 0.434] = [0; 0; -0.121]$$

$$E = [0.077; 0.524; 0.388] - [0.074; 0.508; 0.434] = [0.003; 0.016; -0.046]$$

1.2.3. Find \overline{IK}

$$1.2.3.1. \quad \overline{IK} = [0; 0; -0.121] - [0; 0; 0] = [0; 0; -0.121]$$

1.2.4. Find \widehat{IK}

$$1.2.4.1. \quad |\overline{IK}| = \sqrt{0^2 + 0^2 + (-0.121)^2} = 0.121$$

$$\widehat{IK} = [0; 0; -0.121] / 0.121 = [0; 0; -1]$$

1.3. Derive the Rodrigues Rotation Formula: a formula for rotating a point a desired number of degrees around any normal axis

1.3.1. $\vec{E}_{parallel} = \text{component of } \vec{E} \text{ that is parallel to } \widehat{IK}$

$\vec{E}_{perpendicular} = \text{component of } \vec{E} \text{ that is perpendicular to } \widehat{IK}$

$$\vec{E} = \vec{E}_{parallel} + \vec{E}_{perpendicular}$$

1.3.2. $\vec{E}'_{parallel} = \vec{E}_{parallel}$

$$1.3.2.1. \quad \vec{E}' = \vec{E}_{parallel} + \vec{E}'_{perpendicular}$$

1.3.3. $\Theta = \text{angle from 1.1}$

$$1.3.3.1. \quad \vec{E}' = \vec{E}_{parallel} + \cos\Theta * \vec{E}_{perpendicular} + \sin\Theta * (\widehat{IK} \times \vec{E})$$

$$1.3.3.2. \quad \vec{E}' = (1 - \cos\Theta) * \vec{E}_{perpendicular} + \cos\Theta * \vec{E} + \sin\Theta * (\widehat{IK} \times \vec{E})$$

1.3.4. Final Rodrigues Rotation Formula

$$1.3.4.1. \quad \vec{E}' = (1 - \cos\Theta) * (\vec{E} \cdot \widehat{IK}) * \widehat{IK} + \cos\Theta * \vec{E} + \sin\Theta * (\widehat{IK} \times \vec{E})$$

1.4. Using the Rodrigues Rotation Formula

1.4.1. $\vec{E}' = (1 - \cos(0.43)) * ([0.003; 0.016; -0.046] \cdot [0; 0; -1]) * [0; 0; -1] + \cos(0.43) * [0.003; 0.016; -0.046] + \sin(0.43) * ([0; 0; -1] \times [0.003; 0.016; -0.046])$
 $\vec{E}' = [0.00288; 0.01602; -0.046]$

1.5. Move the origin back

1.5.1. $\vec{E}'_{IK} = [0.00288; 0.01602; -0.046] + [0.074; 0.508; 0.434] = [0.07688; 0.52402; 0.388]$

1.6. Repeat steps 1.1, 1.2, and 1.4 with the axes as IJ and the axis through the ICR orthogonal to the plane containing I, J, and K, making sure that the origin is moved to the correct point, I for IJ and the ICR.

1.6.1. $\vec{E}'_{IJ} = [0.077; 0.52238; 0.38747]$
 $\vec{E}'_{ICR} = [0.07836; 0.524; 0.38929]$

1.7. Average the three E values

1.7.1. $\vec{E}' = [0.07741; 0.52347; 0.38825]$

1.8. Repeat 1.1 - 1.7 for points A, B, C, D, I, J, K, and the ICR

1.9. Repeat 1.1 - 1.8 until total abduction angle is 120° while always using the most recent I, J, K and ICR values

1.10. Repeat 1.1 - 1.9 to find all points for flexion

2. How to find how point F rotates. The example used will also be the humerus abducting from 0° to 10°.

2.1. Move the origin to B, as this is where the humerus is rotating around

2.1.1. $B = [0.203; 0.509; 0.458] - [0.203; 0.509; 0.458] = [0; 0; 0]$
 $F = [0.21; 0.515; 0.13] - [0.203; 0.509; 0.458] = [0.007; 0.006; -0.328]$

2.2. Set the axis of rotation for abduction

2.2.1. $\hat{n} = [0; -1; 0]$

2.3. Use the Rodrigues Rotation Formula

$$2.3.1. \quad \vec{F}' = (1 - \cos(10)) * ([0.007; 0.006; -0.328] \cdot [0; -1; 0]) * [0; -1; 0] + \cos(10) * [0.007; 0.006; -0.328] + \sin(10) * ([0; -1; 0] \times [0.007; 0.006; -0.328]) = [-0.05001; 0.006; -0.32423]$$

2.4. Move origin back

$$2.4.1. \quad \vec{F}' = [-0.05001; 0.006; -0.32423] + [0.203; 0.509; 0.458] = [0.15299; 0.515; 0.13377]$$

2.5. Now the team must account for the movement of the humeral head in the XZ plane

$$2.5.1. \quad B' - B = [0.2029; 0.509; 0.4589] - [0.203; 0.509; 0.458] = [-0.0001; 0; 0.0009]$$

$$2.5.2. \quad F' - (B' - B) = [0.15299; 0.515; 0.13377] - [-0.0001; 0; 0.0009] = [0.15309; 0.515; 0.13287]$$

2.6. Now the team must account for the movement of the humeral head along the y-axis while keeping F in the same XZ plane.

2.6.1. Create a circle, in the same XZ plane as F, of all possible locations of F with the knowns of the length of the humerus and the location of the humeral head at B'

$$2.6.1.1. \quad \text{Center of Circle} = [X_{B'}; 0.515; Z_{B'}] = [0.2029; 0.515; 0.4589]$$

$$2.6.1.2. \quad \text{Radius of Circle} = \sqrt{\text{Length}_{\text{Humerus}}^2 - (Y_{B'} - 0.515)^2} = \sqrt{0.3683^2 - (0.509 - 0.515)^2} = 0.13561$$

2.6.2. Create a vector from the center of the circle to the current position of F and normalize it

$$2.6.2.1. \quad \vec{R} = [0.2029; 0.515; 0.4589] - [0.15309; 0.515; 0.13287] = [0.04981; 0; 0.32603]$$

$$2.6.2.2. \quad |\vec{R}| = [0.04981; 0; 0.32603] / 0.32894 = [0.15173; 0; 0.98842]$$

2.6.3. Find the closest point on the circle to the current position of F. This point on the circle is F'

$$2.6.3.1. \quad F' = [0.15309; 0.515; 0.13287] + 0.3683 * [0.15173; 0; 0.98842] = [0.20897; 0.515; 0.49691]$$

- 2.7. Repeat 2.1 - 2.6, using the correct B and B', until the total abduction angle is 120°
- 2.8. Repeat 2.1 - 2.7, using [1; 0; 0] as the axis of rotation, to find the values of F for flexion

3.5 Material Selection

3.5.1 Motor Selection

The motors used by the 2021-2022 and 2022-2023 teams were the Nema 17 Stepper Motor model number 17HS19-1684S-PG27, which will be shortened to the 17HS19 model for the duration of the report. The 17HS19 model has a number of specifications that allows for efficiency, however, our team had concerns in utilizing these motors due to the amperage requirements of 1.2 Amps. To circumvent this issue, our team looked for other models of Nema 17 motors and decided on the use of the 17HS13-0404S-PG27 motor, which will similarly be shortened to the 17HS13 model. The qualities that make the 17HS13 motor the ideal are the rated current and the maximum permissible torque. The specifications for the 17HS13 motor are given in figure 32 below.

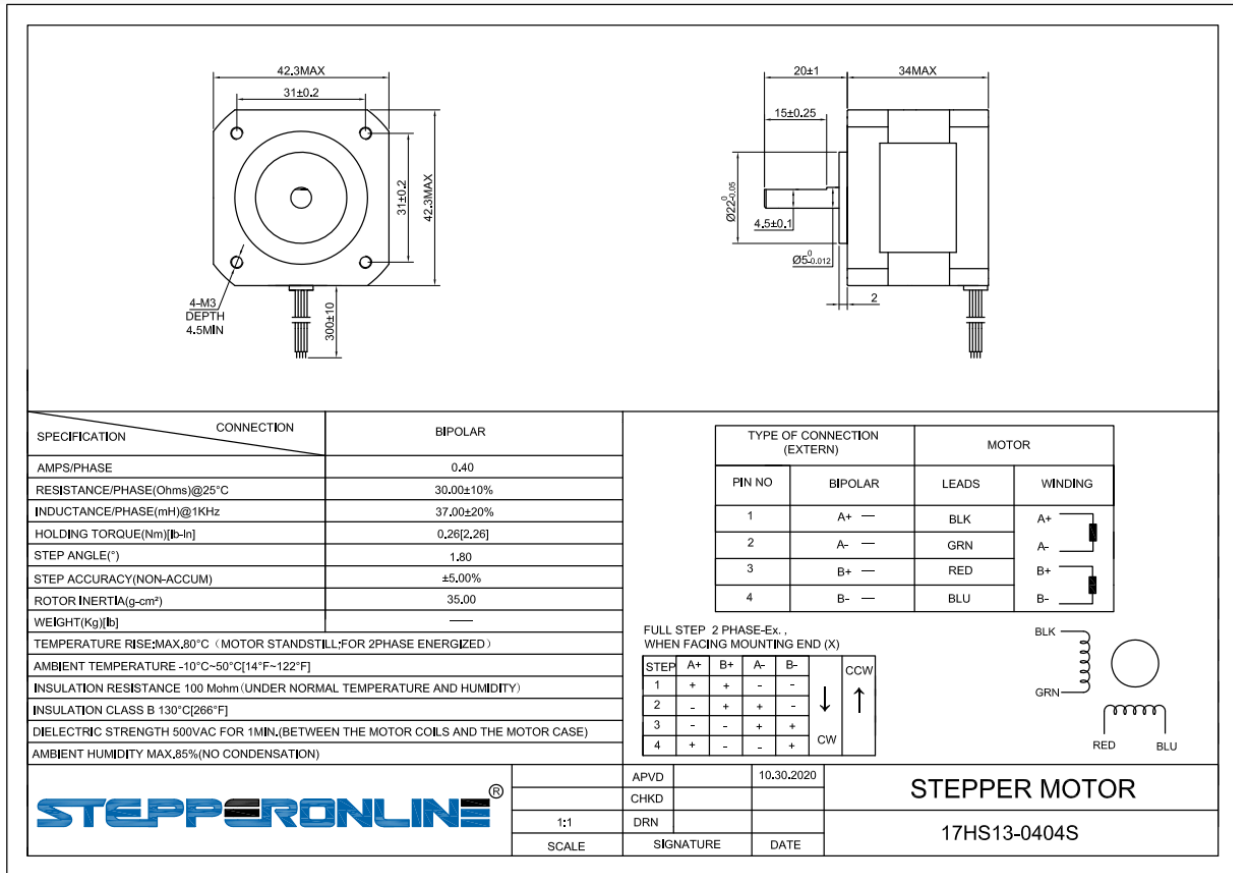


Figure 32: The model 17HS13-0404S-PG27 data sheet (StepperOnline, 2020)

The low rated current of 0.4 amps allows the motor to function on low currents, meaning the circuit will need to involve fewer pieces and draw less current and power into the system, exerting a lower strain on the equipment. The required voltage input for the motors was 12V. The max permissible torque of 3 Newton meters for each motor is capable of pulling on the humerus and scapula with adequate force to induce the rotation and transitions necessary to replicate scapulohumeral rhythm in the shoulder. The two previous teams both used five of the model 17HS19 motors to pull the humerus along their trail of wire that led along the length of the humerus.

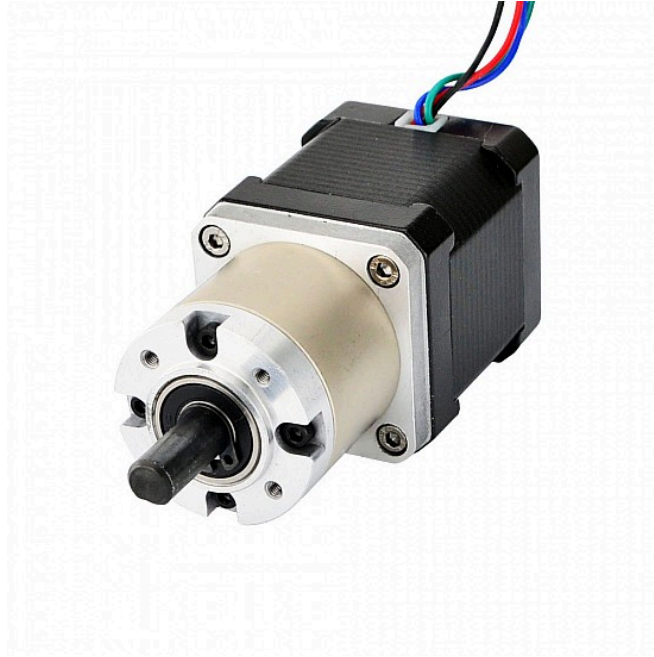


Figure 33: The NEMA model 17HS19-1684S-PG27 motor (StepperOnline, 2020)

For our rig design, discussed in section 3.2, ten model 17HS13 motors were implemented to ensure correct positioning and stability of the humerus and scapula during humeral abduction. We attached the motors to the cage using 3D printed mounts. The locations of the motor placement within the cage are similarly discussed in section 3.2.



Figure 34: The NEMA model 17HS13-0404S-PG27 motor (StepperOnline, 2020)

3.5.2 Connecting Wires

Utilizing the correct materials for each material that the team is trying to simulate is crucial to the project's success. The first team developed a shoulder model with the bones properly assembled. For the material of the bones, they used PLA due to its rigid properties and ease of molding through 3D printing into the desired shapes. Our team will be similarly utilizing PLA for this aspect of the model.

The first team utilized nylon wires as a way of moving the bones to their desired location due to their strength and flexibility, whilst still remaining cost-effective. However, this team did not account for the issue of creep. The deformation caused by the creep changes the length of the nylon wires and thus changes the calculations that must be done to pull on the bones with the right force vectors. The second team utilized rubber threads to better operate under creep conditions, however, the friction caused between the rubber threads and other components of the rig hampered movements. To eliminate these issues, our team decided to change the material used for the connecting wires.

Several options for the connective wires were discussed including a number of polymers and metals as well as the previously utilized nylon 6 wires, however, each material encountered different issues. The nylon 6 wires, as discussed above, were susceptible to creep. Silver alloys were too soft and could easily be damaged. Copper alloys would be susceptible to environmental factors. Finally, various steels were similarly proposed but were too resistant to bending, far too expensive, and had high friction coefficients, making their movements in the model more difficult than necessary. With this in mind, our team considered PTFE coated wires to mitigate friction between the wire and any surfaces contacted, however, a suitable product was not commercially available.

Ultimately, the team utilized braided nylon fishing line to achieve a balance between all sought characteristics. With the values attained, the wire would need to be capable of supporting a maximum of 13.8 MPa without experiencing creep, whilst still being capable of repeatedly bending in the process of pulling the shoulder model into position and not inhibiting the movement of the humerus and scapula all of which braided fishing line achieves.



Figure 36: Braided Fishing Line

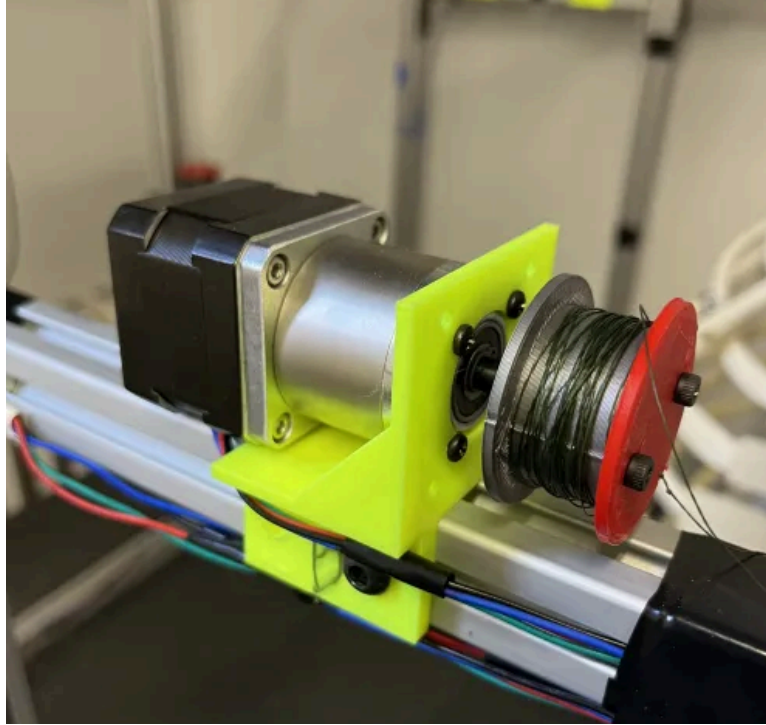


Figure 37: Braided Fishing Line attached to a 17HS13 motor

3.5.3 Motor Driver

We used a stepper motor driver in order to control the motors. The brand name for the driver is ‘Allegro’s A4988 DMOS Microstepping Driver with Translator and Overcurrent Protection’. We bought our driver from Amazon which was manufactured by Shenzhenshi Yongfukang Technology Co. The A4988 has 16 pins of which our team utilized 10 pins. The Vmot and GND are connected to a 9V battery. The 2B, 2A, 1A, and 1B pins are connected to the four motor wires. Figure 39 below shows the corresponding colors to letters. The wiring of the motor to the driver can be arranged in a multitude of variations as long as the one coil on the motor is not connected to two different coil outputs on the driver.

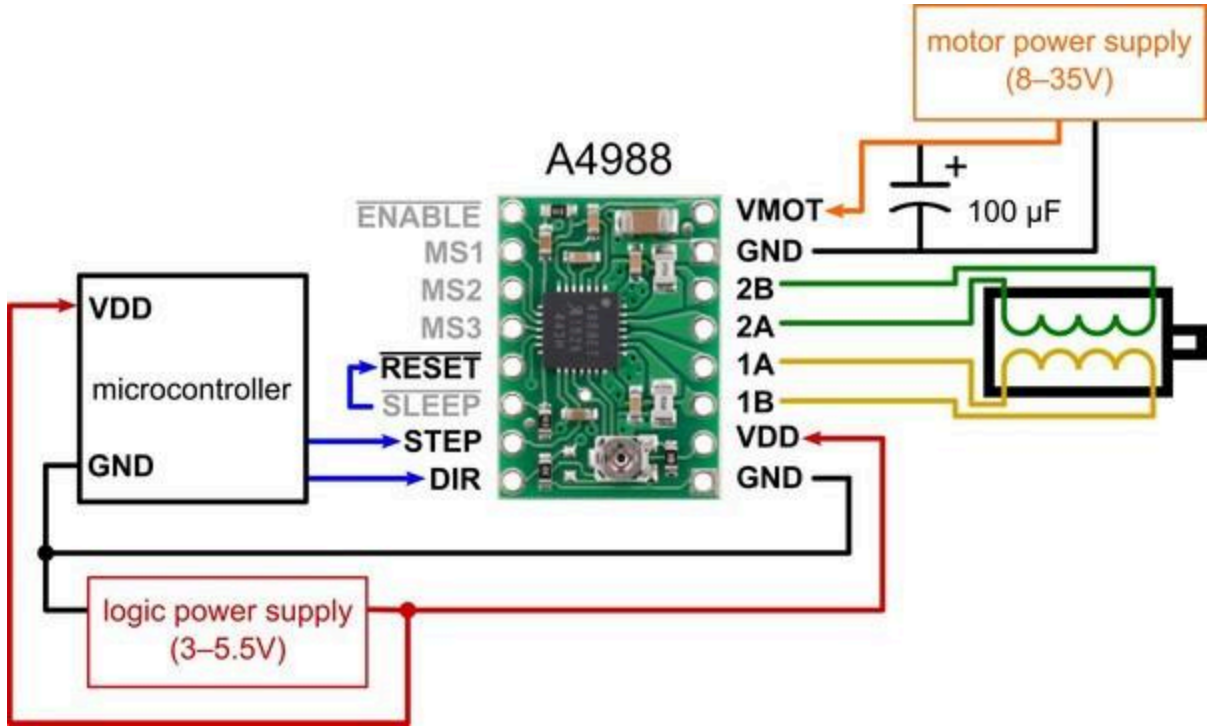


Figure 38: The figure of the driver (Pololu, 2024)

A4988	Motor Datasheet	Color
1A	A+	Green
1B	A-	Black
2A	B+	Red
2B	B-	Blue

Table 8: The chosen orientation of the wires from the motor to the driver

In order to set up the motor driver we needed to adjust the current limit potentiometer. The following equation is used to find the voltage reference for the driver.

$$V_{\text{ref}} = 8 * I_{\text{max}} * R_{\text{cs}}$$

The I_{max} is the max current rated for the motors we were using which is 0.4A. R_{cs} is the current sense resistance of the driver motor, $R_{\text{cs}} = 0.1 \Omega$. Therefore, our V_{ref} would be 0.32V. The figure below shows one of the ways to adjust the current limit potentiometer. For the V Ω port we used an alligator clip that was connected to a screwdriver that we turned the potentiometer with.

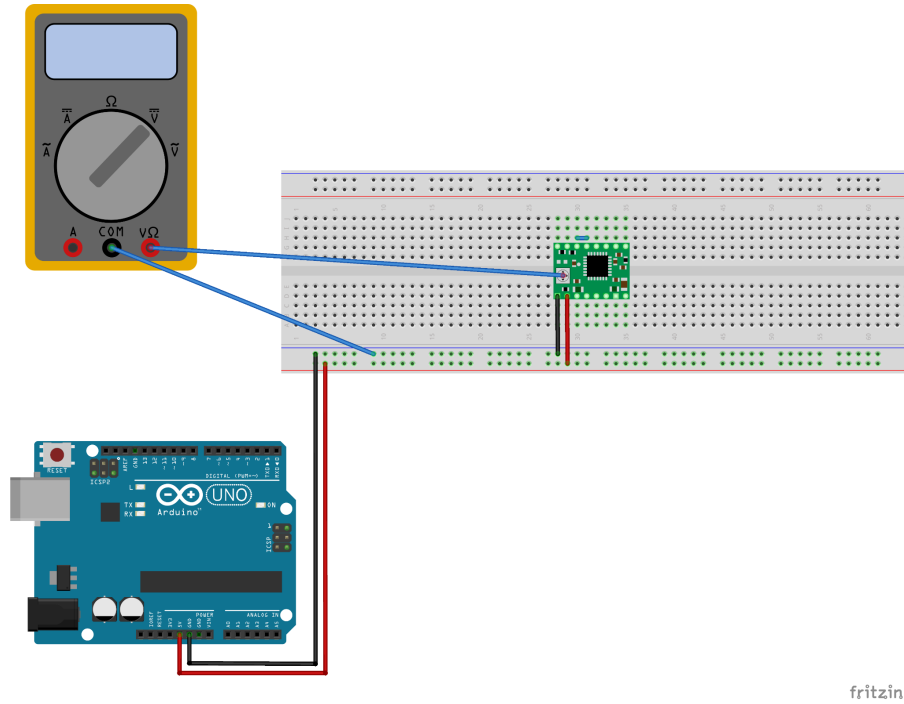


Figure 39: How to adjust current limit potentiometer

Another important note about the A4988 motor driver is the temperatures it can operate at. The maximum junction temperature is 150°C, attaching the heat sink to the motor driver aids to lower the temperature but the drivers can still cause burns with direct contact at operational temperatures.

3.6 Cage Construction and Implementing a Matlab Code

3.6.1 The Cage

The cage surrounding the rig was constructed utilizing aluminum extrusion rods present available in the WPI MQP labs. The exact dimensions of the rods vary and are listed in table 9 below.

Part No.	Aluminum Extrusion Rod Dimensions (Length X Width X Depth)	Quantity
1010 T-Slotted Profile - Four Open T-Slots	0.912m X 1.00" X 1.00"	2

1010 T-Slotted Profile - Four Open T-Slots	2.44m X 1.00" X 1.00"	2
20-2020 T-Slotted Profile - Four Open T-Slots	0.695m X 20mm X 20mm	2
1003-s Smooth Surface T-Slotted Profile - Three Adjacent Open T-Slots	2.44m X 1.00" X 1.00"	1

Table 9: Details of Aluminum Extrusion Rods

The minimum dimension of the cage is 0.5 meters by 0.8 meters by 0.8 meters. Different views of the cage are displayed below in figures 39 through 43. The varying dimensions displayed in the figures are from the different sizes of aluminum extrusion available to the team.

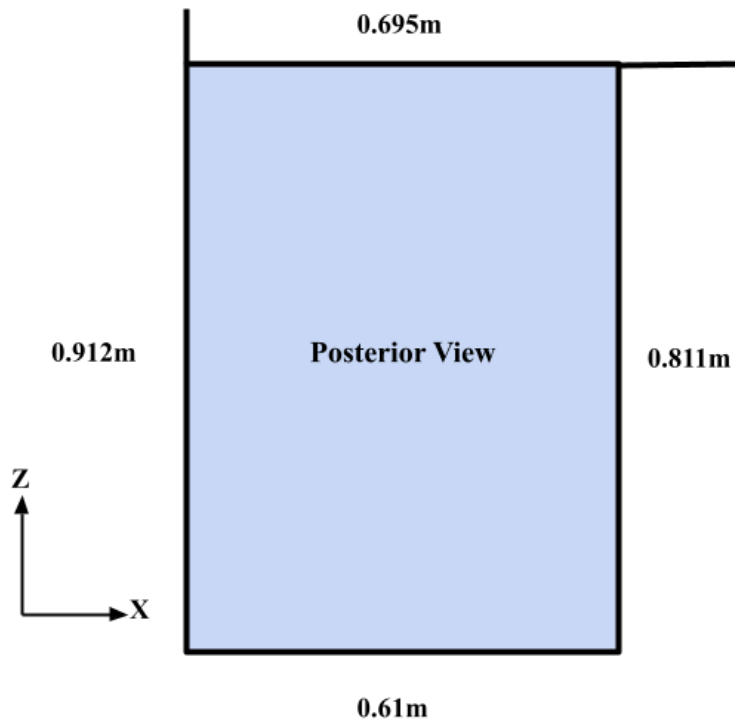


Figure 40: Posterior View of the Cage

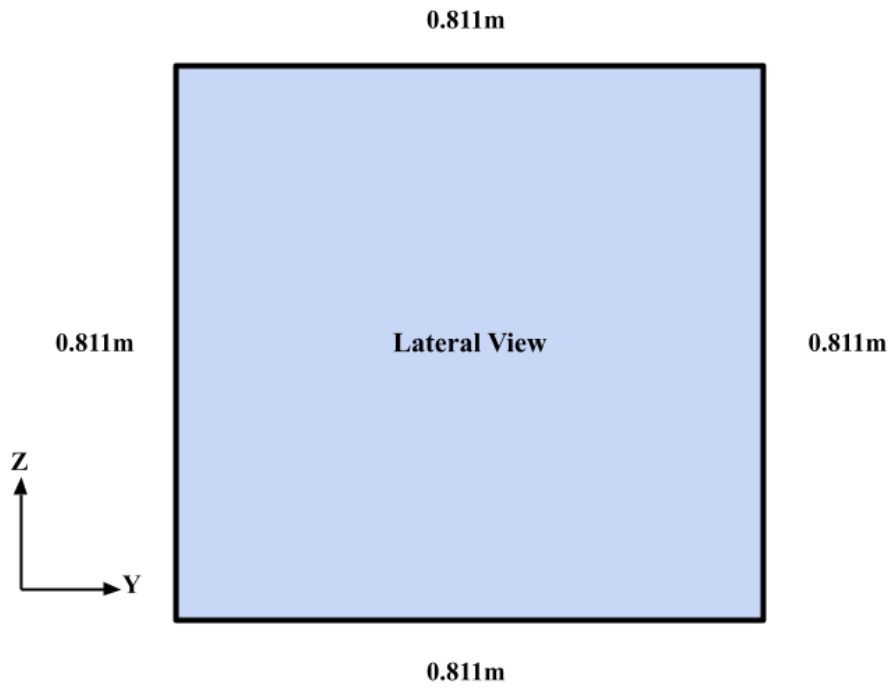


Figure 41: Lateral View of the Cage

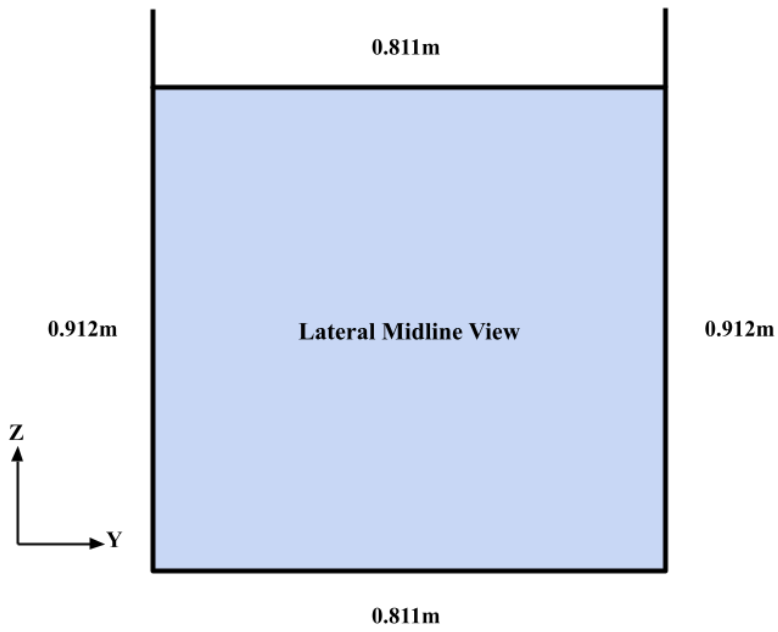


Figure 42: Lateral Midline View of the Cage

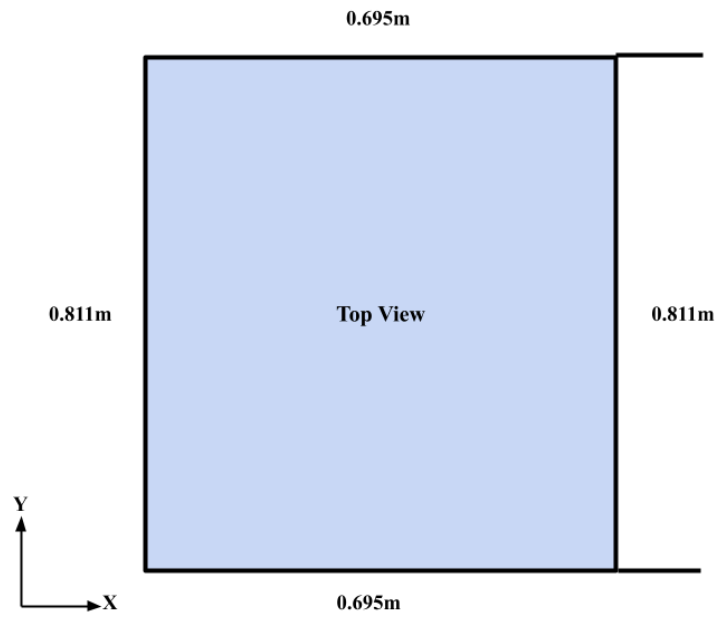


Figure 43: Top View of the Cage

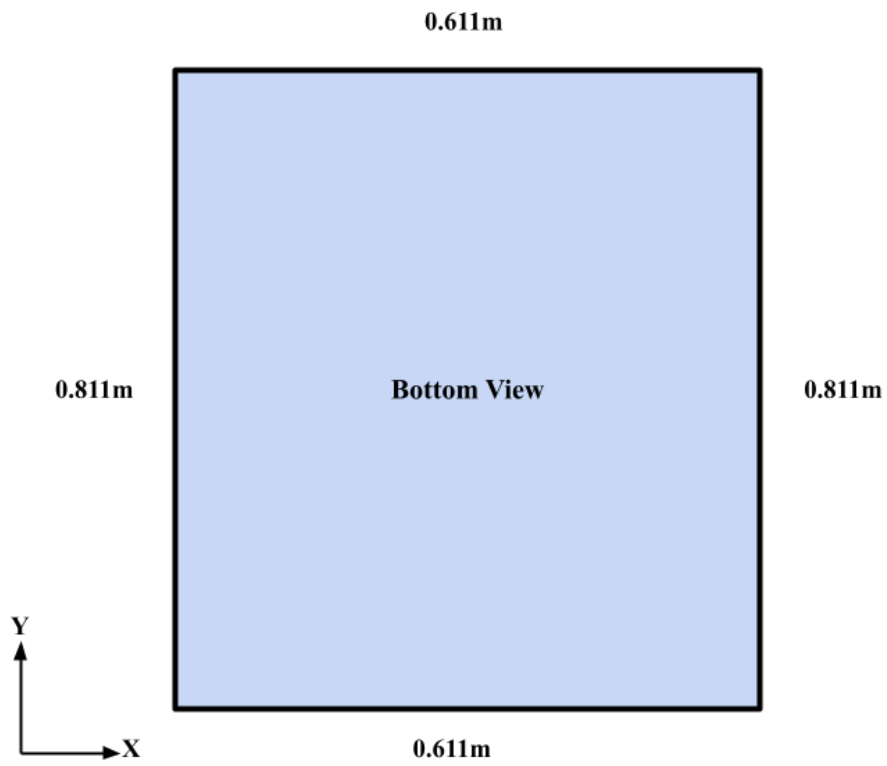


Figure 44: Bottom View of the Cage

Another issue we saw that was due to aging was wood rot in the original rib cage mount. We replaced the old plywood with a $\frac{3}{4}$ inch plywood. Additional bars were installed to further support the cage under the weight of the rig and correctly position the motors in accordance with Figure 25 in section 3.2.1 to pull on the 3D printed bones within. To minimize any clutter and ensure visibility of the rig, the wires for each motor run along the bars of the cage where they conjoin in the circuit on the backside of the board.

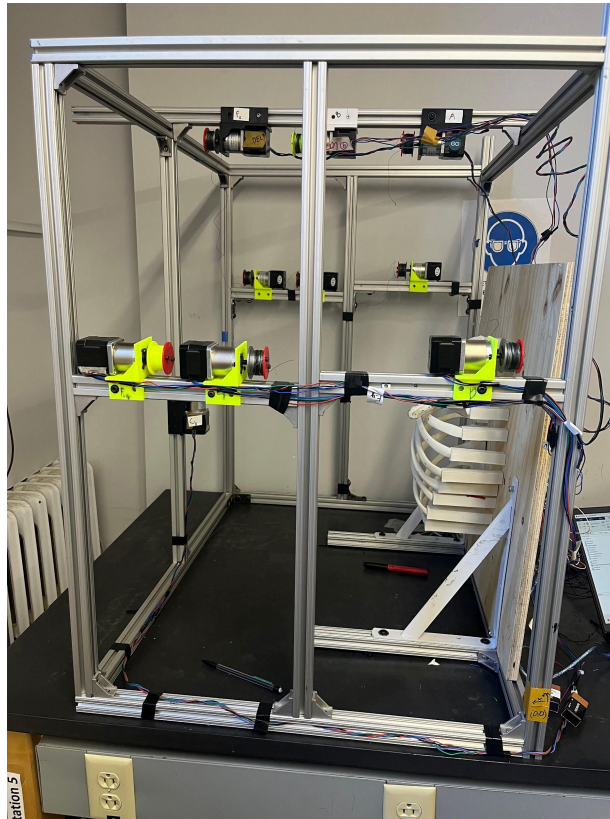


Figure 45: Supporting Bars of the Cage

3.6.2 Coding and the MATLAB Model

The team lead for this portion of the project was Cameron Leffler, who wrote MATLAB code to calculate the positions of each of the six wire attachment points on the scapula and humerus relative to the origin for every 0.1° of arm abduction and flexion. The following documentation explains how the code calculates all of the relative positions of the wire attachment points and wire lengths.

The Code is split into four scripts of code; Setup, Abduction, Flexion, and App code scripts, all of which are run using Arduinos connected in the circuit. The setup code defines the

relative positions of the motors and of the motor attachment points for all possible angles of arm abduction and flexion.

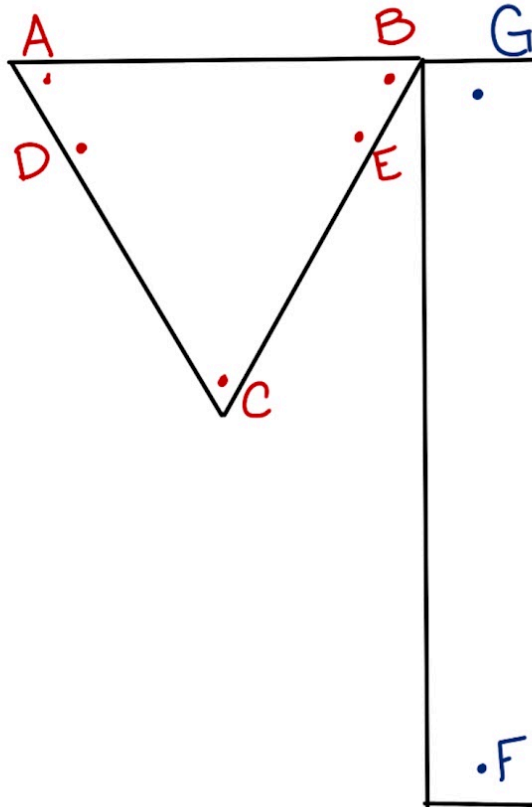


Figure 46: A simplified view of each of the motor attachment points

It does this in the manner stated in section 3.2 using the Rodrigues' Rotation Formula. It then calculates the distance from each motor to the motor attachment point, giving the length of thread between the attachment point and the motor and creates a global matrix of all thread lengths given a desired abduction or flexion angle. The app script graphs the movement of the rig through previous calculations and transmits that information to the abduction and flexion code. The abduction and flexion scripts take an input of a desired angle of abduction or flexion and change the thread length to the correct amount based on the desired abduction or flexion by rotating the motors. Cameron then took these relative positions and made an interactive 3D plot in MATLAB where a user can input an amount of abduction or flexion and the program will show four views of where the wire attachment points will be in 3D space, one angled view from

behind and above, one view from straight on, one view from directly above, and one view straight on from the side, as shown in Figure 56 in Section 3.8.2.

Using the MATLAB code we can determine the position of each point throughout scapular and humeral movement. In figures 46 through 51, we determined the acceleration of each point throughout abduction. The data for the graphs below is made up of over 10,000 calculated data points so the addition of variables was made to make the data more digestible in an excel spreadsheet. The duration of abduction and flexion can be altered by changing the total time and the degrees between data points can be altered to get an average of the data for each point. We wanted to portray the change in acceleration of each point to convey the complexity of the scapulohumeral rhythm.

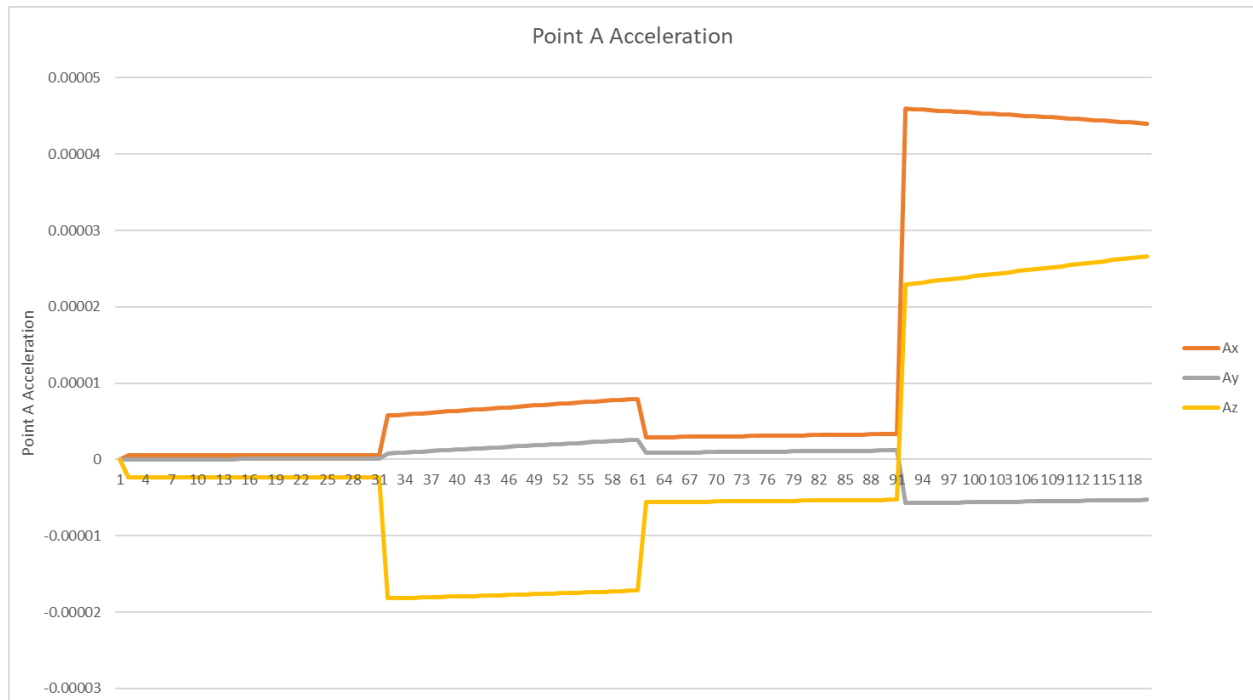


Figure 47: Acceleration of point A over degrees Abduction

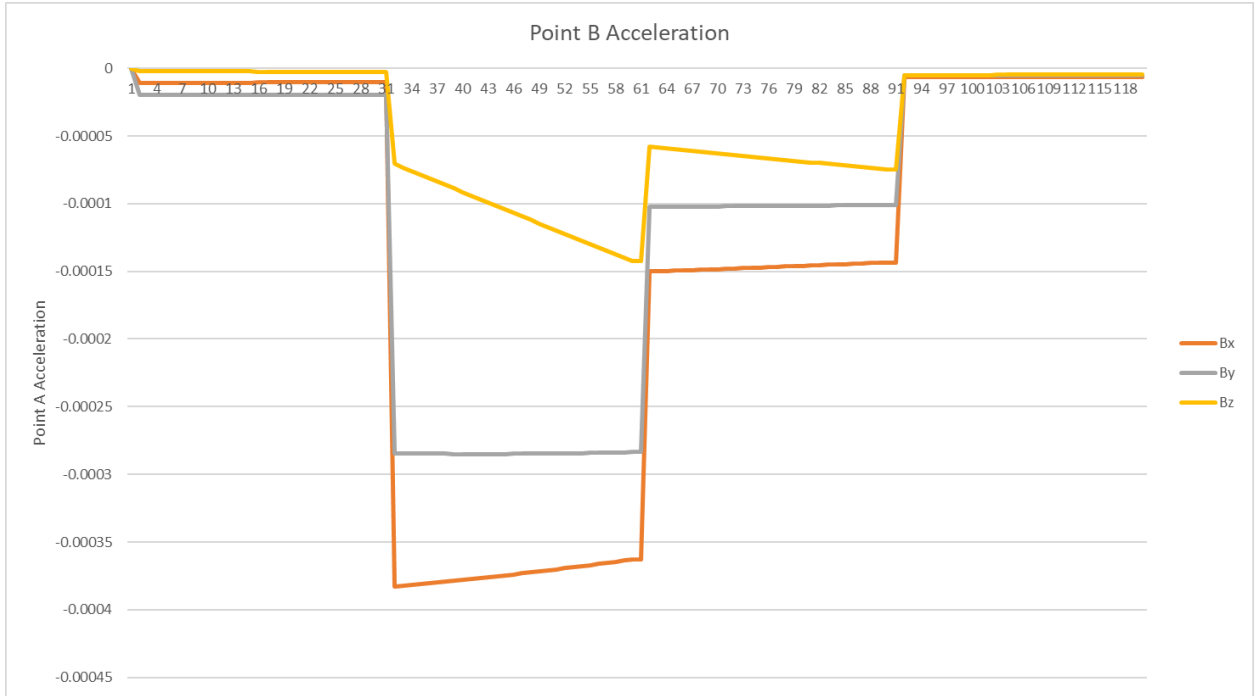


Figure 48: Acceleration of point B over degrees Abduction

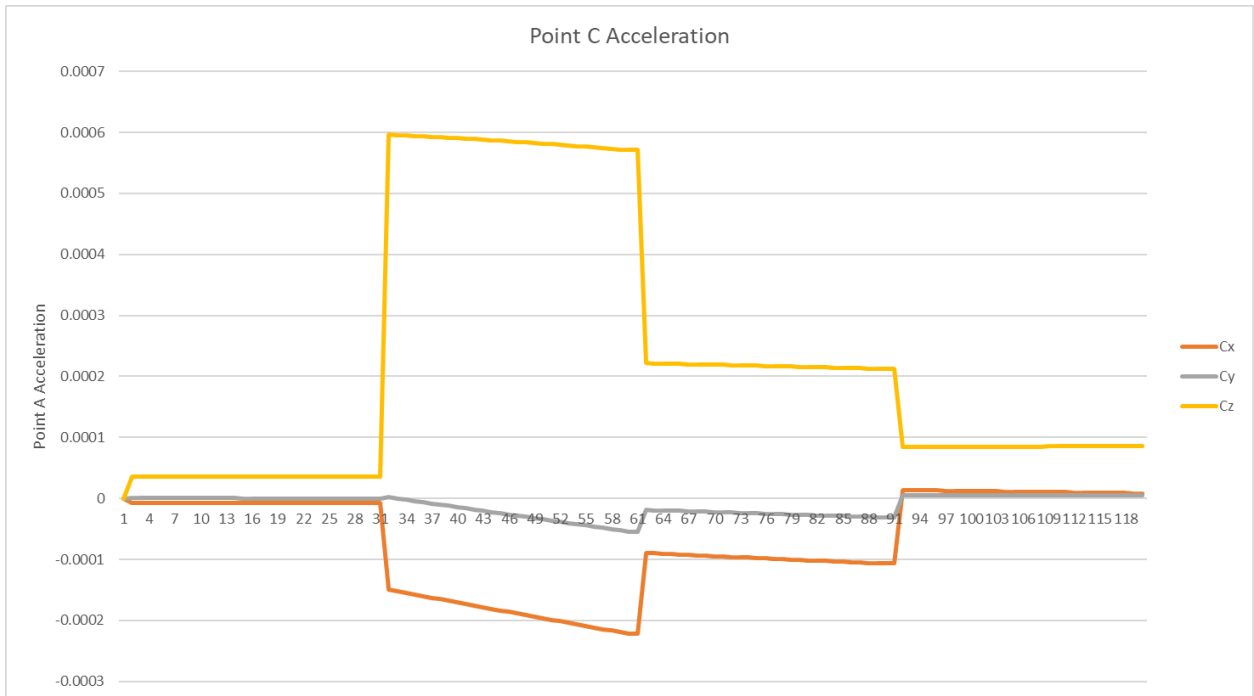


Figure 49: Acceleration of point C over degrees Abduction

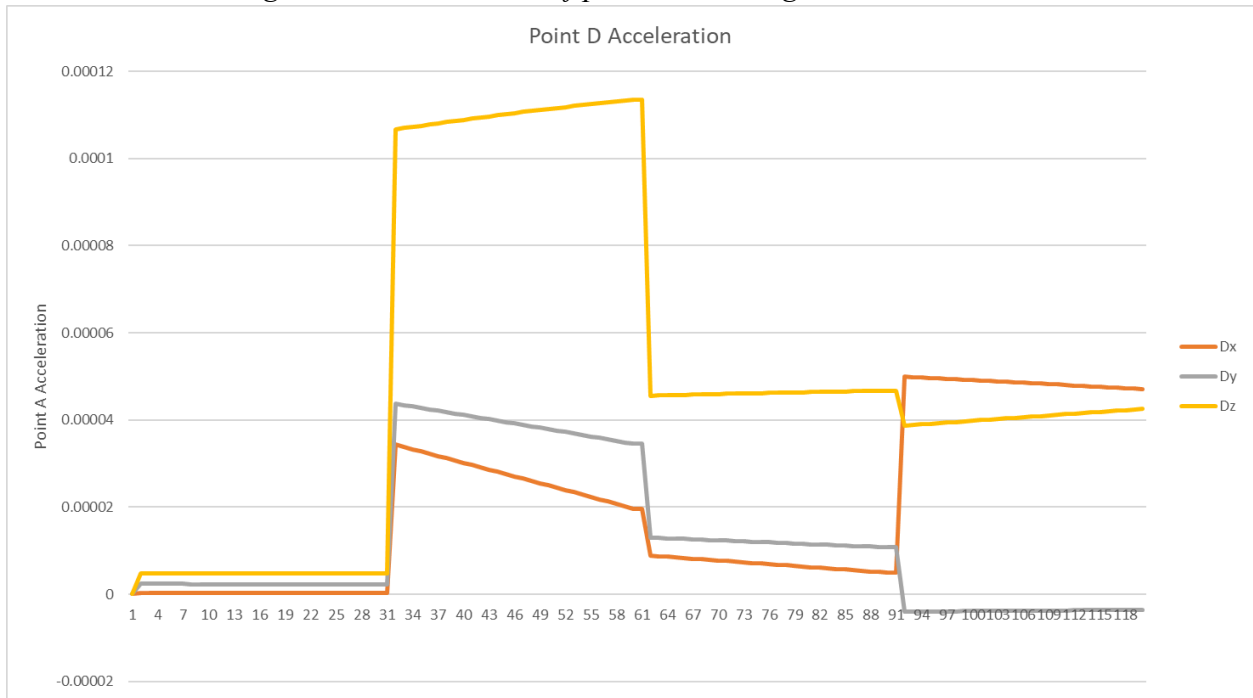


Figure 50: Acceleration of point D over degrees Abduction

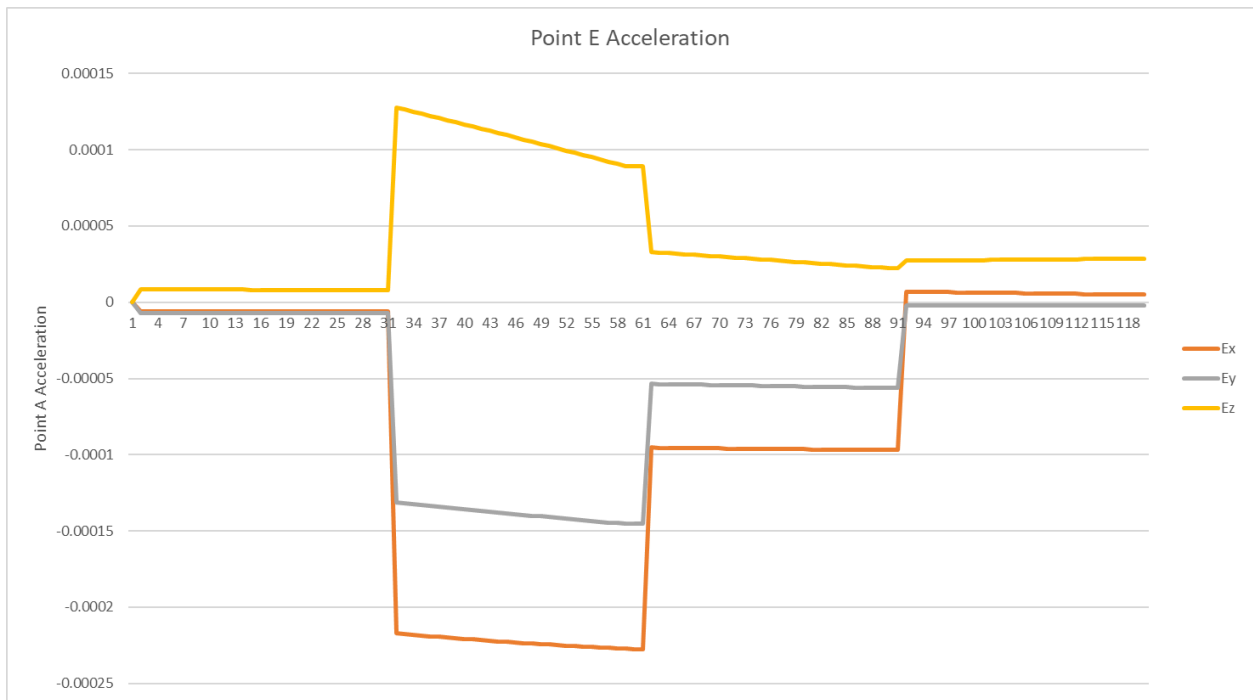


Figure 51: Acceleration of point E over degrees Abduction

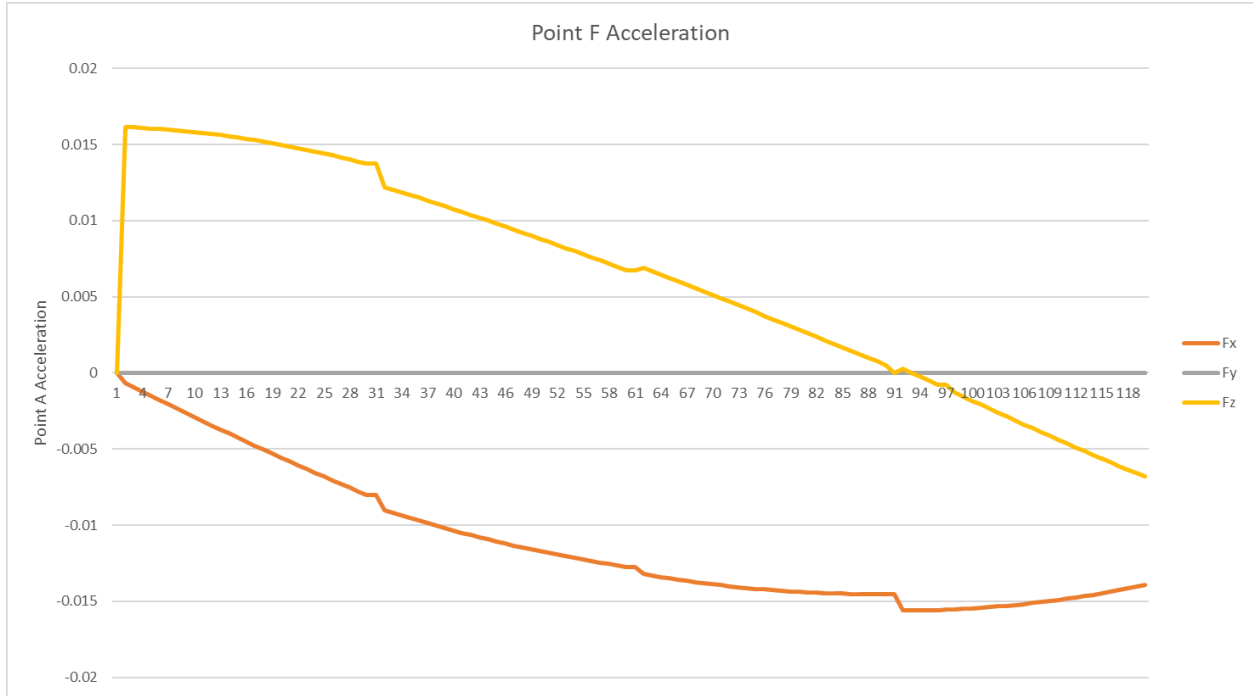


Figure 52: Acceleration of point F over degrees Abduction

We can also use the thread lengths to check our work along with measuring the distances by hand. We can measure xyz manually to make sure the ijk vectors are correct and measure the thread length to confirm the overall vector acceleration. The wire we are using is not elastic under the delivered force so we know that the delta thread length is relatively true.

3.6.3 Circuit Design

The circuitry utilized for the rig underwent a large change from the 2021-2022 team’s circuit design. The 2021-2022 circuit design, displayed below in figure 54, is a simple parallel circuit designed to deliver power and current to each motor simultaneously so as to ensure each motor receives enough voltage to run, however, the equipment used to build the circuit was inadequate to serve our purpose. The breadboard utilized to build the circuit was not built to handle a current higher than 1 amp, which is almost doubled when all five motors are run through the circuit. Additionally a single 9-volt battery is incapable of delivering enough power to support five motors at once, let alone the ten our team would implement.

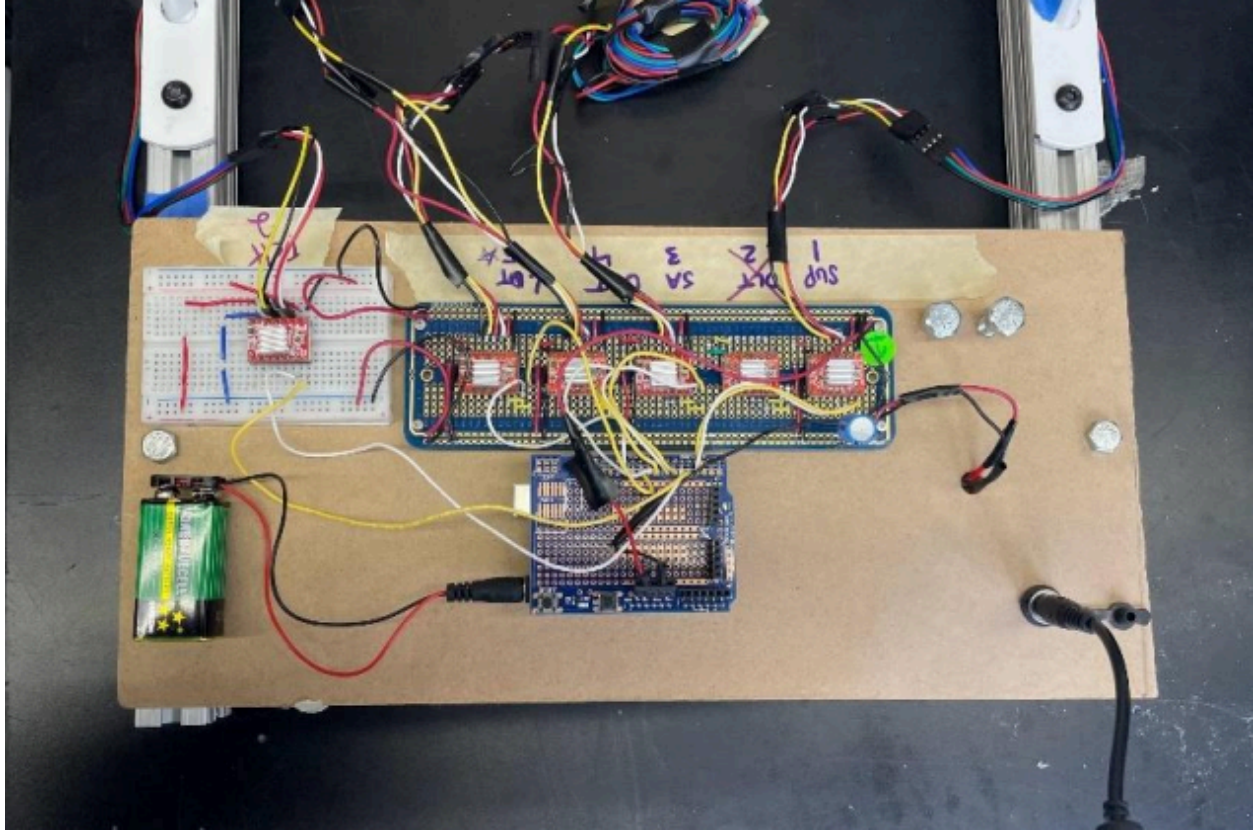
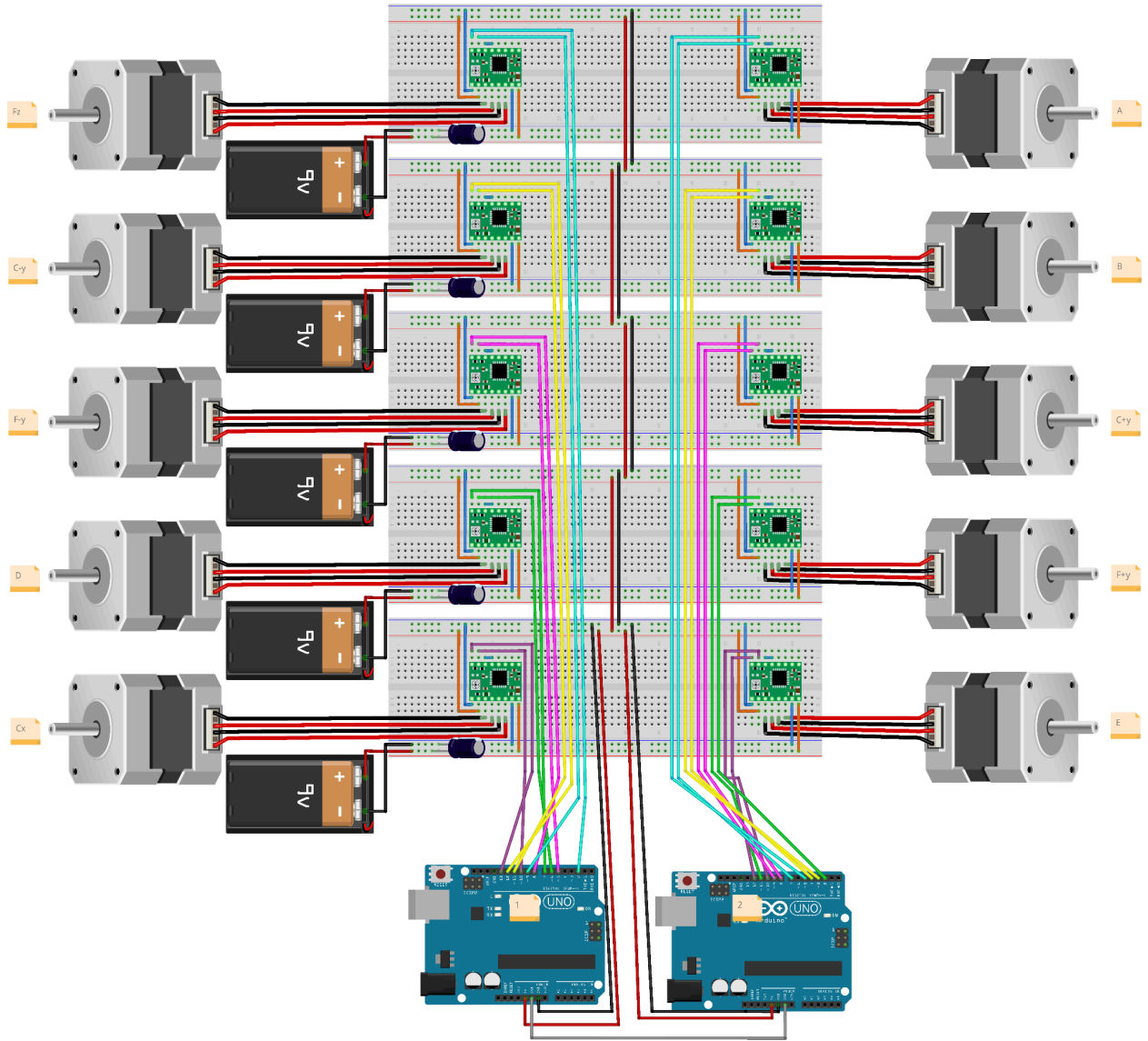


Figure 53: The 2022-2023 Team's Fully Assembled Physical Circuit (McEvelly et al., 2022)

To resolve these issues, our team opted to implement a larger power source, with the intention of utilizing numerous 9-volt batteries at once with plans to ultimately plug the system into a wall outlet. Further alterations to the circuit include the addition of a second Arduino board, to ensure enough pins were available for the ten microprocessor-motor systems. The next iteration of the circuit design is displayed below in Figure 55.

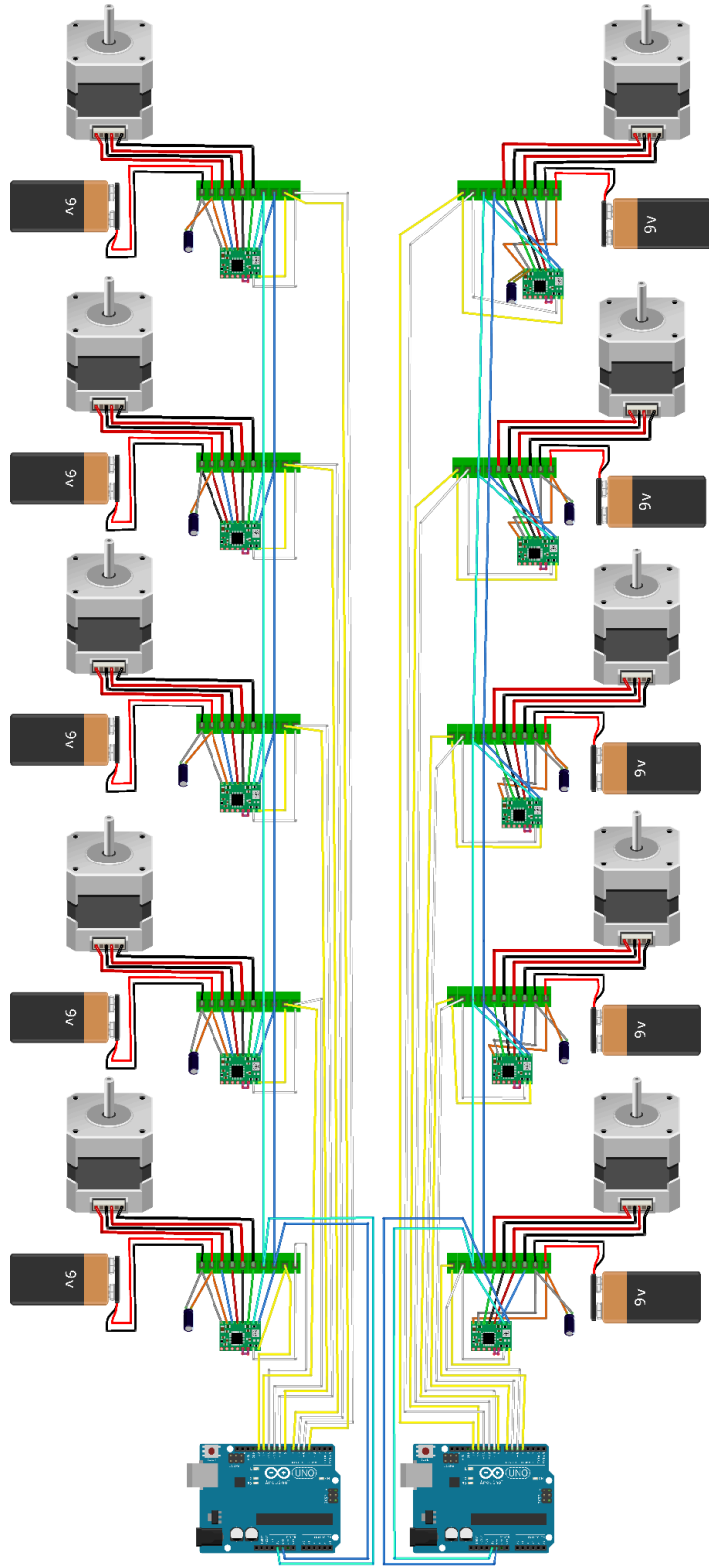


fritzing

Figure 54: Second Iteration of the Circuitry

To circumvent the breadboard's limitations, breadboards were removed from the circuit, instead utilizing space studs, cable nail in clips, and terminal blocks to connect and complete the circuit. The team also experienced trouble operating both Arduinos. This was due to the fact that we had not adjusted the current limit potentiometer and we also had the power source of all ten motor drivers connected to the Arduinos in series. This overloaded one of the Arduinos causing it to short and turn off. To fix these issues we moved from breadboards to 10 circuit terminal blocks instead of the breadboard. We added five more 9V batteries to power each motor individually which we were hoping would improve our low voltage. To fix the shorting Arduino,

instead of all ten of the motor drivers being powered by the 5V output from the Arduino which were run in one series we split it into two series of five. Each series is powered by their own 5V Arduino output pin . The updated schematic is shown in Figure 56 below. One of our largest oversights came with the needed voltage. The original consensus was that 9V would have been enough to power the motors but that was for the previous model of motor used. The 17HS19-1684S-PG27 only needed 2.8V in order to turn, whereas the 17HS13-0404S-PG27 needed around 12V to properly run.



fritzing

Figure 55: Updated Schematic of the Circuitry

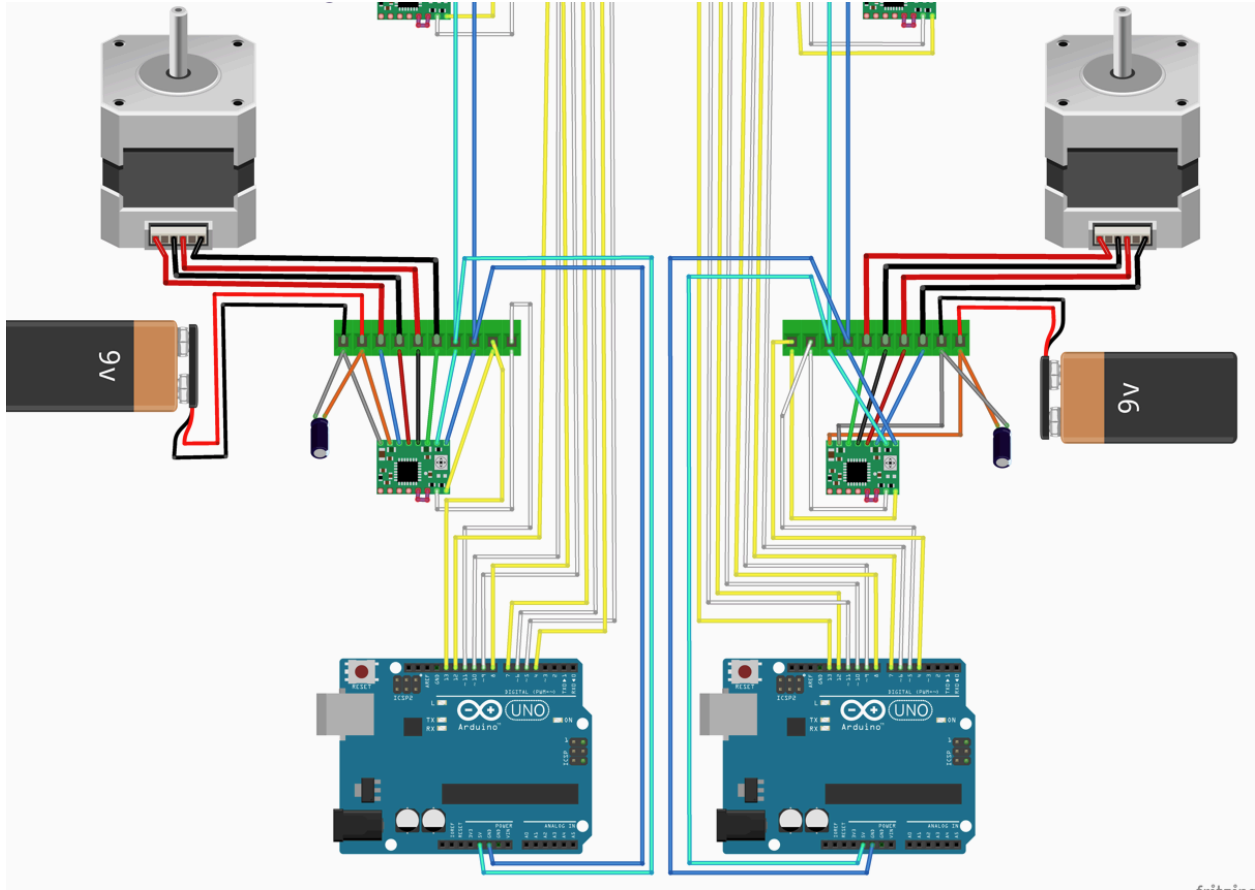


Figure 56: Zoomed in Schematics of the Arduinos

On the A4988 motor driver the RESET pin needs to be HIGH so our team connected it to the SLEEP pin which pulls HIGH by default. We also used a 100uF capacitor to regulate power surges between our motor power supply and the driver. When picking a place for the capacitor our team placed it as close to the driver as possible so there is less surge throughout the wire, especially if the distance between the batteries and the motor drivers is larger.

3.7 Testing

The team successfully constructed the cage and attached the motors to the surrounding frame. We were unable to conduct testing of the fully constructed rig due to time constraints. While the team did not get all 10 motors rotating at once, the team did test to see if the motor positions were able to achieve the correct relative positions of the 3D printed bones. In doing so, all ten motors were tested for their ability to function as expected in the rig as described in the following sections.

3.7.1 Testing Relative Position

The team chose to test the relative positions at rest, then in intervals of 30 degrees of abduction and flexion, ending at 120 degrees of abduction and flexion. The team made this decision as in between these checkpoints the motion of points on the scapula is linear. The team manually set the thread lengths to their desired lengths and suspended the scapula and humerus from the motors in order to show a proof of concept.

3.7.2 Motor Calibration

Motor calibration tests were based on finding out how much the motor changed the thread length as a function of how many seconds the motor spun. The first step was finding the angular velocity of the motor. To do this, the team made a simple MatLab code that can spin the motor for an inputted number of seconds. The team then inputted one, five, and ten seconds and measured the degrees of rotation with tape and a protractor. To refine this measurement, the team made a MatLab code that inputted desired degrees of rotation and spun the motor as such. The team ran the code to ten full rotations, or 3600 degrees, and manually changed the conversion coefficient—that converts from degrees to seconds of rotation—until the motor could spin 3600 degrees within half a degree of precision. The team then calculated, based on the diameter of the spool, how much thread the motor was moving per second and updated the conversion coefficient—that converts from thread length moved to seconds of rotation—in the final code.

3.7.3 Testing Individual Motors

In order to test individual motors, the team wrote a simple MatLab code that talked to one motor at a time and was easily switched between which motor was being tested. Motors were identified to work upon the activation of the code, where the motor would begin to rotate in accordance with the written script. Motors that did not rotate or did not rotate in accordance with the script were identified as dysfunctional. Once it was determined if a motor was functioning properly or not the team troubleshooted to identify the error, further details on the troubleshooting process are provided in the following section.

3.7.4 Troubleshooting

Our team troubleshooted for errors throughout the process of constructing the rig. During the construction of the cage, an angle bar was utilized to ensure proper angles within the cage as well as physical exertion upon the bars to ensure they were properly secured and firm in their placement. Motor tests revealed a number of faulty motors that were promptly replaced or repaired through corrections within the code.

Throughout construction of the rig, circuitry for the rig proved to be the most complex to troubleshoot, as the presence of numerous components, each with their own individual ability to experience error, posed difficult to sort through. Removal of the breadboards, as described in section 3.3, was the first correction to attempt to circumvent the amperage limit that was imposed by the hardware. Further corrections to the circuitry were completed with the use of a DC power supply, allowing the circuitry to experience a number of different amperes and voltages combinations to expose further faults within the wiring by observing if the motors would rotate with varying inputs. By providing a wider range of voltages and amperes, we were able to identify what range of voltages and amperes worked with the circuit and ten 17HS13 motors. Additionally, a voltmeter was utilized to measure the voltage across circuitry components, to ensure the proper distribution of voltage across all key components. Several faulty capacitors were replaced in addition to corrections made to the Arduino boards.

3.8 Results

While relative motion of the scapular and the humerus was not achieved, the team made progress that will be valuable for the continuation of this project, by Cameron Leffler, in D-term and for future teams that continue the project.

3.8.1 Partially Completed Rig

The team constructed a nearly complete model, including the surrounding frame to support the humerus and scapula. The cage is capable of supporting all necessary forces to manipulate the bones to reproduce anatomically correct movements. The circuitry was similarly completed and is capable of delivering sufficient power and commands from the MatLab scripts to all ten motors of the rig.

3.8.2 Interactive Scapula Position Graph

The team lead for this portion of the project, Cameron Leffler, created an interactive graph within MatLab that, with two inputs between 0 and 120 degrees, one for abduction and one for flexion, would replicate the proper anatomical movements of a humerus and scapula within a confined graph. This motion is viewable from numerous varying angles. The viewer can select a degree from a bar located at the bottom of the window with intervals of 1 degree. Figure 57 shows the interactive app set at 90 degrees of humeral flexion. Due to constraints with setting the camera in the MatLab app maker, the axes in the figure are not correct, however, the relative motion is the same.

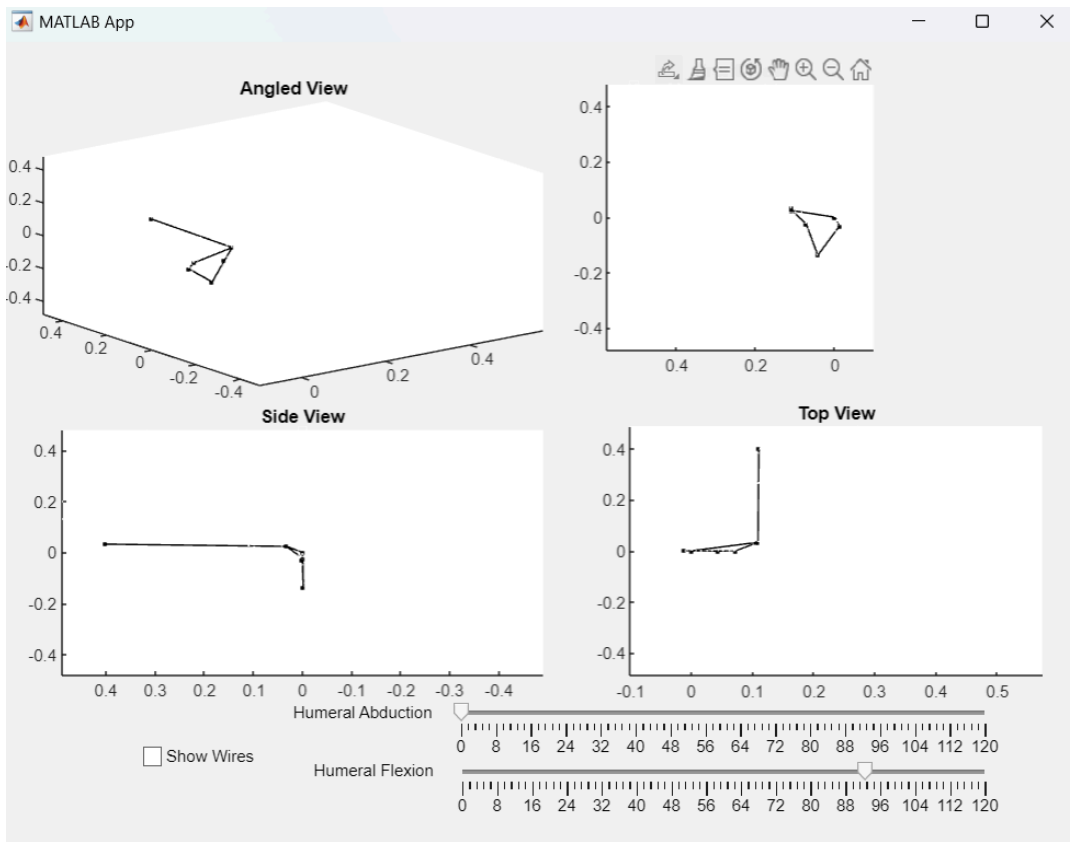


Figure 57: The Interactive Scapula Position Graph

4.0 Discussion

Through review of the results, the team was able to determine our successes and shortcomings throughout the duration of the project.

4.1 Motor Location and Function

The team was successful in relocating the motors to positions that would more easily allow freedom of movement for the rig through abduction and flexion. The surrounding motors pulling from locations external to the humerus and scapula provided far more ideal force vectors to manipulate the movement of the bones. The motors were summarily successful in their calibration with the Arduino code to accurately rotate the correct amount and retract the correct length of braided nylon fishing wire. Unfortunately, due to time constraints, a full test of the motors system was unable to be completed, leaving a lack of experimental results to supplement the theoretical calculations.

4.2 Materials Selection

The team was successful in selecting proper materials to mitigate complications during humeral abduction and flexion. The removal of the restrictive materials placed on the model by the 2022-2023 team, meant to simulate the muscles, ligaments, tendons, and other biological material within the shoulder allowed for freedom in designing the rig, with a larger focus on properly replicating the relative motion between the scapula and humerus. To minimize friction from connection points between the motors and the scapula and humerus, a selection of nylon braided fishing wire was utilized for the low friction coefficient alongside the durability presented by the material. Similar to section 4.1, time constraints limited the team's ability to experimentally test the materials selected.

4.3 MatLab Code and Interactive Position Graph

The team was successful in writing MatLab code to control 10 motors to accurately recreate the scapular humeral rhythm during humeral abduction and flexion and used MatLab to create an interactive position graph showing the relative motion of the scapula and humerus

during humeral abduction and flexion. To the team's knowledge, both of these codes did not exist before this project. The relative positions from the code will be saved and used by Cameron Leffler to create a 3D animation of the scapular humeral rhythm during D-term.

5.0 Broader Impacts

5.1 Engineering Ethics

Over the duration of our project, we sought to be in accordance with the engineering code of ethics implemented by the American Society of Mechanical Engineering. Our team strived to use our understanding of engineering for the benefits of human welfare, increase the competence and prestige of the engineering profession, and to act with honesty and impartiality when developing this project. These fundamental principles integral to the engineering guidelines were held to high standards as we completed our project. This project was completed with the goal of aiding medical students through the use of an educational device, a goal created through the intention of providing beneficial material for the betterment of others. Through this report, we have strived to be truthful to establish integrity within our work. It is our sincere hope that our efforts reflect well on the engineering field.

Our project was a continuation of two prior MQP teams' efforts on the shoulder model, with great effort made to build off the foundation they created whilst respecting their own accomplishments. Their results and data were supplemented by our own research and findings to create a sufficient project that reflects the efforts of all the teams who have dedicated their work towards this shoulder model.

Finally, we sought to complete this project to the fullest extent of our abilities and produce the highest quality model we were capable of creating, utilizing numerous reputable sources and our own engineering expertise to create as accurate a model as possible.

5.2 Social and Global Impact

The primary intention of this model is to be utilized as an educational tool for the improved understanding of the shoulder joint and the complexities that lie within it. This educational tool would go on to benefit a subset of people within society, primarily students seeking to study human anatomy to become doctors. This tool would further these student's understanding of the complexities of the human shoulder, producing more educated doctors who will go on to provide better treatment to patients suffering from injuries, conditions caused by chronic illnesses or genetic defects. Additional applications towards injury prevention are possible such as utilizing the model to explore protective gear for athletes.

5.3 Environmental Impact

The new materials used for the model and rig include braided nylon fishing line wires and aluminum extrusion to construct the cage for the model. The aluminum extrusion used to construct the cage was reused from previous projects. The braided nylon fishing line connecting the bones to the 17HS13 motors is biodegradable and environmentally friendly. Motors used within the rig are composed of a number of metals and electronic components which are not environmentally friendly. Finally, the current power source for the rig, 9V batteries are not environmentally friendly, however, the rig can be modified to draw power from electrical outlets to reduce this waste. The model is projected to be utilized over a large quantity of years without requiring significant replacements to parts or significant upkeep, allowing a minimum amount of materials to be wasted over the course of the model's lifespan.

Materials utilized for our rig by the previous teams includes PLA 3D printed bones and 3D printed motor mounts which are biodegradable and will decompose in 12 weeks time when disposed of. Other materials utilized by the previous teams included KT Tape, Formlabs Elastic 50A, Formlabs Flexible 80A, and Thermoplastic Polyurethane, all of which we removed from our design and model to minimize waste and clutter of the rig, and reduce our environmental impact.

5.4 Economic Impact

The cost of our modifications to the model was relatively low, and is tabulated below. The braided fishing line and aluminum extrusion were inexpensive. The stepper motors contributed to a far larger comparative expense. The electrical components consisting of the arduino board and microprocessors along with all the other circuitry additionally contributed to the cost.

Material	Quantity	Independent Vendor	Cost
17HS13 Motors	10	Yes	~\$300
A4988 Stepper Motor Drivers	10	Yes	~\$13
Braided Nylon Fishing Line	1	Yes	~\$12
Aluminum Extrusion (Varying Sizes)	19	No	Not Applicable
Cable Nail-in Clips	12	Yes	~\$8
Terminal Blocks	12	Yes	~\$120

Table 10: Cost of Materials Used to Modify the Rig

The projected cost of the model is about \$453 USD. While initially costly, when compared to current commercially available educational models, the model becomes far more reasonable in price as most other models range from around \$300 to \$900, with varying features included within the product. Most models on the lower end do not include any joints to display movement, rather they are entirely static. Many models on the upper end of the range include very detailed depictions of muscles and ligaments, but still do not display movement.

6.0 Conclusions and Future Work

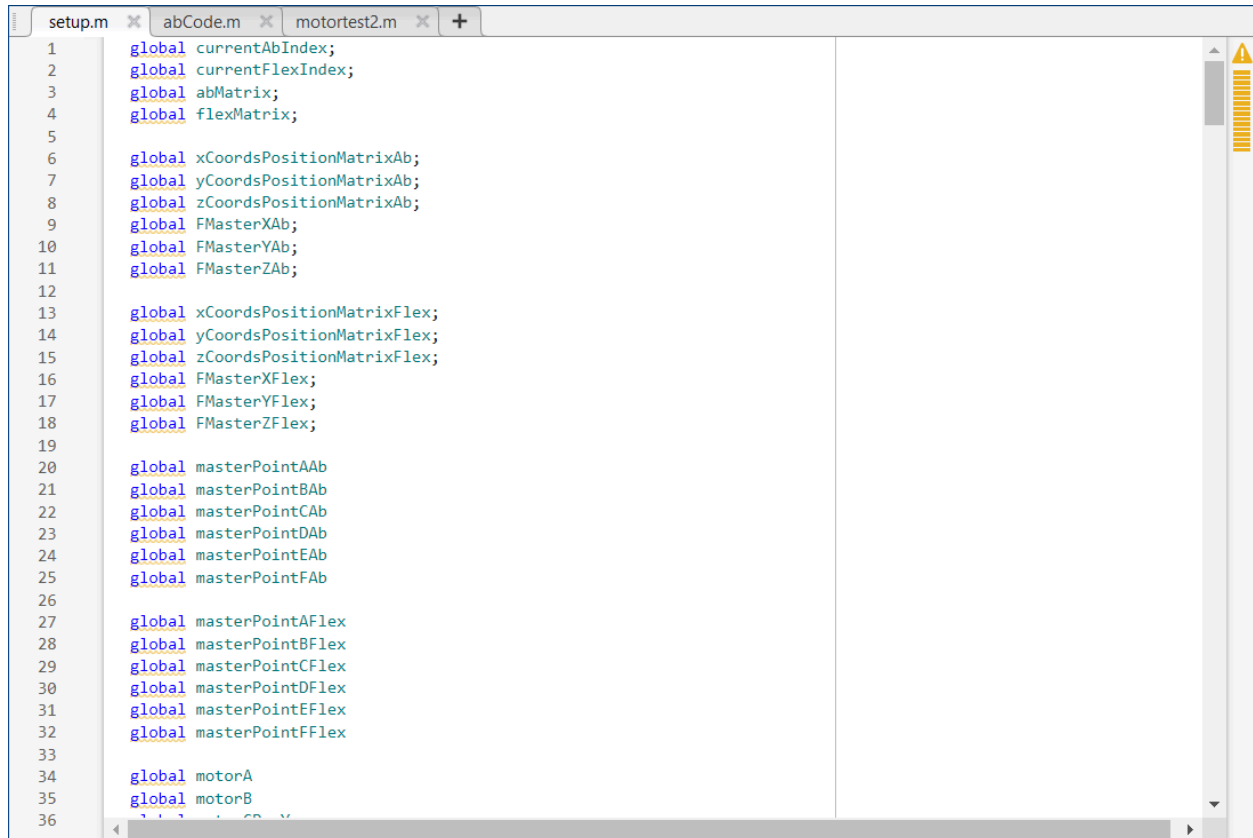
The goal of this project was to demonstrate accurate scapulohumeral rhythm by revising and improving upon the previous team's iterations. To accomplish this, the team stripped the model of the restrictive soft tissue materials and constructed a surrounding cage where motors would deliver force upon the humerus and scapula to direct its movements to replicate the scapulohumeral rhythm during abduction and flexion of the humerus. The team then wrote MatLab scripts to direct movements of the motors to produce our desired motion. Although time constraints prevented further testing of the model and developments of the system, the modifications our team made to the model present potential for a fully realized system that replicates proper anatomical movements.

With the aforementioned time constraints restricting the progress of the model, our team believes that future teams can complete the construction of the rig and upon discovery of any potential errors, can continue to develop it. Of the potential foci future teams can follow, we suggest to first continue development of the current model, finalizing its testing to provide experimental results to supplement theoretical calculations. Additionally, altering the power source for the model from batteries to outlets to avoid repeated purchases of power sources is heavily suggested. Other avenues of development involve a number of options. The development of specialized printed bones to replicate medical conditions such as arthritis would allow for easily swappable parts to bolster the versatility of the model. Adjustments to the model to account for the removed materials from the 2022-2023 team could similarly be made to allow for the biological materials that the 2022-2023 team sought to replicate in their model.

With a fully realized rig and modifications made to the power source, this model has incredible potential as an educational tool. Medical experts that have a deeper understanding of injuries of any type, are capable of treating a greater number of patients. The value in providing medical students a deeper and more thorough understanding of the human shoulder cannot be understated.

7.0 Appendix: MatLab Code

Provided below is the complete code written by our team. The team lead for this portion of the project, as previously stated, was Cameron Leffler



```
1  global currentAbIndex;
2  global currentFlexIndex;
3  global abMatrix;
4  global flexMatrix;
5
6  global xCoordsPositionMatrixAb;
7  global yCoordsPositionMatrixAb;
8  global zCoordsPositionMatrixAb;
9  global FMasterXAb;
10 global FMasterYAb;
11 global FMasterZAb;
12
13 global xCoordsPositionMatrixFlex;
14 global yCoordsPositionMatrixFlex;
15 global zCoordsPositionMatrixFlex;
16 global FMasterXFlex;
17 global FMasterYFlex;
18 global FMasterZFlex;
19
20 global masterPointAAb
21 global masterPointBAb
22 global masterPointCAb
23 global masterPointDAb
24 global masterPointEAb
25 global masterPointFAb
26
27 global masterPointAFlex
28 global masterPointBFlex
29 global masterPointCFlex
30 global masterPointDFlex
31 global masterPointEFlex
32 global masterPointFFlex
33
34 global motorA
35 global motorB
36
```



```

36  global motorCPosY
37  global motorCNegY
38  global motorCX
39  global motorD
40  global motorE
41  global motorFZ
42  global motorFPosY
43  global motorFNegY
44
45  currentFlexIndex = 1;
46  currentAbIndex = 1;
47
48  %%Initial Positions
49  A = [0;0;0];
50  B = [0.11; 0.035; 0.013];
51  C = [0.03;-0.004;-0.141];
52  D = [-0.015;0;-0.03];
53  E = [0.07;0;-0.03];
54  F = [0.11;0.035;-0.3696];
55  G = B;
56  I = [0.01; 0; -0.01];
57  J = [0.12; 0; -0.01];
58  K = [0.01; 0; -0.15];
59
60  motorA = [A(1); A(2); 0.38203];
61  motorB = [B(1); B(2); 0.38203];
62  motorCPosY = [C(1); 0.39; C(3)];
63  motorCNegY = [C(1); -0.39; C(3)];
64  motorCX = [0.474; C(2); 0];
65  motorD = [D(1); -0.39; D(3)];
66  motorE = [E(1); 0.39; E(3)];
67  motorFZ = [0.237; 0; 0.38203];
68  motorFPosY = [0.237; 0.39; 0];
69  motorFNegY = [0.237; -0.39; 0];
70
71  %%%Abduction

```

```

71  %%%Abduction
72
73  %Other starting conditions
74  armAngleAbduction = 0;
75  increaseAbA = 0.1;
76  radIncreaseAbA = deg2rad(increaseAbA);
77  armAngleAbductionMatrix = [armAngleAbduction;0];
78
79  masterPositionMatrixAb = [A,B,C,D,E,I,J,K];
80  xCoordsPositionMatrixAb = [0,0,0,0,0];
81  yCoordsPositionMatrixAb = [0,0,0,0,0];
82  zCoordsPositionMatrixAb = [0,0,0,0,0];
83  FMasterAb = [0.11;0.035;-0.3696];
84  FMasterXAb = [0;0];
85  FMasterYAb = [0;0];
86  FMasterZAb = [0;0];
87
88  wireLengthMatrixAb = allWireLength(motorA,motorB,motorCPosY,motorCNegY,...
89  motorCX,motorD,motorE,motorFPosY,motorFNegY,motorFZ,A,B,C,D,E,F);
90  threadLengthAMatrixAb = [0;0];
91  threadLengthBMatrixAb = [0;0];
92  threadLengthCPosYMatrixAb = [0;0];
93  threadLengthCNegYMatrixAb = [0;0];
94  threadLengthCXMatrixAb = [0;0];
95  threadLengthDMatrixAb = [0;0];
96  threadLengthEMatrixAb = [0;0];
97  threadLengthFPosYMatrixAb = [0;0];
98  threadLengthFNegYMatrixAb = [0;0];
99  threadLengthFZMatrixAb = [0;0];
100
101  counter = 4;
102  i = 1;
103
104  while armAngleAbduction <= 120
105
106

```

```

setup.m x abCode.m x motortest2.m x +
107     %%Set correct angles or rotation
108     if armAngleAbduction <= 30
109         %SA angles for 0-30 degrees of AA
110         upwardRotation = deg2rad(-3.39);
111         anteriorTilt = deg2rad(6.04);
112         externalRotation = deg2rad(1.29);
113
114         upwardRotationStep = upwardRotation/(30/increaseAbA);
115         anteriorTiltStep = anteriorTilt/(30/increaseAbA);
116         externalRotationStep = externalRotation/(30/increaseAbA);
117
118         ICR = A;
119     end
120
121     if armAngleAbduction > 30 && armAngleAbduction <= 60
122         %SA angles for 30-60 degrees of AA
123         upwardRotation = deg2rad(-26.34)-deg2rad(-3.39);
124         anteriorTilt = deg2rad(22.28)-deg2rad(6.04);
125         externalRotation = deg2rad(5.93)-deg2rad(1.29);
126
127         upwardRotationStep = upwardRotation/(30/increaseAbA);
128         anteriorTiltStep = anteriorTilt/(30/increaseAbA);
129         externalRotationStep = externalRotation/(30/increaseAbA);
130
131         ICR = A;
132     end
133
134     if armAngleAbduction > 60 && armAngleAbduction <= 90
135         %SA angles for 60-90 degrees of AA
136         upwardRotation = deg2rad(-41.25)-deg2rad(-26.34);
137         anteriorTilt = deg2rad(31.45)-deg2rad(22.28);
138         externalRotation = deg2rad(8.92)-deg2rad(5.93);
139
140         upwardRotationStep = upwardRotation/(30/increaseAbA);
141         anteriorTiltStep = anteriorTilt/(30/increaseAbA);
142

```

```

setup.m x abCode.m x motortest2.m x +
142         externalRotationStep = externalRotation/(30/increaseAbA);
143
144         ICR = A;
145     end
146
147     if armAngleAbduction > 90 && armAngleAbduction <= 120
148         %SA angles for 90-120 degrees of AA
149         upwardRotation = deg2rad(-50.85)-deg2rad(-41.25);
150         anteriorTilt = deg2rad(33.49)-deg2rad(31.45);
151         externalRotation = deg2rad(10.71)-deg2rad(8.92);
152
153         upwardRotationStep = upwardRotation/(30/increaseAbA);
154         anteriorTiltStep = anteriorTilt/(30/increaseAbA);
155         externalRotationStep = externalRotation/(30/increaseAbA);
156
157         changeX = B(1) - A(1);
158         changeY = B(2) - A(2);
159         changeZ = B(3) - A(3);
160         ICR = [changeX/2;changeY/2;changeZ/2];
161     end
162
163     BforF = B;
164
165     masterPositionMatrixAb(counter:counter+2,:) = fullRotation(A,B,C,D,E,I,...
166         J,K,upwardRotationStep,anteriorTiltStep,externalRotationStep,ICR);
167     FMasterAb(counter:counter+2,1) = humeralAbduction(BforF,B,F,radIncreaseAbA);
168
169     A = masterPositionMatrixAb(counter:counter+2,1);
170     B = masterPositionMatrixAb(counter:counter+2,2);
171     C = masterPositionMatrixAb(counter:counter+2,3);
172     D = masterPositionMatrixAb(counter:counter+2,4);
173     E = masterPositionMatrixAb(counter:counter+2,5);
174     I = masterPositionMatrixAb(counter:counter+2,6);
175     J = masterPositionMatrixAb(counter:counter+2,7);
176     K = masterPositionMatrixAb(counter:counter+2,8);
177

```

```

setup.m x abCode.m x motortest2.m x +
177     F = FMasterAb(counter:counter+2,1);
178
179     armAngleAbductionMatrix((counter-1)/3) = armAngleAbduction;
180
181     threadLengthAMatrixAb((counter-1)/3) = wireLengthMatrixAb(1,1);
182     threadLengthBMatrixAb((counter-1)/3) = wireLengthMatrixAb(1,2);
183     threadLengthCPosYMatrixAb((counter-1)/3) = wireLengthMatrixAb(1,3);
184     threadLengthCNegYMatrixAb((counter-1)/3) = wireLengthMatrixAb(1,4);
185     threadLengthCMatrixAb((counter-1)/3) = wireLengthMatrixAb(1,5);
186     threadLengthDMatrixAb((counter-1)/3) = wireLengthMatrixAb(1,6);
187     threadLengthEMatrixAb((counter-1)/3) = wireLengthMatrixAb(1,7);
188     threadLengthFPosYMatrixAb((counter-1)/3) = wireLengthMatrixAb(1,8);
189     threadLengthFNegYMatrixAb((counter-1)/3) = wireLengthMatrixAb(1,9);
190     threadLengthFZMatrixAb((counter-1)/3) = wireLengthMatrixAb(1,10);
191
192     wireLengthMatrixAb = allWireLength(motorA,motorB,motorCPosY,motorCNegY,...
193         motorCX,motorD,motorE,motorFPosY,motorFNegY,motorFZ,A,B,C,D,E,F);
194
195     armAngleAbduction = armAngleAbduction + increaseAbA;
196     counter = counter + 3;
197 end
198
199 while i < size(masterPositionMatrixAb,1)/3
200     xCoordsPositionMatrixAb(i,:) = masterPositionMatrixAb(i*3-2,1:5);
201     yCoordsPositionMatrixAb(i,:) = masterPositionMatrixAb(i*3-1,1:5);
202     zCoordsPositionMatrixAb(i,:) = masterPositionMatrixAb(i*3,1:5);
203
204     i = i+1;
205 end
206
207     i = 1;
208
209 while i < size(FMasterAb,1)/3
210     FMasterXAb(i,:) = FMasterAb(i*3-2,:);
211     FMasterYAb(i,:) = FMasterAb(i*3-1,:);
212

```

```

setup.m x abCode.m x motortest2.m x +
212     FMasterZAb(i,:) = FMasterAb(i*3,:);
213
214     i = i+1;
215 end
216
217
218     abMatrix = [threadLengthAMatrixAb,threadLengthBMatrixAb,threadLengthCPosYMatrixAb,...
219         threadLengthCNegYMatrixAb, threadLengthDMatrixAb,threadLengthEMatrixAb,...
220         threadLengthFPosYMatrixAb,threadLengthFNegYMatrixAb,threadLengthFZMatrixAb];
221
222
223     %% Reset Initial Positions
224     A = [0;0;0];
225     B = [0.11; 0.035; 0.013];
226     C = [0.03;-0.004;-0.141];
227     D = [-0.015;0;-0.03];
228     E = [0.07;0;-0.03];
229     F = [0.11;0.035;-0.3696];
230     I = [0.01; 0; -0.01];
231     J = [0.12; 0; -0.01];
232     K = [0.01; 0; -0.15];
233
234     %%%%%%% Flexion Time
235
236     wireLengthMatrixFlex = allWireLength(motorA,motorB,motorCPosY,motorCNegY,...
237         motorCX,motorD,motorE,motorFPosY,motorFNegY,motorFZ,A,B,C,D,E,F);
238
239     % Other starting conditions
240     armAngleFlex = 0;
241     increaseFlexA = 0.1;
242     radIncreaseFlexA = deg2rad(increaseFlexA);
243     armAngleFlexMatrix = [armAngleFlex;0];
244
245     masterPositionMatrixFlex = [A,B,C,D,E,I,J,K];
246     xCoordsPositionMatrixFlex = [0,0,0,0,0];
247     yCoordsPositionMatrixFlex = [0,0,0,0,0];

```

```

setup.m x abCode.m x motortest2.m x +
247 yCoordsPositionMatrixFlex = [0,0,0,0,0];
248 zCoordsPositionMatrixFlex = [0,0,0,0,0];
249 FMasterFlex = [0.11;0.035;-0.3696];
250 FMasterXFlex = [0;0];
251 FMasterYFlex = [0;0];
252 FMasterZFlex = [0;0];
253
254 threadLengthAMatrixFlex = [0;0];
255 threadLengthBMatrixFlex = [0;0];
256 threadLengthCPosYMatrixFlex = [0;0];
257 threadLengthCNegYMatrixFlex = [0;0];
258 threadLengthCMatrixFlex = [0;0];
259 threadLengthDMatrixFlex = [0;0];
260 threadLengthEMatrixFlex = [0;0];
261 threadLengthFPosYMatrixFlex = [0;0];
262 threadLengthFNegYMatrixFlex = [0;0];
263 threadLengthFZMatrixFlex = [0;0];
264
265 counter = 4;
266 i = 1;
267
268 while armAngleFlex <= 120
269
270
271     %%Set correct angles or rotation
272     if armAngleFlex <= 30
273         %SA angles for 0-30 degrees of AA
274         upwardRotation = deg2rad(-1.55);
275         anteriorTilt = deg2rad(-1.82);
276         externalRotation = deg2rad(-1.13);
277
278         upwardRotationStep = upwardRotation/(30/increaseFlexA);
279         anteriorTiltStep = anteriorTilt/(30/increaseFlexA);
280         externalRotationStep = externalRotation/(30/increaseFlexA);
281
282

```

```

setup.m x abCode.m x motortest2.m x +
282     ICR = A;
283     end
284
285     if armAngleFlex > 30 && armAngleFlex <= 60
286         %SA angles for 30-60 degrees of AA
287         upwardRotation = deg2rad(-9.14)-deg2rad(-1.55);
288         anteriorTilt = deg2rad(-0.08)-deg2rad(-1.82);
289         externalRotation = deg2rad(-1.93)-deg2rad(-1.13);
290
291         upwardRotationStep = upwardRotation/(30/increaseFlexA);
292         anteriorTiltStep = anteriorTilt/(30/increaseFlexA);
293         externalRotationStep = externalRotation/(30/increaseFlexA);
294
295         ICR = A;
296     end
297
298     if armAngleFlex > 60 && armAngleFlex <= 90
299         %SA angles for 60-90 degrees of AA
300         upwardRotation = deg2rad(-15.03)-deg2rad(-9.14);
301         anteriorTilt = deg2rad(3.80)-deg2rad(-0.08);
302         externalRotation = deg2rad(-1.95)-deg2rad(-1.93);
303
304         upwardRotationStep = upwardRotation/(30/increaseFlexA);
305         anteriorTiltStep = anteriorTilt/(30/increaseFlexA);
306         externalRotationStep = externalRotation/(30/increaseFlexA);
307
308         ICR = A;
309     end
310
311     if armAngleFlex > 90 && armAngleFlex <= 120
312         %SA angles for 90-120 degrees of AA
313         upwardRotation = deg2rad(-26.35)-deg2rad(-15.03);
314         anteriorTilt = deg2rad(11.16)-deg2rad(3.80);
315         externalRotation = deg2rad(0.22)-deg2rad(-1.95);
316
317

```

```
setup.m x abCode.m x motortest2.m x +
317     upwardRotationStep = upwardRotation/(30/increaseFlexA);
318     anteriorTiltStep = anteriorTilt/(30/increaseFlexA);
319     externalRotationStep = externalRotation/(30/increaseFlexA);
320
321     changeX = B(1) - A(1);
322     changeY = B(2) - A(2);
323     changeZ = B(3) - A(3);
324     ICR = [changeX/2;changeY/2;changeZ/2];
325 end
326
327 BforF = B;
328
329 masterPositionMatrixFlex(counter:counter+2,:) = fullRotation(A,B,C,D,E,...
330     I,J,K,upwardRotationStep,anteriorTiltStep,externalRotationStep,ICR);
331 FMasterFlex(counter:counter+2,1) = humeralFlexion(BforF,B,F,radIncreaseFlexA);
332
333 A = masterPositionMatrixFlex(counter:counter+2,1);
334 B = masterPositionMatrixFlex(counter:counter+2,2);
335 C = masterPositionMatrixFlex(counter:counter+2,3);
336 D = masterPositionMatrixFlex(counter:counter+2,4);
337 E = masterPositionMatrixFlex(counter:counter+2,5);
338 I = masterPositionMatrixFlex(counter:counter+2,6);
339 J = masterPositionMatrixFlex(counter:counter+2,7);
340 K = masterPositionMatrixFlex(counter:counter+2,8);
341 F = FMasterFlex(counter:counter+2,1);
342
343 armAngleFlexMatrix((counter-1)/3) = armAngleFlex;
344
345 threadLengthAMatrixFlex((counter-1)/3) = wireLengthMatrixFlex(1,1);
346 threadLengthBMatrixFlex((counter-1)/3) = wireLengthMatrixFlex(1,2);
347 threadLengthCPosYMatrixFlex((counter-1)/3) = wireLengthMatrixFlex(1,3);
348 threadLengthCNegYMatrixFlex((counter-1)/3) = wireLengthMatrixFlex(1,4);
349 threadLengthCXMatrixFlex((counter-1)/3) = wireLengthMatrixFlex(1,5);
350 threadLengthDMatrixFlex((counter-1)/3) = wireLengthMatrixFlex(1,6);
351 threadLengthEMatrixFlex((counter-1)/3) = wireLengthMatrixFlex(1,7);
352
```

```

352     threadLengthFPosYMatrixFlex((counter-1)/3) = wireLengthMatrixFlex(1,8);
353     threadLengthFNegYMatrixFlex((counter-1)/3) = wireLengthMatrixFlex(1,9);
354     threadLengthFZMatrixFlex((counter-1)/3) = wireLengthMatrixFlex(1,10);
355
356     wireLengthMatrixFlex = allWireLength(motorA,motorB,motorCPosY,motorCNegY,...
357         motorCX,motorD,motorE,motorFPosY,motorFNegY,motorFZ,A,B,C,D,E,F);
358
359     armAngleFlex = armAngleFlex + increaseFlexA;
360     counter = counter + 3;
361 end
362
363 while i < size(masterPositionMatrixFlex,1)/3
364     xCoordsPositionMatrixFlex(i,:) = masterPositionMatrixFlex(i*3-2,1:5);
365     yCoordsPositionMatrixFlex(i,:) = masterPositionMatrixFlex(i*3-1,1:5);
366     zCoordsPositionMatrixFlex(i,:) = masterPositionMatrixFlex(i*3,1:5);
367
368     i = i+1;
369 end
370
371 i = 1;
372
373 while i < size(FMasterFlex,1)/3
374     FMasterXFlex(i,:) = FMasterFlex(i*3-2,:);
375     FMasterYFlex(i,:) = FMasterFlex(i*3-1,:);
376     FMasterZFlex(i,:) = FMasterFlex(i*3,:);
377
378     i = i+1;
379 end
380
381 flexMatrix = [threadLengthAMatrixFlex,threadLengthBMatrixFlex,...
382     threadLengthCPosYMatrixFlex, threadLengthCNegYMatrixFlex, threadLengthDMatrixFlex,...
383     threadLengthEMatrixFlex, threadLengthFPosYMatrixFlex,threadLengthFNegYMatrixFlex,...
384     threadLengthFZMatrixFlex];
385
386
387

```

```

388     masterPointAAb = [xCoordsPositionMatrixAb(:,1),yCoordsPositionMatrixAb(:,1),zCoordsPositionMatrixAb(:,1)];
389     masterPointBAb = [xCoordsPositionMatrixAb(:,2),yCoordsPositionMatrixAb(:,2),zCoordsPositionMatrixAb(:,2)];
390     masterPointCAb = [xCoordsPositionMatrixAb(:,3),yCoordsPositionMatrixAb(:,3),zCoordsPositionMatrixAb(:,3)];
391     masterPointDAb = [xCoordsPositionMatrixAb(:,4),yCoordsPositionMatrixAb(:,4),zCoordsPositionMatrixAb(:,4)];
392     masterPointEAb = [xCoordsPositionMatrixAb(:,5),yCoordsPositionMatrixAb(:,5),zCoordsPositionMatrixAb(:,5)];
393     masterPointFAb = [FMasterXAb(:,1),FMasterYAb(:,1),FMasterZAb(:,1)];
394
395     masterPointAFlex = [xCoordsPositionMatrixFlex(:,1),yCoordsPositionMatrixFlex(:,1),zCoordsPositionMatrixFlex(:,1)];
396     masterPointBFlex = [xCoordsPositionMatrixFlex(:,2),yCoordsPositionMatrixFlex(:,2),zCoordsPositionMatrixFlex(:,2)];
397     masterPointCFlex = [xCoordsPositionMatrixFlex(:,3),yCoordsPositionMatrixFlex(:,3),zCoordsPositionMatrixFlex(:,3)];
398     masterPointDFlex = [xCoordsPositionMatrixFlex(:,4),yCoordsPositionMatrixFlex(:,4),zCoordsPositionMatrixFlex(:,4)];
399     masterPointEFlex = [xCoordsPositionMatrixFlex(:,5),yCoordsPositionMatrixFlex(:,5),zCoordsPositionMatrixFlex(:,5)];
400     masterPointFFlex = [FMasterXFlex(:,1),FMasterYFlex(:,1),FMasterZFlex(:,1)];
401
402

```

```

Editor - C:\Users\gray\OneDrive\Documents\MATLAB\mqp\rotation.m *
+2  motortest2.m  allWireLength.m  fullRotation.m  humeralAbduction.m  humeralFlexion.m  rotation.m *
1  function [outputVector] = rotation(inputVector,thetaICR,thetaIJ,thetaIK,I,J,K,ICR)
2  %ROTATION Finds where a point will be after a rotation around all three
3  %axes
4
5  %moving origin to I
6  ICenteredI = [0;0;0];
7  ICenteredJ = [J(1)-I(1);J(2)-I(2);J(3)-I(3)];
8  ICenteredK = [K(1)-I(1);K(2)-I(2);K(3)-I(3)];
9  ICenteredInputVector = [inputVector(1)-I(1);inputVector(2)-I(2);inputVector(3)-I(3)];
10
11 %Finding axis IJ and IK
12 IJ = ICenteredJ - ICenteredI;
13 magIJ = sqrt((IJ(1))^2+(IJ(2))^2+(IJ(3))^2);
14 normalIJ = IJ/magIJ;
15
16 IK = ICenteredI - ICenteredK;
17 magIK = sqrt((IK(1))^2+(IK(2))^2+(IK(3))^2);
18 normalIK = IK/magIK;
19
20 %Rotation around IJ
21 dotIJ = dot(ICenteredInputVector,normalIJ);
22 crossIJ = cross(normalIJ,ICenteredInputVector);
23
24 ICenteredMidVector1 = ((1-cos(thetaIJ))*(dotIJ)*(normalIJ))+((cos(thetaIJ))*...
25 (ICenteredInputVector))+((sin(thetaIJ))*(crossIJ));
26 midVector1 = [ICenteredMidVector1(1)+I(1);ICenteredMidVector1(2)+I(2);ICenteredMidVector1(3)+I(3)];
27
28 %Rotation around JK
29 dotIK = dot(ICenteredInputVector,normalIK);
30 crossIK = cross(normalIK,ICenteredInputVector);
31
32 ICenteredMidVector2 = ((1-cos(thetaIK))*(dotIK)*(normalIK))+((cos(thetaIK))*...
33 (ICenteredInputVector))+((sin(thetaIK))*(crossIK));
34 midVector2 = [ICenteredMidVector2(1)+I(1);ICenteredMidVector2(2)+I(2);ICenteredMidVector2(3)+I(3)];
35
36 %Moving Origin to ICR
37 ICRCenteredJ = [J(1)-ICR(1);J(2)-ICR(2);J(3)-ICR(3)];
38 ICRCenteredK = [K(1)-ICR(1);K(2)-ICR(2);K(3)-ICR(3)];
39 ICRCenteredICR = [0;0;0];
40 ICRCenteredInputVector = [inputVector(1)-ICR(1);inputVector(2)-ICR(2);inputVector(3)-ICR(3)];
41
42 %Making ICR Axis
43 ICRJ = ICRCenteredJ - ICRCenteredICR;
44 ICRK = ICRCenteredK - ICRCenteredICR;
45 axisICR = cross(ICRJ,ICRK);
46 magICR = sqrt((axisICR(1))^2+(axisICR(2))^2+(axisICR(3))^2);
47 normalICR = axisICR/magICR;
48
49 %Rotation around ICR
50 dotICR = dot(ICRCenteredInputVector,normalICR);
51 crossICR = cross(normalICR,ICRCenteredInputVector);
52
53 ICRCenteredMidVector3 = ((1-cos(thetaICR))*(dotICR)*(normalICR))+((cos(thetaICR))*...
54 (ICRCenteredInputVector))+((sin(thetaICR))*(crossICR));
55 midVector3 = [ICRCenteredMidVector3(1)+ICR(1);ICRCenteredMidVector3(2)+ICR(2);ICRCenteredMidVector3(3)+ICR(3)];
56
57 %Calc the output
58 outputVector = (midVector1+midVector2+midVector3)/3;
59
60 end

```

```

36 %Moving Origin to ICR
37 ICRCenteredJ = [J(1)-ICR(1);J(2)-ICR(2);J(3)-ICR(3)];
38 ICRCenteredK = [K(1)-ICR(1);K(2)-ICR(2);K(3)-ICR(3)];
39 ICRCenteredICR = [0;0;0];
40 ICRCenteredInputVector = [inputVector(1)-ICR(1);inputVector(2)-ICR(2);inputVector(3)-ICR(3)];
41
42 %Making ICR Axis
43 ICRJ = ICRCenteredJ - ICRCenteredICR;
44 ICRK = ICRCenteredK - ICRCenteredICR;
45 axisICR = cross(ICRJ,ICRK);
46 magICR = sqrt((axisICR(1))^2+(axisICR(2))^2+(axisICR(3))^2);
47 normalICR = axisICR/magICR;
48
49 %Rotation around ICR
50 dotICR = dot(ICRCenteredInputVector,normalICR);
51 crossICR = cross(normalICR,ICRCenteredInputVector);
52
53 ICRCenteredMidVector3 = ((1-cos(thetaICR))*(dotICR)*(normalICR))+((cos(thetaICR))*...
54 (ICRCenteredInputVector))+((sin(thetaICR))*(crossICR));
55 midVector3 = [ICRCenteredMidVector3(1)+ICR(1);ICRCenteredMidVector3(2)+ICR(2);ICRCenteredMidVector3(3)+ICR(3)];
56
57 %Calc the output
58 outputVector = (midVector1+midVector2+midVector3)/3;
59
60 end

```

```

+2 abCode.m x motortest2.m x allWireLength.m x fullRotation.m x humeralAbduction.m x humeralFlexion.m * x +
1 function [FPrime] = humeralFlexion(B,BPrime,F,armAngleChange)
2 %humeralFlexion finds the position of the bottom of the humerus
3
4 BCenteredF = [F(1)-B(1);F(2)-B(2);F(3)-B(3)];
5
6 normalAxisofRotation = [1;0;0];
7
8 %Rotation around B
9 dotHumeral = dot(BCenteredF,normalAxisofRotation);
10 crossHumeral = cross(normalAxisofRotation,BCenteredF);
11
12 BCenteredMidVector = ((1-cos(armAngleChange))*(dotHumeral)*(normalAxisofRotation))+...
13 ((cos(armAngleChange))*(BCenteredF))+((sin(armAngleChange))*(crossHumeral));
14
15
16 midVector = [0.11; BCenteredMidVector(2)+B(2);BCenteredMidVector(3)+B(3)];
17 midVector2 = [0.11; midVector(2) + (B(2)-BPrime(2)); midVector(3) + (B(3)-BPrime(3))];
18
19 circleCenter = [0.11; BPrime(2); BPrime(3)];
20 radiusOfCircle = sqrt(abs(((0.3683)^2)-((BPrime(1)-0.11)^2)));
21
22 center2F = midVector2 - circleCenter;
23 magCenter2F = sqrt(center2F(2)^2+center2F(3)^2);
24 normalCenter2F = center2F/magCenter2F;
25 FPrime = [0.11;circleCenter(2)+(radiusOfCircle*normalCenter2F(2));circleCenter(3)+(radiusOfCircle*normalCenter2F(3))];
26
27 end

```

```

setup.m x abCode.m x motortest2.m x allWireLength.m x fullRotation.m x humeralAbduction.m * x +
1 function [FPrime] = humeralAbduction(B,BPrime,F,armAngleChange)
2 %humeralAbduction finds the position of the bottom of the humerus
3
4 BCenteredF = [F(1)-B(1);F(2)-B(2);F(3)-B(3)];
5
6 normalAxisofRotation = [0;-1;0];
7
8 %Rotation around B
9 dotHumeral = dot(BCenteredF,normalAxisofRotation);
10 crossHumeral = cross(normalAxisofRotation,BCenteredF);
11
12 BCenteredMidVector = ((1-cos(armAngleChange))*(dotHumeral)*(normalAxisofRotation))+...
13 ((cos(armAngleChange))*(BCenteredF))+((sin(armAngleChange))*(crossHumeral));
14
15
16 midVector = [BCenteredMidVector(1)+B(1);0.035;BCenteredMidVector(3)+B(3)];
17 midVector2 = [midVector(1) + (B(1)-BPrime(1)); 0.035; midVector(3) + (B(3)-BPrime(3))];
18
19 circleCenter = [BPrime(1); 0.035; BPrime(3)];
20 radiusOfCircle = sqrt(((0.3683)^2)-((BPrime(2)-0.035)^2));
21
22 center2F = midVector2 - circleCenter;
23 magCenter2F = sqrt(center2F(1)^2+center2F(3)^2);
24 normalCenter2F = center2F/magCenter2F;
25 FPrime = [circleCenter(1)+(radiusOfCircle*normalCenter2F(1));0.035;circleCenter(3)+(radiusOfCircle*normalCenter2F(3))];
26
27 end

```



```
setup.m x abCode.m x motortest2.m x allWireLength.m x fullRotation.m x +
1 function [positionMatrix] = fullRotation(A,B,C,D,E,I,J,K,upwardRotation,anteriorTilt,externalRotation,ICR)
2 %FULLROTATION rotates all points around the three axes
3 |
4 rotatedA = rotation (A,upwardRotation,anteriorTilt,externalRotation,I,J,K,ICR);
5 rotatedB = rotation (B,upwardRotation,anteriorTilt,externalRotation,I,J,K,ICR);
6 rotatedC = rotation (C,upwardRotation,anteriorTilt,externalRotation,I,J,K,ICR);
7 rotatedD = rotation (D,upwardRotation,anteriorTilt,externalRotation,I,J,K,ICR);
8 rotatedE = rotation (E,upwardRotation,anteriorTilt,externalRotation,I,J,K,ICR);
9 rotatedK = rotation (K,upwardRotation,anteriorTilt,externalRotation,I,J,K,ICR);
10 rotatedJ = rotation (J,upwardRotation,anteriorTilt,externalRotation,I,J,K,ICR);
11 rotatedI = rotation (I,upwardRotation,anteriorTilt,externalRotation,I,J,K,ICR);
12
13 positionMatrix = [rotatedA,rotatedB,rotatedC,rotatedD,rotatedE,rotatedI,rotatedJ,rotatedK];
14
15 end
```

```
setup.m x abCode.m x motortest2.m x allWireLength.m x +
1 function [wireLengths] = allWireLength(motorA,motorB,motorCPosY,motorCNegY,motorCX,motorD,motorE,motorFPosY,...
2   motorFNegY,motorFZ,A,B,C,D,E,F)
3 %WIRELENGTH Finds the length of a wire given the motor and the attachment
4 %point
5
6 threadLengthA = sqrt((motorA(1)-A(1))^2+(motorA(2)-A(2))^2+(motorA(3)-A(3))^2);
7 threadLengthB = sqrt((motorB(1)-B(1))^2+(motorB(2)-B(2))^2+(motorB(3)-B(3))^2);
8 threadLengthCPosY = sqrt((motorCPosY(1)-C(1))^2+(motorCPosY(2)-C(2))^2+(motorCPosY(3)-C(3))^2);
9 threadLengthCNegY = sqrt((motorCNegY(1)-C(1))^2+(motorCNegY(2)-C(2))^2+(motorCNegY(3)-C(3))^2);
10 threadLengthCX = sqrt((motorCX(1)-C(1))^2+(motorCX(2)-C(2))^2+(motorCX(3)-C(3))^2);
11 threadLengthD = sqrt((motorD(1)-D(1))^2+(motorD(2)-D(2))^2+(motorD(3)-D(3))^2);
12 threadLengthE = sqrt((motorE(1)-E(1))^2+(motorE(2)-E(2))^2+(motorE(3)-E(3))^2);
13 threadLengthFPosY = sqrt((motorFPosY(1)-F(1))^2+(motorFPosY(2)-F(2))^2+(motorFPosY(3)-F(3))^2);
14 threadLengthFNegY = sqrt((motorFNegY(1)-F(1))^2+(motorFNegY(2)-F(2))^2+(motorFNegY(3)-F(3))^2);
15 threadLengthFZ = sqrt((motorFZ(1)-F(1))^2+(motorFZ(2)-C(2))^2+(motorFZ(3)-F(3))^2);
16
17 wireLengths = [threadLengthA,threadLengthB,threadLengthCPosY,threadLengthCNegY,threadLengthCX,threadLengthD,threadLengthE,
18   threadLengthFPosY,threadLengthFNegY,threadLengthFZ];
19 end
```

```

1 function [currentAbIndex] = abCode(desiredIndex)
2
3 global currentAbIndex;
4
5 global currentFlexIndex
6 global abMatrix;
7
8 if currentFlexIndex > 1
9     flexCode(1)
10 end
11
12 a1 = arduino('COM4', 'Uno');
13 a2 = arduino('COM3', 'Uno');
14
15 pinDirA = "D12";
16 pinDirB = "D13";
17 pinDirCPosY = "D8";
18 pinDirCNegY = "D8";
19 pinDirCX = "D13";
20
21 pinDirD = "D12";
22 pinDirE = "D4";
23 pinDirFPosY = "D7";
24 pinDirFNegY = "D7";
25 pinDirFZ = "D4";
26
27
28
29 pinMovA = "D10";
30 pinMovB = "D11";
31 pinMovCPosY = "D9";
32 pinMovCNegY = "D9";
33 pinMovCX = "D11";
34
35 pinMovD = "D10";
36 pinMovE = "D5";
37 pinMovFPosY = "D6";
38 pinMovFNegY = "D6";
39 pinMovFZ = "D5";
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60
61
62
63
64
65
66
67
68
69
70
71
72

```

```

37 pinMovFPosY = "D6";
38 pinMovFNegY = "D6";
39 pinMovFZ = "D5";
40
41
42
43
44
45
46
47
48
49
50
51
52
53
54
55
56
57
58
59
60
61
62
63
64
65
66
67
68
69
70
71
72

```

```
setup.m x abCode.m x motortest2.m x +
75 i = 1;
76
77 if currentAbIndex < desiredIndex
78     while currentAbIndex < desiredIndex
79
80         while i<=5
81             deltaLength = abs(abMatrix(currentAbIndex,i)-abMatrix(currentAbIndex+1,i));
82
83             rotationDuration = deltaLength*116.886;
84
85             if abMatrix(currentAbIndex+1,i) > abMatrix(currentAbIndex,i)
86                 writeDigitalPin(a1,directionPins1(i),1)
87                 writeDigitalPin(a2,directionPins2(i),1)
88             else
89                 writeDigitalPin(a1,directionPins1(i),0)
90                 writeDigitalPin(a2,directionPins2(i),0)
91             end
92
93             writePWMDutyCycle(a1,movementPins1(i),0)
94             writePWMDutyCycle(a2,movementPins2(i),0)
95             minDutyCycle = 0.03;
96             maxDutyCycle = 0.12;
97             writePWMDutyCycle(a1,movementPins1(i),minDutyCycle)
98             writePWMDutyCycle(a2,movementPins2(i),minDutyCycle)
99
100             startTime = tic;
101
102             while toc(startTime) < rotationDuration
103                 % Adjust the duty cycle gradually to simulate rotation
104                 currentDutyCycle = minDutyCycle + (toc(startTime) / rotationDuration)...
105                     * (maxDutyCycle - minDutyCycle);
106                 writePWMDutyCycle(a1, movementPins1(i), currentDutyCycle);
107                 writePWMDutyCycle(a2, movementPins2(i), currentDutyCycle);
108
109                 % Add a small delay for smoother motion (adjust as needed)
110                 pause(0.01);
```

```
setup.m x abCode.m x motortest2.m x +
111         end
112
113         % Stop the servo motor by setting the duty cycle to 0
114         writePWMDutyCycle(a1, movementPins1(i), 0);
115         writePWMDutyCycle(a2, movementPins2(i), 0);
116         i = i+1;
117     end
118     currentAbIndex = currentAbIndex + 1;
119     i = 1;
120 end
121 else
122     while currentAbIndex > desiredIndex
123
124         while i<=5
125             deltaLength = abs(abMatrix(currentAbIndex,i)-abMatrix(currentAbIndex-1,i));
126
127
128             rotationDuration = deltaLength*116.886;
129
130
131             if abMatrix(currentAbIndex-1,i) > abMatrix(currentAbIndex,i)
132                 writeDigitalPin(a1,directionPins1(i),1)
133                 writeDigitalPin(a2, directionPins2(i),1)
134             else
135                 writeDigitalPin(a1,directionPins1(i),0)
136                 writeDigitalPin(a2,directionPins2(i),0)
137             end
138
139             writePWMDutyCycle(a1,movementPins1(i),0)
140             writePWMDutyCycle(a2,movementPins2(i),0)
141             minDutyCycle = 0.03;
142             maxDutyCycle = 0.12;
143             writePWMDutyCycle(a1,movementPins1(i),minDutyCycle)
144             writePWMDutyCycle(a2,movementPins2(i),minDutyCycle)
145
146
147             startTime = tic;
148
149             while toc(startTime) < rotationDuration
150                 % Adjust the duty cycle gradually to simulate rotation
151                 currentDutyCycle = minDutyCycle + (toc(startTime) / rotationDuration)...
152                     * (maxDutyCycle - minDutyCycle);
153                 writePWMDutyCycle(a1, movementPins1(i), currentDutyCycle);
154                 writePWMDutyCycle(a2, movementPins2(i), currentDutyCycle);
155
156                 % Add a small delay for smoother motion (adjust as needed)
157                 pause(0.01);
158             end
159
160             % Stop the servo motor by setting the duty cycle to 0
161             writePWMDutyCycle(a1, movementPins1(i), 0);
162             writePWMDutyCycle(a2, movementPins2(i), 0);
163             i = i+1;
164         end
165         currentAbIndex = currentAbIndex - 1;
166         i = 1;
167     end
168 end
169 clear a1
170 clear a2
171 end
```

```

1 function [currentFlexIndex] = flexCode(desiredIndex)
2
3 global currentFlexIndex;
4
5 global currentFlexIndex
6 global flexMatrix;
7
8 if currentFlexIndex > 1
9     flexCode(1)
10 end
11
12 a1 = arduino('COM4', 'Uno');
13 a2 = arduino('COM3', 'Uno');
14
15 pinDirA = "D12";
16 pinDirB = "D13";
17 pinDirCPosY = "D8";
18 pinDirCNegY = "D8";
19 pinDirCX = "D13";
20
21 pinDirD = "D12";
22 pinDirE = "D4";
23 pinDirFPosY = "D7";
24 pinDirFNegY = "D7";
25 pinDirFZ = "D4";
26
27
28
29 pinMovA = "D10";
30 pinMovB = "D11";
31 pinMovCPosY = "D9";
32 pinMovCNegY = "D9";
33 pinMovCX = "D11";
34
35 pinMovD = "D10";
36 pinMovE = "D5";
37

```

```

37 pinMovFPosY = "D6";
38 pinMovFNegY = "D6";
39 pinMovFZ = "D5";
40
41
42 configurePin(a2,pinDirA,'DigitalOutput')
43 configurePin(a2,pinDirB,'DigitalOutput')
44 configurePin(a2,pinDirCPosY,'DigitalOutput')
45 configurePin(a1,pinDirCNegY,'DigitalOutput')
46 configurePin(a1,pinDirCX,'DigitalOutput')
47 configurePin(a1,pinDirD,'DigitalOutput')
48 configurePin(a2,pinDirE,'DigitalOutput')
49 configurePin(a1,pinDirFZ,'DigitalOutput')
50 configurePin(a2,pinDirFPosY,'DigitalOutput')
51 configurePin(a1,pinDirFNegY,'DigitalOutput')
52
53 configurePin(a2,pinMovA,'PWM')
54 configurePin(a2,pinMovB,'PWM')
55 configurePin(a2,pinMovCPosY,'PWM')
56 configurePin(a1,pinMovCNegY,'PWM')
57 configurePin(a1,pinMovCX,'PWM')
58 configurePin(a1,pinMovD,'PWM')
59 configurePin(a2,pinMovE,'PWM')
60 configurePin(a1,pinMovFPosY,'PWM')
61 configurePin(a2,pinMovFNegY,'PWM')
62 configurePin(a1,pinMovFZ,'PWM')
63
64
65
66 directionPins1 = [pinDirFZ, pinDirCNegY, pinDirFNegY, pinDirD, pinDirCX];
67 directionPins2 = [pinDirA, pinDirB, pinDirCPosY, pinDirFPosY, pinDirE];
68
69
70 movementPins1 = [pinMovFZ, pinMovCNegY, pinMovFNegY, pinMovD, pinMovCX];
71 movementPins2 = [pinMovA, pinMovB, pinMovCPosY, pinMovFPosY, pinMovE];
72

```

```

75     i = 1;
76
77     if currentFlexIndex < desiredIndex
78         while currentFlexIndex < desiredIndex
79
80             while i<=5
81                 deltaLength = abs(flexMatrix(currentFlexIndex,i)-flexMatrix(currentFlexIndex+1,i));
82
83                 rotationDuration = deltaLength*116.886;
84
85                 if flexMatrix(currentFlexIndex+1,i) > flexMatrix(currentFlexIndex,i)
86                     writeDigitalPin(a1,directionPins1(i),1)
87                     writeDigitalPin(a2,directionPins2(i),1)
88                 else
89                     writeDigitalPin(a1,directionPins1(i),0)
90                     writeDigitalPin(a2,directionPins2(i),0)
91                 end
92
93                 writePWMDutyCycle(a1,movementPins1(i),0)
94                 writePWMDutyCycle(a2,movementPins2(i),0)
95                 minDutyCycle = 0.03;
96                 maxDutyCycle = 0.12;
97                 writePWMDutyCycle(a1,movementPins1(i),minDutyCycle)
98                 writePWMDutyCycle(a2,movementPins2(i),minDutyCycle)
99
100                startTime = tic;
101
102                while toc(startTime) < rotationDuration
103                    % Adjust the duty cycle gradually to simulate rotation
104                    currentDutyCycle = minDutyCycle + (toc(startTime) / rotationDuration)...
105                        * (maxDutyCycle - minDutyCycle);
106                    writePWMDutyCycle(a1, movementPins1(i), currentDutyCycle);
107                    writePWMDutyCycle(a2, movementPins2(i), currentDutyCycle);
108
109                    % Add a small delay for smoother motion (adjust as needed)
110                    pause(0.01);

```

```

111         end
112
113         % Stop the servo motor by setting the duty cycle to 0
114         writePWMDutyCycle(a1, movementPins1(i), 0);
115         writePWMDutyCycle(a2, movementPins2(i), 0);
116         i = i+1;
117     end
118     currentFlexIndex = currentFlexIndex + 1;
119     i = 1;
120 end
121 else
122     while currentFlexIndex > desiredIndex
123
124         while i<=5
125             deltaLength = abs(flexMatrix(currentFlexIndex,i)-flexMatrix(currentFlexIndex-1,i));
126
127
128             rotationDuration = deltaLength*116.886;
129
130
131             if flexMatrix(currentFlexIndex-1,i) > flexMatrix(currentFlexIndex,i)
132                 writeDigitalPin(a1,directionPins1(i),1)
133                 writeDigitalPin(a2, directionPins2(i),1)
134             else
135                 writeDigitalPin(a1,directionPins1(i),0)
136                 writeDigitalPin(a2,directionPins2(i),0)
137             end
138
139             writePWMDutyCycle(a1,movementPins1(i),0)
140             writePWMDutyCycle(a2,movementPins2(i),0)
141             minDutyCycle = 0.03;
142             maxDutyCycle = 0.12;
143             writePWMDutyCycle(a1,movementPins1(i),minDutyCycle)
144             writePWMDutyCycle(a2,movementPins2(i),minDutyCycle)
145
146

```

```

147     startTime = tic;
148
149     while toc(startTime) < rotationDuration
150         % Adjust the duty cycle gradually to simulate rotation
151         currentDutyCycle = minDutyCycle + (toc(startTime) / rotationDuration)...
152             * (maxDutyCycle - minDutyCycle);
153         writePWMDutyCycle(a1, movementPins1(i), currentDutyCycle);
154         writePWMDutyCycle(a2, movementPins2(i), currentDutyCycle);
155
156         % Add a small delay for smoother motion (adjust as needed)
157         pause(0.01);
158     end
159
160     % Stop the servo motor by setting the duty cycle to 0
161     writePWMDutyCycle(a1, movementPins1(i), 0);
162     writePWMDutyCycle(a2, movementPins2(i), 0);
163     i = i+1;
164 end
165 currentFlexIndex = currentFlexIndex - 1;
166 i = 1;
167 end
168 end
169 clear a1
170 clear a2
171 end

```

```

1 classdef shoulderRotationApp < matlab.apps.AppBase
2
3     % Properties that correspond to app components
4     properties (Access = public)
5         UIFigure          matlab.ui.Figure
6         ShowWireCheckBox  matlab.ui.control.CheckBox
7         HumeralFlexionSlider  matlab.ui.control.Slider
8         HumeralFlexionSliderLabel  matlab.ui.control.Label
9         HumeralAbductionSlider  matlab.ui.control.Slider
10        HumeralAbductionSliderLabel  matlab.ui.control.Label
11        UIAxesTop              matlab.ui.control.UIAxes
12        UIAxesSide              matlab.ui.control.UIAxes
13        UIAxesFront             matlab.ui.control.UIAxes
14        UIAxesAngled            matlab.ui.control.UIAxes
15    end
16
17    % Callbacks that handle component events
18    methods (Access = private)
19
20        % Code that executes after component creation
21        function startupFcn(app)
22
23            setup
24
25            global xCoordsPositionMatrixAb
26            global yCoordsPositionMatrixAb
27            global fMasterXAb
28            global fMasterYAb
29            global fMasterZAb
30
31            plot3(app.UIAxesAngled,[xCoordsPositionMatrixAb(1,1) xCoordsPositionMatrixAb(1,2) xCoordsPositionMatrixAb(1,5) xCoordsPositionMatrixAb(1,3) xCoordsPositionMatrixAb(1,4) xCoordsPositionMatrixAb(1,1)], ...
32                [yCoordsPositionMatrixAb(1,1) yCoordsPositionMatrixAb(1,2) yCoordsPositionMatrixAb(1,5) yCoordsPositionMatrixAb(1,3) yCoordsPositionMatrixAb(1,4) yCoordsPositionMatrixAb(1,1)], ...
33                [zCoordsPositionMatrixAb(1,1) zCoordsPositionMatrixAb(1,2) zCoordsPositionMatrixAb(1,5) zCoordsPositionMatrixAb(1,3) zCoordsPositionMatrixAb(1,4) zCoordsPositionMatrixAb(1,1)], 'k-', ...
34                [xCoordsPositionMatrixAb(5,2) fMasterXAb(1)], [yCoordsPositionMatrixAb(5,2) fMasterYAb(1)], [zCoordsPositionMatrixAb(5,2) fMasterZAb(1)], '-k-');
35
36            plot3(app.UIAxesFront,[xCoordsPositionMatrixAb(1,1) xCoordsPositionMatrixAb(1,2) xCoordsPositionMatrixAb(1,5) xCoordsPositionMatrixAb(1,3) xCoordsPositionMatrixAb(1,4) xCoordsPositionMatrixAb(1,1)], ...
37                [yCoordsPositionMatrixAb(1,1) yCoordsPositionMatrixAb(1,2) yCoordsPositionMatrixAb(1,5) yCoordsPositionMatrixAb(1,3) yCoordsPositionMatrixAb(1,4) yCoordsPositionMatrixAb(1,1)], ...
38                [zCoordsPositionMatrixAb(1,1) zCoordsPositionMatrixAb(1,2) zCoordsPositionMatrixAb(1,5) zCoordsPositionMatrixAb(1,3) zCoordsPositionMatrixAb(1,4) zCoordsPositionMatrixAb(1,1)], 'k-', ...
39                [xCoordsPositionMatrixAb(5,2) fMasterXAb(1)], [yCoordsPositionMatrixAb(5,2) fMasterYAb(1)], [zCoordsPositionMatrixAb(5,2) fMasterZAb(1)], '-k-');
40
41            app.UIAxesFront.CameraPosition = [0.05,1,-0.075];
42            app.UIAxesFront.CameraTarget = [0.05,0,-0.075];
43

```

```

44            plot3(app.UIAxesSide,[xCoordsPositionMatrixAb(1,1) xCoordsPositionMatrixAb(1,2) xCoordsPositionMatrixAb(1,5) xCoordsPositionMatrixAb(1,3) xCoordsPositionMatrixAb(1,4) xCoordsPositionMatrixAb(1,1)], ...
45                [yCoordsPositionMatrixAb(1,1) yCoordsPositionMatrixAb(1,2) yCoordsPositionMatrixAb(1,5) yCoordsPositionMatrixAb(1,3) yCoordsPositionMatrixAb(1,4) yCoordsPositionMatrixAb(1,1)], ...
46                [zCoordsPositionMatrixAb(1,1) zCoordsPositionMatrixAb(1,2) zCoordsPositionMatrixAb(1,5) zCoordsPositionMatrixAb(1,3) zCoordsPositionMatrixAb(1,4) zCoordsPositionMatrixAb(1,1)], 'k-', ...
47                [xCoordsPositionMatrixAb(5,2) fMasterXAb(1)], [yCoordsPositionMatrixAb(5,2) fMasterYAb(1)], [zCoordsPositionMatrixAb(5,2) fMasterZAb(1)], '-k-');
48
49            app.UIAxesSide.CameraPosition = [-1,0,-0.075];
50            app.UIAxesSide.CameraTarget = [0,0,-0.075];
51
52            plot3(app.UIAxesTop,[xCoordsPositionMatrixAb(1,1) xCoordsPositionMatrixAb(1,2) xCoordsPositionMatrixAb(1,5) xCoordsPositionMatrixAb(1,3) xCoordsPositionMatrixAb(1,4) xCoordsPositionMatrixAb(1,1)], ...
53                [yCoordsPositionMatrixAb(1,1) yCoordsPositionMatrixAb(1,2) yCoordsPositionMatrixAb(1,5) yCoordsPositionMatrixAb(1,3) yCoordsPositionMatrixAb(1,4) yCoordsPositionMatrixAb(1,1)], ...
54                [zCoordsPositionMatrixAb(1,1) zCoordsPositionMatrixAb(1,2) zCoordsPositionMatrixAb(1,5) zCoordsPositionMatrixAb(1,3) zCoordsPositionMatrixAb(1,4) zCoordsPositionMatrixAb(1,1)], 'k-', ...
55                [xCoordsPositionMatrixAb(5,2) fMasterXAb(1)], [yCoordsPositionMatrixAb(5,2) fMasterYAb(1)], [zCoordsPositionMatrixAb(5,2) fMasterZAb(1)], '-k-');
56
57            app.UIAxesTop.CameraPosition = [0.05,0,2];
58            app.UIAxesTop.CameraTarget = [0.05,0,0];
59
60            global currentAbIndex
61            global currentFlexIndex
62
63            if currentAbIndex > 1
64                abCode(1)
65            elseif currentFlexIndex > 1
66                flexCode(1)
67            end
68        end
69
70    % Value changed function: HumeralAbductionSlider
71    function HumeralAbductionSliderValueChanged(app, event)
72
73        global xCoordsPositionMatrixAb
74        global yCoordsPositionMatrixAb
75        global zCoordsPositionMatrixAb
76        global fMasterXAb
77        global fMasterYAb
78        global fMasterZAb
79
80        global masterPointAAb
81        global masterPointBAb
82        global masterPointCAb
83        global masterPointDAb
84        global masterPointEAb
85        global masterPointFAb
86

```



```
216 global motor0
217 global motorE
218 global motorF
219 global motorFPosy
220 global motorFnegy
221
222 changingValue = event.Value;
223 app.HumeralAbductionSlider.Value = 0;
224 getPoint = round((round(changingValue,1)/0.1)*1);
225
226 if app.ShowWireCheckBox.Value == 1
227     wireColor = 'r-';
228 elseif app.ShowWireCheckBox.Value == 0
229     wireColor = 'b-square';
230 end
231
232
233 plot3(app.UAxesAngled,[masterPointFlex(getPoint,1) motor0(1)], [masterPointFlex(getPoint,2) motor0(2)], [masterPointFlex(getPoint,3) motor0(3)], wireColor, ...
234 [masterPointBFlex(getPoint,1) motor0B(1)], [masterPointBFlex(getPoint,2) motor0B(2)], [masterPointBFlex(getPoint,3) motor0B(3)], wireColor, ...
235 [masterPointCFlex(getPoint,1) motor0C(1)], [masterPointCFlex(getPoint,2) motor0C(2)], [masterPointCFlex(getPoint,3) motor0C(3)], wireColor, ...
236 [masterPointDFlex(getPoint,1) motor0D(1)], [masterPointDFlex(getPoint,2) motor0D(2)], [masterPointDFlex(getPoint,3) motor0D(3)], wireColor, ...
237 [masterPointEFlex(getPoint,1) motor0E(1)], [masterPointEFlex(getPoint,2) motor0E(2)], [masterPointEFlex(getPoint,3) motor0E(3)], wireColor, ...
238 [masterPointFFlex(getPoint,1) motor0F(1)], [masterPointFFlex(getPoint,2) motor0F(2)], [masterPointFFlex(getPoint,3) motor0F(3)], wireColor, ...
239 [xCoordsPositionMatrixFlex(getPoint,1) xCoordsPositionMatrixFlex(getPoint,2) xCoordsPositionMatrixFlex(getPoint,3) xCoordsPositionMatrixFlex(getPoint,4) xCoordsPositionMatrixFlex(getPoint,1)], ...
240 [yCoordsPositionMatrixFlex(getPoint,1) yCoordsPositionMatrixFlex(getPoint,2) yCoordsPositionMatrixFlex(getPoint,3) yCoordsPositionMatrixFlex(getPoint,4) yCoordsPositionMatrixFlex(getPoint,1)], ...
241 [zCoordsPositionMatrixFlex(getPoint,1) zCoordsPositionMatrixFlex(getPoint,2) zCoordsPositionMatrixFlex(getPoint,3) zCoordsPositionMatrixFlex(getPoint,4) zCoordsPositionMatrixFlex(getPoint,1)], ...
242 [xCoordsPositionMatrixFlex(getPoint,2) #MasterXFlex(getPoint,1)], [yCoordsPositionMatrixFlex(getPoint,2) #MasterYFlex(getPoint,1)], [zCoordsPositionMatrixFlex(getPoint,2) #MasterZFlex(getPoint,1)], 'k-')
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249 plot3(app.UAxesFront,[masterPointFlex(getPoint,1) motor0A(1)], [masterPointFlex(getPoint,2) motor0A(2)], [masterPointFlex(getPoint,3) motor0A(3)], wireColor, ...
250 [masterPointBFlex(getPoint,1) motor0B(1)], [masterPointBFlex(getPoint,2) motor0B(2)], [masterPointBFlex(getPoint,3) motor0B(3)], wireColor, ...
251 [masterPointCFlex(getPoint,1) motor0C(1)], [masterPointCFlex(getPoint,2) motor0C(2)], [masterPointCFlex(getPoint,3) motor0C(3)], wireColor, ...
252 [masterPointDFlex(getPoint,1) motor0D(1)], [masterPointDFlex(getPoint,2) motor0D(2)], [masterPointDFlex(getPoint,3) motor0D(3)], wireColor, ...
253 [masterPointEFlex(getPoint,1) motor0E(1)], [masterPointEFlex(getPoint,2) motor0E(2)], [masterPointEFlex(getPoint,3) motor0E(3)], wireColor, ...
254 [masterPointFFlex(getPoint,1) motor0F(1)], [masterPointFFlex(getPoint,2) motor0F(2)], [masterPointFFlex(getPoint,3) motor0F(3)], wireColor, ...
255 [xCoordsPositionMatrixFlex(getPoint,1) xCoordsPositionMatrixFlex(getPoint,2) xCoordsPositionMatrixFlex(getPoint,3) xCoordsPositionMatrixFlex(getPoint,4) xCoordsPositionMatrixFlex(getPoint,1)], ...
256 [yCoordsPositionMatrixFlex(getPoint,1) yCoordsPositionMatrixFlex(getPoint,2) yCoordsPositionMatrixFlex(getPoint,3) yCoordsPositionMatrixFlex(getPoint,4) yCoordsPositionMatrixFlex(getPoint,1)], ...
257 [zCoordsPositionMatrixFlex(getPoint,1) zCoordsPositionMatrixFlex(getPoint,2) zCoordsPositionMatrixFlex(getPoint,3) zCoordsPositionMatrixFlex(getPoint,4) zCoordsPositionMatrixFlex(getPoint,1)], ...
258 [xCoordsPositionMatrixFlex(getPoint,2) #MasterXFlex(getPoint,1)], [yCoordsPositionMatrixFlex(getPoint,2) #MasterYFlex(getPoint,1)], [zCoordsPositionMatrixFlex(getPoint,2) #MasterZFlex(getPoint,1)], 'k-')
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605 % Component initialization
606 methods (Access = private)
607
608 % Create UIFigure and components
609 function createComponents(app)
610
611 % Create UIFigure and hide until all components are created
612 app UIFigure = uifigure('visible', 'off');
613 app UIFigure.Position = [100 100 786 588];
614 app UIFigure.Name = 'MATLAB App';
615
616 % Create UIAxesAngled
617 app UIAxesAngled = uiaxes(app UIFigure);
618 title(app UIAxesAngled, 'Angled View');
619 app UIAxesAngled.XLim = [-0.1 0.574];
620 app UIAxesAngled.VLim = [-0.49 0.49];
621 app UIAxesAngled.ZLim = [-0.48 0.48];
622 app UIAxesAngled.Position = [1 326 399 239];
623
624 % Create UIAxesFront
625 app UIAxesFront = uiaxes(app UIFigure);
626 title(app UIAxesFront, 'Front View');
627 app UIAxesFront.XLim = [-0.1 0.574];
628 app UIAxesFront.VLim = [-0.49 0.49];
629 app UIAxesFront.ZLim = [-0.48 0.48];
630 app UIAxesFront.Position = [399 326 388 239];
631
632 % Create UIAxesSide
633 app UIAxesSide = uiaxes(app UIFigure);
634 title(app UIAxesSide, 'Side View');
635 app UIAxesSide.View = [0 0];
636 app UIAxesSide.XLim = [-0.1 0.574];
637 app UIAxesSide.VLim = [-0.49 0.49];
638 app UIAxesSide.ZLim = [-0.48 0.48];
639 app UIAxesSide.Position = [20 107 380 220];
640
641 % Create UIAxesTop
642 app UIAxesTop = uiaxes(app UIFigure);
643 title(app UIAxesTop, 'Top View');
644 app UIAxesTop.CameraPosition = [0 0 1];
645 app UIAxesTop.CameraTarget = [0 0 0];
646 app UIAxesTop.XLim = [-0.1 0.574];
647 app UIAxesTop.VLim = [-0.49 0.49];

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647 app UIAxesTop.VLim = [-0.49 0.49];
648 app UIAxesTop.ZLim = [-0.48 0.48];
649 app UIAxesTop.Position = [370 107 387 220];
650
651 % Create HumeralAbductionSliderLabel
652 app HumeralAbductionSliderLabel = uilabel(app UIFigure);
653 app HumeralAbductionSliderLabel.HorizontalAlignment = 'right';
654 app HumeralAbductionSliderLabel.Position = [209 88 106 22];
655 app HumeralAbductionSliderLabel.Text = 'Humeral Abduction';
656
657 % Create HumeralAbductionSlider
658 app HumeralAbductionSlider = uislider(app UIFigure);
659 app HumeralAbductionSlider.Limits = [0 120];
660 app HumeralAbductionSlider.ValueChangedFcn = createCallbackFcn(app, @HumeralAbductionSliderValueChanged, true);
661 app HumeralAbductionSlider.Position = [336 97 382 3];
662
663 % Create HumeralFlexionSliderLabel
664 app HumeralFlexionSliderLabel = uilabel(app UIFigure);
665 app HumeralFlexionSliderLabel.HorizontalAlignment = 'right';
666 app HumeralFlexionSliderLabel.Position = [224 45 92 22];
667 app HumeralFlexionSliderLabel.Text = 'Humeral Flexion';
668
669 % Create HumeralFlexionSlider
670 app HumeralFlexionSlider = uislider(app UIFigure);
671 app HumeralFlexionSlider.Limits = [0 120];
672 app HumeralFlexionSlider.ValueChangedFcn = createCallbackFcn(app, @HumeralFlexionSliderValueChanged, true);
673 app HumeralFlexionSlider.Position = [337 54 381 3];
674
675 % Create ShowWiresCheckBox
676 app ShowWiresCheckBox = uicontrol(app UIFigure);
677 app ShowWiresCheckBox.ValueChangedFcn = createCallbackFcn(app, @ShowWiresCheckBoxValueChanged, true);
678 app ShowWiresCheckBox.Text = 'Show Wires';
679 app ShowWiresCheckBox.Position = [104 45 86 43];
680
681 % Show the figure after all components are created
682 app UIFigure.Visible = 'on';
683 end
684 end
685
686 % App creation and deletion
687 methods (Access = public)
688
689 % Construct app
690

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671 app HumeralFlexionSlider.Limits = [0 120];
672 app HumeralFlexionSlider.ValueChangedFcn = createCallbackFcn(app, @HumeralFlexionSliderValueChanged, true);
673 app HumeralFlexionSlider.Position = [337 54 381 3];
674
675 % Create ShowWiresCheckBox
676 app ShowWiresCheckBox = uicontrol(app UIFigure);
677 app ShowWiresCheckBox.ValueChangedFcn = createCallbackFcn(app, @ShowWiresCheckBoxValueChanged, true);
678 app ShowWiresCheckBox.Text = 'Show Wires';
679 app ShowWiresCheckBox.Position = [104 45 86 43];
680
681 % Show the figure after all components are created
682 app UIFigure.Visible = 'on';
683 end
684 end
685
686 % App creation and deletion
687 methods (Access = public)
688
689 % Construct app
690 function app = shoulderRotationApp
691
692 % Create UIFigure and components
693 createComponents(app)
694
695 % Register the app with App Designer
696 registerApp(app, app UIFigure)
697
698 % Execute the startup function
699 runStartupFcn(app, @startupFcn)
700
701 if nargin == 0
702 clear app
703 end
704 end
705
706 % Code that executes before app deletion
707 function delete(app)
708
709 % Delete UIFigure when app is deleted
710 delete(app UIFigure)
711 end
712 end
713 end

```

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